IN THE UNITED STATES PATENT AND TRADEMARK OFFICE
BEFORE THE US PATENT OFFICE BOARD OF PATENT APPEALS AND INTERFERENCES

Applicant:	Mark D. Scott et al.	Examiner: R. Hayes
Serial No.:	09/323,765	Group Art Unit: 1647
Filed:	June 1, 1999	Docket: 259.006US1
Title:	ANTIGENIC MODULATION OF CELLS	

SUBSTITUTE APPEAL BRIEF

MAIL STOP: APPEAL BRIEF - PATENTS
P.O. BOX 1450
Commissioner for Patents
Alexandria, VA22313-1450

Sir:

Applicants present this **SUBSTITUTE BRIEF ON APPEAL** in triplicate to the US PATENT OFFICE BOARD OF PATENT APPEALS AND INTERFERENCES and **request a personal appearance before the Board. The fee for payment of the personal appearance will be paid upon receipt of the Examiner's Answer.**

The U.S. Patent and Trademark Office is hereby authorized to debit any costs and fees associated with this Petition to Deposit Account No. 50-1391.

CERTIFICATE UNDER 37 C.F.R. 1.10:
'Express Mail' mailing number: EM 125426707 US
Date of Deposit: 24 April 2008
The undersigned hereby certifies that this Transmittal Letter and the paper or fee, as described herein, are being deposited with the United States Postal Service 'Express Mail Post Office To Addressee' service under 37 CFR 1.10 and is addressed to Mail Stop APPEAL BRIEF-PATENTS, Commissioner for Patents, PO Box 1450, Alexandria, VA 22313.

By: _____
MARK A. LITMAN

TABLE OF CONTENTS

REAL PARTY IN INTEREST

The real party in interest in this Appeal is the licensee of the full right, title and interest in this Application, Canadian Blood Services, 1800 Alta Vista, Ottawa, Ontario CANADA K1G 4J5.

RELATED APPEALS AND INTERFERENCES

The Appellant(s), the legal representative prosecuting this application and Appeal, and the assignee are not aware of any Appeals or Interferences that will directly affect or have a bearing on the Board's of Patent Appeals and Interferences decision in this pending Appeal.

STATUS OF CLAIMS

Claims 1-26, 28 and 31 are pending. Claims 27, 29-30 and 32-52 have been cancelled.

The amendment to claim 28, after final rejection, has been entered.

STATUS OF AMENDMENTS

An Amendment was filed after the Final Rejection on 20 July 2005 amending only claim 28 to remove a rejection under 35 USC112, second paragraph. The Amendment has been entered.

SUMMARY OF CLAIMED SUBJECT MATTER

Acute tissue rejection causes damage to tissue when antibody binding and complement fixation underlie the destruction of donor tissue. (Page 1, lines 22-29). Attempts to reduce the impact or occurrence of tissue rejection has focused on selection of compatible tissue (e.g., blood typing), chemical intervention to reduce rejection, and direct chemical blocking on the tissue (Page 1, line 26 through page 3, line 24). The use of adducts of materials with biactivated tresylPEG (polyethylene glycol) on a targeted materials has been specifically shown in the prior art (Page 4, lines 22-26). Improved methods of reducing or avoiding rejection are always desirable.

The present invention claims non-immunogenic cells (**Independent claims 1, 2, 3, 4, 5, 6 and 7**) and a method (**Independent claim 24**) by which cells may be converted to a non-immunogenic status by covalent attachment of a hydrophilic, biocompatible, non-immunogenic providing compound or polymer, with the cell displaying increased viability as compared to cells having even the same hydrophilic group attached by other chemical associations and reactions (Page 5, lines 2-27; page 6, lines 3-12; and pages 27-32). A hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently is attached to said surface so that recognition of said antigenic determinants on said surface is blocked by said covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer. (Claim 1)

Mapping of Independent Claims

1. A non-aggregating, non-immunogenic anuclear cellular composition consisting of **[page 11, line 8]**:

   a) a mammalian anuclear cell having a cell surface and antigenic determinants on said surface **[page 11, lines 9-10]**;

   b) a sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently attached to said surface so that recognition of said antigenic

determinants on said surface is blocked by said covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer **[page 11, lines 12-16]**.

2. (PREVIOUSLY PRESENTED) A non-aggregating, non-immunogenic nuclear cellular composition **[page 11, lines 8 and 18]** in which at least 25% by number of nuclear cells in said composition remain viable for 96 hours consisting of **[page 11, lines 18-19]**:

a) a mammalian nuclear cell having a cell surface and antigenic determinants on said surface **[page 11, lines 20-21]**;

b) a sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently attached to said surface so that recognition of said antigenic determinants on said surface is blocked by said covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer **[page 11, lines 22-27]**.

3. (PREVIOUSLY PRESENTED) A non-aggregating, non-immunogenic nuclear cellular composition **[page 11, lines 8 and 18; and page 12, line 1]]** having insufficient amounts of toxic materials within said composition to be toxic to nuclear cells within said composition consisting essentially of **[page 12, lines 1-3]**:

a) a mammalian nuclear cell having a cell surface and antigenic determinants on said surface; **[page 12, lines 4-6]**

b) a sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently attached to said surface so that recognition of said antigenic determinants on said surface is blocked by said covalently bonded hydrophilic,

biocompatible, non-immunogenicity providing compound or polymer. **[page 12, lines 7-11]**

4. (PREVIOUSLY PRESENTED) A non-aggregating, non-immunogenic anuclear or nuclear cellular composition consisting of: **[page 12, line 13]**

a) a mammalian anuclear or nuclear cell having a cell surface and antigenic determinants on said surface; **[page 12, lines 14-15]**

b) a sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently attached to said surface so that recognition of said antigenic determinants on said anuclear or nuclear cell surface is blocked by said covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer, said composition being free of any by-products from the covalent attachment of said hydrophilic, biocompatible, non-immunogenicity providing compound or polymer to said anuclear or nuclear cell surface. **[page 12, lines 16-14]**

5. (PREVIOUSLY PRESENTED) A non-aggregating, non-immunogenic cellular composition **[page 11, lines 8 and 18]** having insufficient amounts of toxic materials within said composition to be toxic to cells within said composition consisting essentially of: **[page 12, lines 26-27]**

a. a mammalian nuclear cell having a cell surface and antigenic determinants on said surface; **[page 12, lines 28-29]**

b. a sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently attached to said surface so that recognition of said antigenic determinants on said surface is blocked by said covalently

bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer. **[page 13, lines 1-15]**

6. (PREVIOUSLY PRESENTED) A viable, non-aggregating, non-immunogenic cellular composition consisting essentially of **[page 11, lines 8 and 18; and page 13, line 7]]**:

a) a mammalian nuclear cell having a cell surface and antigenic determinants on said surface; **[page 13, lines 8-9]**

b) a sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently attached to said surface so that recognition of said antigenic determinants on said surface is blocked by said covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer. **[page 13, lines 10-13]**

7. (PREVIOUSLY PRESENTED) A non-immunogenic cellular composition consisting essentially of: **[page 11, lines 8 and 18]**

a. a mammalian nuclear cell having a cell surface and antigenic determinants on said surface; **[page 13, lines 8-9]**

a sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently attached to said surface so that recognition of said antigenic determinants on said surface is blocked by said covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer. **[page 13, lines 10-13]**

24. (PREVIOUSLY PRESENTED) A method of producing a non-immunogenic mammalian cell, said method comprising: **[page 8, lines 20-30]**

covalently attaching an amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer to the cell

surface, directly or by means of a linking moiety, so that said hydrophilic, biocompatible, nonimmunogenicity providing compound or polymer blocks recognition of antigenic determinants on the cell surface and yields a non-immunogenic cell. **[page 13, lines 10-28]**

GROUNDS OF REJECTION TO BE REVIEWED ON APPEAL

1) **Claims 2-7, 18-21, 23-25, 28 and 31 have been rejected under 35 U.S.C. 102(e) as anticipated by Desai et al. (U.S. Patent No. 5,578,442) in light of Lin at al. (*1976*).**

2) **Claims 1, 4, 8, 10-16, 24 and 26 have been rejected under 35 U.S.C. 102(b) as anticipated by Francis et al. (WO 95/06058).**

3) **Claims 1-26, 28 and 31 have been rejected under 35 U.S.C. 103(a) as obvious over the combination of Desai et al. in light of Lin et al. (*1976*) and in view of Francis et al. (WO 95/06058)**

ARGUMENT

Solely for the purposes of expediting this Appeal and complying with the requirements of 37 C.F.R. 1.192(c)(7), the following grouping of claims is presented. This grouping is not intended to constitute any admission on the record that claims within groups may or may not be independently asserted in subsequent litigation or that for any judicial determination other than this Appeal, the claims may or may not stand by themselves against any challenge to their validity or enforceability.

The claims will be respectively grouped under the various rejections

1) **Claims 2-7, 18-21, 23-25, 28 and 31 have been rejected under 35 U.S.C. 102(e) as anticipated by Desai et al. (U.S. Patent No. 5,578,442) in light of Lin et al. (*1974*).**

Claims 2-7 and 24 shall stand or fall with the patentability of claim 2.

Claims 18, 28 and 31 shall stand or fall with the patentability of claim 18, this claim specifically reciting a linking group not specifically recited in earlier claims.

Claims 19-23 and 25 shall stand or fall together with the patentability of claim 19, based upon the recitation of the attachment of the covalent bond directly to the antigenic determinants.

2) **Claims 1, 4, 8, 10-16, 24 and 26 have been rejected under 35 U.S.C. 102(b) as anticipated by Francis et al. (WO 95/06058).**

Claims 1, 8, 15, 24 and 26 shall stand or fall with the patentability of claim 1.

Claim 4 shall stand or fall by itself, this claim reciting the absence of toxic bye-products, a limitation not present in other claims.

Claim 10 and 16 shall stand or fall with the patentability of claim 10, reciting a specific blocking group.

Claim 11 shall stand or fall by itself, reciting a specific blocking group.

Claim 12 shall stand or fall by itself, reciting a specific blocking group.

Claim 13 shall stand or fall by itself, reciting a specific position of attachment with regard to the cell.

Claim 14 shall stand or fall by itself, reciting a specific linking group.

3) Claims 1-26, 28 and 31 have been rejected under 35 U.S.C. 103(a) as obvious over the combination of Desai et al. in light of Lin et al. (1974) in view of Francis et al.

Claims 1, 3, 8, 15, 17, 24, 25 and 26 shall stand or fall with the patentability of claim 1.

Claims 2 and 9 shall stand or fall with the patentability of claim 2, reciting a specific degree and test for stability.

Claim 4 shall stand or fall by itself, this claim reciting the absence of toxic bye-products, a limitation not present in other claims.

Claims 5, 6 and 7 shall stand or fall with the patentability of claim 5, this claim differing from claim 1 in reciting a nuclear cell.

Claim 10 and 16 shall stand or fall with the patentability of claim 10, reciting a specific blocking group.

Claim 11 shall stand or fall by itself, reciting a specific blocking group.

Claim 12 shall stand or fall by itself, reciting a specific blocking group.

Claim 13 and 19-23 shall stand or fall with the patentability of claim 13, reciting a specific position of attachment with regard to the cell.

Claim 14 shall stand or fall by itself, reciting a specific linking group.

Claim 18 shall stand or fall by itself, reciting a specific position of attachment to the cell surface.

ASRGUMENTS OF APPELLANTS

1) Claims 2-7, 18-21, 23-25, 28 and 31 have been rejected under 35 U.S.C. 102(e) as anticipated by Desai et al. (U.S. Patent No. 5,578,442) in light of Lin et al. (1974).

Please note that claims 24 and 25 are method claims.

The Claims (represented by Claim 2, which is also highlighted for emphasis, below) specifically recite that the composition includes:

2. A non-aggregating, non-immunogenic nuclear cellular composition in which at least 25% by number of nuclear cells in said composition remain viable for 96 hours consisting of:

a) a mammalian nuclear cell having a cell surface and antigenic determinants on said surface; and

b) sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer **covalently attached to said surface** so that recognition of said antigenic determinants on said surface is blocked by said covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer. (Emphasis added).

These recitations are absolute and clear limitations on every claim remaining in the application. That specific limitation must be taught by Desai et al. for this rejection to be tenable. Desai et al do not teach covalent bonding of a non-immunogenic compound on a cell particle surface.

There is no specific disclosure that has been cited in the Office Action which asserts that the linker molecule is covalently bonded to the cell particle. The disclosure of Desai et al. clearly shows both the limitation of "covalent bonding" and bonding to a "cell particle" limitation to be absent from the invention contemplated by Desai et al.

Absence of Covalent Bonding

On column 5, line 38 through column 6, line 60, Desai et al. clearly describe a method and composition which "associates" a polycationic species with the negatively charged cell surface (e.g., column 5, lines 55-60). The language and disclosure in this section clearly denotes and describes an ionic association of the polycationic composition

which renders the cells non-immunogenic, Desai et al. repeatedly use language and description consistent with only ionic associations and inconsistent with covalent bonding. Even the reaction mechanisms for removal of the polycation binding to the cells and tissue is clearly incapable of relating to covalent bonding. Note specifically column 5, lines 55-67. The anions used to remove the polycationic materials from the cell surfaces must have high ionic strength. To remove a material from the cell surface that had been covalently bonded, specific types of chemical activity would have to be described.

The same section also refers to the necessary concentration of anionic species to reverse polycation binding to cells or tissue (column 5, lines 61-67). This language is specifically consistent with the existence of ionic binding and is inconsistent with covalent bonding. The fact that there is never any disclosure of specific reactive groups and reactions between the linker molecule and the cell surface is a further indication of the absence of any teaching or disclosure of covalent bonding to the cell surface by the linker molecule. In the absence of any indication of the necessary groups and reaction conditions for covalent bonding, and the consistent reference to ionic associations and ionic methods of release, it is absolutely clear that Desai et al. do not teach covalent bonding of the linker molecule to the cell surface.

Desai et al. cannot sustain a rejection under 35 U.S.C. 102(e) against the claims. The reference does not teach covalent bonding of the linker molecule to the cell particle surface or even to a cell surface. Although the Office Action repeats its assertion of the inherent formation of covalent bonds with the surfaces of cells or tissues, these assertion do not survive any serious scientific evaluation of the underlying technology.

The evidence to the contrary is that if the listed acids were capable of inherently forming covalent bonds with cells and tissues (in the absence of enzymes or catalysts for that specific reaction), life as we know it would cease on the Earth. If these and the other available alpha-amino acids could covalently bond to cells and tissues without enzymatic activity (which is not present in the *in vitro* environment of Desai), the cells and tissues

within the body would bond together. This would mean that blood cells would bond to vascular walls (e.g., cause clots and strokes), would crosslink tissue (e.g., the lungs), and cause other undesirable activities within the human body. These acids are present in foods, supplements and by-products of digestion and would covalently bond to the surface of the stomach, intestines, and other organs.

The Examiner has referred to portions of the Desai et al. specification where "free radical polymerization" is referred to, and these discussions have been asserted to reflect covalent bonding **to the cell**. The referred to section referred to free radical polymerization of components in the composition to each other, and there is no free radical polymerization to a cell, which would kill the cell. This would clearly fail to effect the successful recitation in claim 2 of the level of viability of the cell. This inability of strongly reactive materials to allow viability to continue in cells is supported by the showing on pages 27-32 of the specification, wherein the milder covalent bonding effected by the method of the invention enhanced cell survivability over the more intense bonding of Francis. Desai does not show covalent bonding **to the cell**, and if the language of the disclosure is misinterpreted to reflect free radical polymerization to the cell, that cell, like the cells of Francis (as shown on pages 27-32 of the specification) would not have a high degree of viability as recited in claim 2. Note the cited sections of the specification that the examiner refers to:

> "Optionally, **the polycationic species** employed in the practice of the present invention **can be further modified with one or more functional groups capable of undergoing free radical polymerization**. Suitable functional groups for this purpose include unsaturated species capable of free radical polymerization, such as, for example, acrylate groups, vinyl groups, methacrylate groups, and the like. When cells or tissues are treated with such modified polycationic species, the graft copolymer can be further subjected to free radical polymerization conditions, thereby stabilizing the association of graft copolymer with the cell surface. In

addition, the further crosslinking of the graft copolymer forms a highly stabilized, immunoprotective coating of water-soluble polymer about the treated cell or tissue.

The stabilization referred to in this paragraph is not free radical polymerization to the surface, but rather increasing the molecular weight of the species. The paragraph clearly states that the graft copolymer is crosslinked, not that there is any reaction to the cell surface by free radical polymerization. Any attempt to interpret the statement in the manner inherently asserted by the rejection is to extend the teachings of the reference to technology neither taught, implied or inherent. There simply is no showing of covalent bonding to the surface of the cell. The constant and repeated removability of the "polycationic species" clearly establishes that there is no covalent bonding. The rejection is clearly in error and must be withdrawn.

In summary, with regard to all claims (which recite covalent bonding), there appears to be clear evidence that the listed polyamino acids do not spontaneously, within the environment presented by Desai, form covalent bonds with cells and tissues.

NOTE: There is no Lin et al. reference (1976). The actual In et al. reference of record, cited and provided on June 3, 2004 (Not June 1, 2004 as indicated) is Lin and Riggs, "Photochemical Attachment of *lac* Repressor to Bromodeoxyuridine-Substituted *lac* Operator by Ultraviolet Radiation," *Proc. Nat. Acad. Sci.* Vol. **71**, No. 3, pp. 947-951, March 1974 (with a communication date of October 27, 1973). The reference to Lin et al. (1976) having been confusing and misleading.

Refutation of Materiality and Relevance and Impact of Lin et al. (1974)

It is first to be noted that Lin et al. has been cited in combination with Desai under 35 USC 102(e) so that the Lin et al. reference can do no more than explain the inherency of the teachings of DFesai and can add absolutely no material content to suggest modification of the actual teachings of Desai. To that end, Lin provides nothing of substance and does not overcome the reasons given above for the failure of the rejection.

The basis of the citation of Lin is to imply and assert that UV-crosslinking forms covalent bonds. The failure of this reference is that this teaching of Lin et al. (1974) is specific to linking protein to DNA. However, Cesai does not crosslink protein to DNA and the invention is not crosslinking protein to DNA. Rather, polymer units are covalently reacted to the surface of cells to form non-immunogenic functions to the cell. The polymerizable moieties discussed by Desai, **as noted above,** are not polymerized to the cell, but are polymerized to form a polymer and then the polymer is attached through ionic functions (forming an ionic bond, not covalent bond) with other species and possibly the cell surface. **Lin et al. (1974) is therefore ineffective as teaching any inherency in Desai as it is a non-equivalent process and phenomenon, and even if combined under 35 USC 103(a), which it has not been, offers no teaching that enables forming a covalent bond as recited in the claims.** The rejection is completely in error, with or without Lin et al. (**1974**).

Claims 2-7 and 24 shall stand or fall with the patentability of claim 2. As noted above, all of the claims fail to even show covalent bonding. There has been no showing either of the survivability recited in claim 2. That rate cannot be assumed, especially in view of the comparative showing in the specification (e.g., pages 27-32) evidencing the uniqueness and unobviousness of those results.

Claims 18, 28 and 31 shall stand or fall with the patentability of claim 18, this claim specifically reciting a linking group not specifically recited in earlier claims. Desai et al. do not show a linking unit derived from a cyanuric chloride reaction product. This rejection is therefore further not anticipated by the Desai et al. teachings.

Claims 19-23 and 25 shall stand or fall together with the patentability of claim 19, based upon the recitation of the attachment of the covalent bond directly to the antigenic determinants. Even given an erroneous conclusion that Desai et al. teach covalent bonding to the surface of the cell (which it **DOES NOT**), there is no teaching that Desai

et al. show bonding directly to the determinants. These claims are therefore additionally novel over the reference.

2. Claims 1, 4, 8, 10-16, 24 and 26 have been rejected under 35 U.S.C. 102(b) as anticipated by Francis et al. (WO 95/06058).

Claims 1, 4, 8, 10-16, 24 and 26 have been rejected under 35 U.S.C. 102(b) as anticipated by Francis et al. (WO 95/06058). This rejection is also respectfully traversed. Although Francis does apparently incidentally show the covalent bonding of a moiety (including PEG, the erythrocytes of Example 7) to the surface of a red blood cell, the bonding is done for the purpose of differentiating cells (so that they may be separated by ionic or electrostatic or other physical process), and only mammalian cells, as opposed to cell particles are bonded with the differentiating compound. **Please note that claims 24 and 26 are method claims.**

This rejection therefore fails because the combination of references fails to provide any motivation for the covalent bonding of compounds to the surface of nuclear or anuclear cells **with the provision of an anti-immunogenic effect**. Even with the teaching of Francis that compounds can be covalently bonded to mammalian cells (including red blood cells in Example 7), the specification specifically replicated the process of Francis et al., compared those cells to cells produced according to the present invention, and clearly established that the process of Francis et al. (**which was not intended to provide an anti-immunogenic** effect) did not produce an anti-immunogenic effect. In this regard, please note Example IX, and especially the conclusion on Page 30, lines 15-29, especially where it is stated in lines 25-29 that:

> "**As shown, CmPEG readily modifies the RBC** [red blood cell] **surface and confers immunocamoflage. In contrast, the TmPEG method as taught by Francis fails to significantly modify RBC and does not yield any protection from immune recognition (Figure 1).** (*emphasis added*)

All of the claims, in various language, effectively recited "A non-aggregating, non-immunogenic ... cellular composition..." Francis et al. has been shown to provide a cell composition that is **NOT** non-immunogenic. Francis et al. has therefore been shown to fail to anticipate the present invention. As direct, detailed, and uncontraverted evidence has been provided that shows that Francis et al. fails to anticipate this critical language of the claims, the rejection is clearly in error and must be withdrawn.

There is no motivation to perform a non-immunizing activity on nuclear or anuclear cells and clear evidence that the process of Francis et al. cannot provide that activity. Without such ability or motivation, there is no underlying basis for the assertion of obviousness.

The point of this argument is that Francis, even if covalent attachment is shown, destroys or greatly reduces the viability of the cells, contrary to the teachings of the present invention. This result is consistent with the purpose of Francis, which does not seek to create viable cells with immunogenic properties, but merely intends to provide a method of separating cells by bonding weighted polymers to them to make them more easily separable. This gross material addition to cells to make them more distinguishable is not material or functionally related to the purpose of creating **viable immunogenic cells**. Having no intent at cell survival, Francis uses techniques that reduce cell viability to a degree (shown by comparison in the specification examples on page 27-32) that are outside the limits of all claims. The term viable, alone, is sufficient to show lack of anticipation between the teachings of Francis and the claimed invention.

Claims 1, 8, 15, 24 and 26 shall stand or fall with the patentability of claim 1. The novelty of these claims has been firmly established above.

Claim 4 shall stand or fall by itself, this claim reciting the absence of toxic bye-products, a limitation not present in other claims. The novelty of this claim has been established above. Additionally, the examples and accompanying descriptions on pages 27-32 show that Francis produces waste bye-products that damage the cells. The reference therefore clearly fails to anticipate the invention as claimed.

Claims 5, and 7 shall stand or fall with the patentability of claim 5, this claim differing from claim 1 in reciting a nuclear cell. The arguments for establishing the novelty of these claims is otherwise identical to those presented with respect to claim 1 above.

Claim 10 and 16 shall stand or fall with the patentability of claim 10, reciting a specific blocking group. Francis does not show a linking unit derived from a cyanuric chloride reaction product. This rejection is therefore further not anticipated by the Francis teachings.

Claim 11 shall stand or fall by itself, reciting a specific blocking group. This specific blocking group has not been asserted to be shown by Francis and is therefore novel.

Claim 12 shall stand or fall by itself, reciting a specific blocking group. This specific blocking group has not been asserted to be shown by Francis and is therefore novel.

Claim 13 shall stand or fall by itself, reciting a specific position of attachment with regard to the cell. Francis has not been found nor asserted to show covalent bonding directly to the determinants on the cell surface. The rejection must additionally fail for that reason.

Claim 14 shall stand or fall by itself, reciting a specific linking group. Francis does not show a linking unit derived from a cyanuric chloride reaction product. This rejection is therefore further not anticipated by the Francis teachings.

3 . Claims 1-26, 28 and 31 have been rejected under 35 U.S.C. 103(a) as obvious over the combination of Desai et al. in light of Lin et al. (1976) in view of Francis et al.

This rejection is clearly in error, at least for the following reason. Desai et al. has been clearly established as failing to show covalent bonding of PEG to cell surfaces. The Francis et al. reference, showing a specific format for providing covalent bonding of PEG

to a cell surface for a purpose other than providing non-immunogenicity, **fails to provide non-immunogenicity by his sole described method.** That fact has been established by direct comparison of the Francis et al. method and a method according to the practice of the invention. Therefore, even if the methods of Desai et al. and Francis et al. were combined, they would not be expected to provide the properties recited in the claims. There is no predictability, motivation or assurance that any combined product or process of Desai in view of Francis could produce a viable cell without consideration of the teachings of the present Application.

The rejection is therefore clearly in error. Not only was the covalent bonding shown by Francis et al. not intended to provide non-immunogenicity, the actual effect of the process failed to provide non-immunogenicity. The combination therefore fails to show that the invention as a whole, including the resulting properties, are obvious. The rejection therefore fails to meet minimum statutory requirements to establish a *prima facie* case of obviousness. The rejection is in error and must be withdrawn.

Additionally, the purpose for the covalent bonding of compounds to mammalian cell shown by Francis is for a fundamentally different purpose than that shown by Desai. Desai requires the preparation of reversible, non-adhesive cells, while Francis is teaching the preparation of adducts of a polymer and a targeted material, which are shown to be differentiable (e.g., in solvents so that they separate). Although Desai does teach that his reversible attachment (ionic attachment) of can reduce aggregation, Francis appears to indicate that aggregation still occurs with both his inventive composition and with control compositions (Examples 3 and 4). There is no nexus between the two references that would allow their combination, even if they are proposed to be combined. In addition, with this fundamental difference in the objective of the two references, they would not be combined to motivate one skilled in the art to modify the surface of a cell particle, a process not taught in either reference.

The basis of the citation of Lin is to imply and assert that UV-crosslinking forms covalent bonds. The failure of this reference is that this teaching of Lin et al. (1974) is

specific to linking protein to DNA. However, Desai does not crosslink protein to DNA and the invention is not crosslinking protein to DNA. Rather, polymer units are covalently reacted to the surface of cells to form non-immunogenic functions to the cell. The polymerizable moieties discussed by Desai, **as noted above,** are not polymerized to the cell, but are polymerized to form a polymer and then the polymer is attached through ionic functions (forming an ionic bond, not covalent bond) with other species and possibly the cell surface. **Lin et al. (1974) is therefore ineffective as teaching any obviousness from the teachings of Desai as it is a non-equivalent process and phenomenon, and even if combined under 35 USC 103(a), Lin et al. (1974) offers no teaching that enables forming a covalent bond between the non-immunogenic responsive polymer and the cell as recited in the claims.** The rejection is completely in error, with or without Lin et al. (**1974**).

Claims 1, 3, 8, 15, 17, 24, 25 and 26 shall stand or fall with the patentability of claim 1. The arguments directly above reflect the basic position on this set of claims. Those arguments are also applicable to all other claims in the Application, even where additional novel and unobvious features are shown. **Please note that claims 24, 25 and 26 are Method claims.**

Claims 2 and 9 shall stand or fall with the patentability of claim 2, reciting a specific degree and test for stability. Extensive comparisons were provided in the specification on pages 27-32 which have not been given their technical respect. That evidence is compelling on the fact that the recited covalent bonding and the specific degree of viability (which is recited in these claims) has not been shown to be taught, obvious, enabled or otherwise available from the teachings of these references. These properties are clearly not inherent as the reprise of the Francis process shows a significantly lower viability rate. There is no legal basis for the continued assertion of unobviousness except by ignoring the data and examples or by applying unwarranted pejorative attacks on the examples.

Claim 4 shall stand or fall by itself, this claim reciting the absence of toxic bye-products, a limitation not present in other claims. The novelty of this claim has been established above. Additionally, the examples and accompanying descriptions on pages 27-32 show that Francis produces waste bye-products that damage the cells. The reference therefore clearly fails to anticipate the invention as claimed.

Claims 5, 6 and 7 shall stand or fall with the patentability of claim 5, this claim differing from claim 1 in reciting a nuclear cell. Patentability arguments are otherwise the same as those provided above for Claim 1.

Claim 10 and 16 shall stand or fall with the patentability of claim 10, reciting a specific blocking group. Neither Francis nor Desai et al. show a linking unit derived from a cyanuric chloride reaction product. This rejection is therefore further not anticipated by the Francis teachings.

Claim 11 shall stand or fall by itself, reciting a specific blocking group. Neither Desai et al. nor Francis show this specific blocking group. It has not been asserted to be shown by Francis or Desai and is therefore novel and unobvious.

Claim 12 shall stand or fall by itself, reciting a specific blocking group. Neither Desai et al. nor Francis show this specific blocking group. It has not been asserted to be shown by Francis or Desai and is therefore novel and unobvious.

Claim 13 and 19-23 shall stand or fall with the patentability of claim 13, reciting a specific position of attachment with regard to the cell. Neither Desai et al. nor Francis has been asserted to specifically show attachment at the determinant sites. In the absence of such a teaching in either reference, the rejection must fail.

Claim 14 shall stand or fall by itself, reciting a specific linking group. Neither Desai et al. or Francis shows a linking unit derived from a cyanuric chloride reaction product. This rejection is therefore further not anticipated by the Francis teachings.

Claim 18 shall stand or fall by itself, reciting a specific position of attachment to the cell surface. Neither Desai et al. or Francis shows a linking unit derived from a

cyanuric chloride reaction product. This rejection is therefore further not anticipated by the Francis teachings.

This rejection is in error and must be withdrawn.

CONCLUSION

All rejections of record have been shown in detail to be in error. The rejection should be reversed and all claims should be indicated as allowable.

Applicants believe the claims are in condition for allowance and request reconsideration of the application and allowance of the claims. The Examiner is invited to telephone the below-signed attorney at 952-832-9090 to discuss any questions that may remain with respect to the present application.

Respectfully submitted,
MARK D. SCOTT, et al.

By Their Representatives,
MARK A. LITMAN & ASSOCIATES, P.A.
York Business Center, Suite 205
3209 West 76th Street
Edina, MN 55435
(952)832.9090

Date 24 APRIL2008 By _____
Mark A. Litman
Reg. No. 26,390

I hereby certify that this correspondence is being deposited with the United States Postal Service as first class mail in an envelope addressed to Box: APPEAL BRIEF - PATENTS, P.O. BOX 1450; Commissioner for Patents, Alexandria, VA 22313-1450 on 24 APRIL2008.

CERTIFICATE UNDER 37 C.F.R. 1.10:
'Express Mail' mailing number: EM 125426707 US
Date of Deposit: 24 April 2008
The undersigned hereby certifies that this Transmittal Letter and the paper or fee, as described herein, are being deposited with the United States Postal Service 'Express Mail Post Office To Addressee' service under 37 CFR 1.10 and is addressed to Mail Stop APPEAL BRIEF-PATENTS, Commissioner for Patents, PO Box 1450, Alexandria, VA 22313.

By: _____
MARK A. LITMAN

APPENDIX - THE CLAIMS ON APPEAL

1. (ON APPEAL) A non-aggregating, non-immunogenic anuclear cellular composition consisting of:

c) a mammalian anuclear cell having a cell surface and antigenic determinants on said surface;

d) a sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently attached to said surface so that recognition of said antigenic determinants on said surface is blocked by said covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer.

2. (ON APPEAL) A non-aggregating, non-immunogenic nuclear cellular composition in which at least 25% by number of nuclear cells in said composition remain viable for 96 hours consisting of:

c) a mammalian nuclear cell having a cell surface and antigenic determinants on said surface;

d) a sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently attached to said surface so that recognition of said antigenic determinants on said surface is blocked by said covalently

bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer.

3. (ON APPEAL) A non-aggregating, non-immunogenic nuclear cellular composition having insufficient amounts of toxic materials within said composition to be toxic to nuclear cells within said composition consisting essentially of:

c) a mammalian nuclear cell having a cell surface and antigenic determinants on said surface;

d) a sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently attached to said surface so that recognition of said antigenic determinants on said surface is blocked by said covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer.

4. (ON APPEAL) A non-aggregating, non-immunogenic anuclear or nuclear cellular composition consisting of:

c) a mammalian anuclear or nuclear cell having a cell surface and antigenic determinants on said surface;

d) a sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently attached to said surface so that recognition of said antigenic determinants on

said anuclear or nuclear cell surface is blocked by said covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer, said composition being free of any by-products from the covalent attachment of said hydrophilic, biocompatible, non-immunogenicity providing compound or polymer to said anuclear or nuclear cell surface.

5. (ON APPEAL) A non-aggregating, non-immunogenic cellular composition having insufficient amounts of toxic materials within said composition to be toxic to cells within said composition consisting essentially of:

a. a mammalian nuclear cell having a cell surface and antigenic determinants on said surface;

b. a sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently attached to said surface so that recognition of said antigenic determinants on said surface is blocked by said covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer.

6. (ON APPEAL) A viable, non-aggregating, non-immunogenic cellular composition consisting essentially of:

c) a mammalian nuclear cell having a cell surface and antigenic determinants on said surface;

d) a sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently attached to said surface so that recognition of said antigenic determinants on said surface is blocked by said covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer.

7. (ON APPEAL) A non-immunogenic cellular composition consisting essentially of:

a. a mammalian nuclear cell having a cell surface and antigenic determinants on said surface;

a sufficient amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer covalently attached to said surface so that recognition of said antigenic determinants on said surface is blocked by said covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer.

8. (ON APPEAL) The cellular composition of claim 1 wherein said hydrophilic, biocompatible, non-immunogenicity providing compound or polymer is a polyalkylene glycol.

9. (ON APPEAL) The cellular composition of claim 1 wherein said hydrophilic, biocompatible, non-immunogenicity providing compound or polymer is a methoxypolyalkylene glycol.

10. (ON APPEAL) The cellular composition of claim 1 wherein said hydrophilic, biocompatible, non-immunogenicity providing compound or polymer is a dextran.

11. (ON APPEAL) The cellular composition of claim 1 wherein said hydrophilic, biocompatible, non-immunogenicity providing compound or polymer is Ficoll.

12. (ON APPEAL) The cellular composition of claim 1 wherein said hydrophilic, biocompatible, non-immunogenicity providing compound or polymer is arabinogalactan.

13. (ON APPEAL) The cellular composition of claim 1 wherein said linking moieties are covalently bonded to said antigenic determinants on said cell surface.

14. (ON APPEAL) The cellular composition of claim 1 wherein said cell is an anuclear cell and the covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer is covalently bonded to the nuclear cell through a unit derived from reaction of a cyanuric chloride linking group on the covalently bonded

hydrophilic, biocompatible, non-immunogenicity providing compound or polymer to the cell surface.

15. (ON APPEAL) The cellular composition of claim 1 wherein said anuclear cell is a red blood cell.

16. (ON APPEAL) The cellular composition of claim 10 wherein the antigenic determinants comprise a blood group antigenic determinants.

17. (ON APPEAL) The cellular composition of claim 1 wherein said anuclear cell is a platelet.

18. (ON APPEAL) The cellular composition of claim 2 wherein said cell is a lymphocyte and the covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer is covalently bonded to the nuclear cell through a unit derived from reaction of a cyanuric chloride linking group on the covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer to the cell surface.

19. (ON APPEAL) The cellular composition of claim 2 wherein linking moieties covalently attach the hydrophilic, biocompatible, non-immunogenicity providing

compound or polymer to said surface, said linking moieties are covalently attached to said antigenic determinants on said cell surface and said nucleated cell is a vascular endothelial cell.

20. (ON APPEAL) The cellular composition of claim 2 wherein linking moieties covalently attach the hydrophilic, biocompatible, non-immunogenicity providing compound or polymer to said surface, said linking moieties are covalently attached to said antigenic determinants on said cell surface and said nucleated cell is a hepatic cell.

21. (ON APPEAL) The cellular composition of claim 2 wherein linking moieties covalently attach the hydrophilic, biocompatible, non-immunogenicity providing compound or polymer to said surface, said linking moieties are covalently attached to said antigenic determinants on said cell surface and said nucleated cell is a neuronal cell.

22. (ON APPEAL) The cellular composition of claim 2 wherein linking moieties covalently attach the hydrophilic, biocompatible, non-immunogenicity providing compound or polymer to said surface, said linking moieties are covalently attached to said antigenic determinants on said cell surface and said nucleated cell is a pancreatic cell.

23. (ON APPEAL)The cellular composition of claim 2 wherein linking moieties covalently attach the hydrophilic, biocompatible, non-immunogenicity providing compound or polymer to said surface, said linking moieties are covalently attached to said antigenic determinants on said cell surface and said nucleated cell is an epithelial cell.

24. (ON APPEAL) A method of producing a non-immunogenic mammalian cell, said method comprising:

> covalently attaching an amount of hydrophilic, biocompatible, non-immunogenicity providing compound or polymer to the cell surface, directly or by means of a linking moiety, so that said hydrophilic, biocompatible, nonimmunogenicity providing compound or polymer blocks recognition of antigenic determinants on the cell surface and yields a non-immunogenic cell.

25. (ON APPEAL)The method of claim 24 wherein linking moieties covalently attach the hydrophilic, biocompatible, non-immunogenicity providing compound or polymer to said surface, said linking moiety is covalently bonded to said antigenic determinants on said cell surface.

26. (ON APPEAL) The method of claim 24 wherein said cell is a red blood cell.

27. (CANCELLED)

28, (ON APPEAL) The cellular composition of claim 21 wherein said cell is part of a tissue or organ and the covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer is covalently bonded to the nuclear cell through a unit derived from reaction of a cyanuric chloride linking group on the covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer to the cell surface.

29. (CANCELLED)

30. (CANCELLED)

31. (ON APPEAL) The cellular composition of claim 1 wherein said cell is a platelet and the covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer is covalently bonded to the nuclear cell through a unit derived from reaction of a cyanuric chloride linking group on the covalently bonded hydrophilic, biocompatible, non-immunogenicity providing compound or polymer to the cell surface.

32.-52. (CANCELLED)

Evidence Appendix Page(s)

Solely because the Notice of Non-Compliant Brief specifically requested the following statement, the copies of the **REFERENCES** of:

1) Desai (US Patent No. 5,578,442); and
2) Lin and Riggs, "Photochemical Attachment of *lac* Repressor to Bromodeoxyuridine-Substituted *lac* Operator by Ultraviolet Radiation," *Proc. Nat. Acad. Sci.* Vol. **71**, No. 3, pp. 947-951, March 1974 (with a communication date of October 27, 1973); and
3) Francis et al. (WO 95/06058)

are included herewith. Appellants would like to point out that this material is not evidence, but cited references. Extrinsic evidence does not include the references cited by the Examiner. Rather, commentary to the Rules state:

"Evidence appendix. An appendix containing copies of any evidence submitted pursuant to § § 1.130, 1.131, or 1.132 of this title or of any other evidence entered by the examiner and relied upon by appellant in the appeal, along with a statement setting forth where in the record that evidence was entered in the record by the examiner. Reference to unentered evidence is not permitted in the brief. See § 41.33 for treatment of evidence submitted after appeal. This appendix may also include copies of the evidence relied upon by the examiner as to grounds of rejection to be reviewed on appeal."

The cited references, in spite of the requirements of the Examiner which have been complied with, do not constitute extrinsic evidence as intended by this section. It is still the position of the Counsel of record that no extrinsic evidence is relied upon in this Appeal. There is no evidence of record with which this Appeal must be concerned other than the arguments and the references themselves, but Applicants again are attempting to fully comply with every request by the PTO.

Related proceedings appendix page(s)

There are no related proceedings in any official court, board, judicial or quasi-judicial venue in the United States regarding this Application or any related application to the knowledge of Appellants and their Counsel.

Proc. Nat. Acad. Sci.
Vol. 71, No. 3, pp. 947–951, March 1974

Photochemical Attachment of *lac* Repressor to Bromodeoxyuridine-Substituted *lac* Operator by Ultraviolet Radiation

(catabolite gene activator protein/protein–DNA interaction/nitrocellulose-filter assay)

SYR-YAUNG LIN AND ARTHUR D. RIGGS

City of Hope National Medical Center, Duarte, California 91010

Communicated by Matthew Meselson, October 27, 1973

ABSTRACT **The transducing phage λh80*dlac* carries the *lac* operator, whereas wild-type λh80 does not. We find that in high salt (0.18 M KCl), ultraviolet radiation causes the formation of a very stable complex between repressor and 5-bromodeoxyuridine (BrdU)-substituted λh80*dlac* but not to BrdU-λh80 DNA. Studies with inducers of the *lac* operon confirm the specificity of attachment. In low salt (0.01 M KCl), ultraviolet radiation will also attach repressor nonspecifically to BrdU-λh80 DNA. The stability of the complex suggests that covalent bonds are formed. We also report that another regulatory protein, the catabolite gene activator protein, can be attached similarly to DNA.**

Smith first noted that ultraviolet (UV) radiation cross-links protein to DNA, both *in vivo* and *in vitro* (1). The experimental evidence for cross-linking was that after UV treatment, DNA was not extractable from sodium dodecyl sulfate (SDS)–protein precipitates. This work has been reviewed (2). Proteins known to bind to DNA were not studied. Recently, Markovitz (3) demonstrated that UV irradiation results in covalent bond formation between DNA polymerase and DNA. Stimulated by the work of Markovitz, we tried to demonstrate the specific cross-linking of *lac* repressor to *lac* operator in λh80*dlac* DNA. These experiments were not successful until 5-bromodeoxyuridine (BrdU)-substituted λh80*dlac* DNA was used. We report here the photochemical attachment of *lac* repressor specifically to BrdU-substituted *lac* operator.

METHODS

We prepared *lac* repressor (i^{superq}) from strain M96 following the procedure of Müller-Hill, Beyreuther, and Gilbert (4). To ensure purity, additional chromatography on DEAE-Sephadex was done (5). The preparation was free of impurities detectable by SDS–acrylamide gel electrophoresis and all DNA-binding activity (including photochemical cross-linking) sedimented in a sucrose gradient as *lac* repressor. The nitrocellulose filter assay for repressor–DNA complexes has been described in detail (6, 7). Because of somewhat lower background and better reproducibility, we are now using type HAMK filters from the Millipore Corp. The basic procedures for preparing BrdU-substituted λh80*dlac* [^{32}P]DNA and λh80 [^{32}P]DNA are published (8). For this work the thymine-requiring double lysogen, JG108 ($\lambda h_{80}C_{I857}S_{c68}dlac$, $\lambda h_{80}C_{I857}S_{c68}$), was grown in medium containing 10 μg/ml of BrdU and 0.2 μg/ml of thymidine for 30 min prior to heat induction. This procedure leads to about 90% substitution BrdU for thymidine as estimated by buoyant density measurements in CsCl (9).

For most experiments, ultraviolet light treatment was at a distance of 11 cm from a short wavelength mineral light (Ultraviolet Products, model UVS-11). The sample (0.75 ml) was in 0.5 × 2-inch polyallomer tubes situated directly below the UV lamp. Irradiation was usually done at room temperature (25°) in buffer I, which contains: 10 mM KCl, 10 mM Tris·HCl (pH 7.4), 0.1 mM EDTA, 0.1 mM dithiothreitol, 5% (v/v) dimethylsulfoxide, and 50 μg/ml of BSA. The BSA was heat treated at 70° for 2 hr at pH 9.0. UV dosage was measured with an ultraviolet meter (Ultraviolet Products, model J-225). Test tubes with the bottom cut out were used to estimate the dose actually received by the sample.

RESULTS

The specific binding of *lac* repressor to *lac* operator has been firmly established (10, 11) and studied in detail using nitrocellulose filters to asay for repressor–operator complex (6, 12–14). Repressor binding to operator is eliminated by isopropyl-β-D-thiogalactoside (IPTG), a good inducer of the *lac* operon. IPTG at 10^{-3} M causes preformed repressor–operator complexes to dissociate in a few seconds, even in low ionic strength buffers (ref. 13, and our unpublished data). The binding of repressor to operator is also very sensitive to salt concentration and preformed repressor–operator coinplexes dissociate quickly in high salt (13). *Lac* repressor has a relatively weak, but nonetheless measurable, affinity for DNA not containing the *lac* operator (7). Repressor binding to nonoperator DNA is sensitive to ionic strength, but is not affected by IPTG (7).

The results above were obtained using normal, unsubstituted DNA. However, as shown in Fig. 1, the binding of repressor to BrdU-substituted DNA is basically similar. Specificity for operator is easily demonstrated because IPTG eliminates the binding (Fig. 1 and ref. 8) and no binding is observed if DNA without the *lac* operon (BrdU-λh80 [^{32}P]-DNA) is used (data not shown). An important difference between normal and BrdU-substituted operator is that the rate of dissociation of *lac* repressor is ten times slower from the latter (8). Recent work (Lin and Riggs, unpublished) has established that the equilibrium affinity of *lac* repressor for both operator and nonoperator BrdU-substituted DNA is increased about one order of magnitude.

Specific attachment. Fig. 2*A* shows that, in 0.18 M KCl, UV irradiation leads to the formation of IPTG-resistant complexes between repressor and BrdU-λh80*dlac* DNA. The zero

Abbreviations: BSA, bovine-serum albumin; BrdU, 5-bromodeoxyuridine; CAP, catabolite gene-activator protein; IPTG, isopropyl-β-D-thiogalactoside; SDS, sodium dodecyl sulfate; UV, ultraviolet.

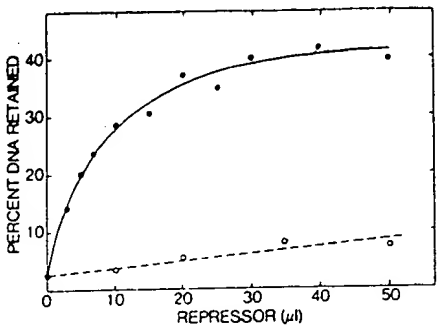


FIG. 1. Binding of *lac* repressor to BrdU-substituted λh80-*dlac* [^{32}P]DNA. Various amounts of repressor were added to 0.4 ml of buffer I, containing 25 ng of BrdU-substituted λh80-*dlac* [^{32}P]DNA. The reaction mixtures were incubated at room temperature for at least 30 min before filtration on Millipore filters. In some tubes, IPTG was added to a final concentration of 10^{-3} M before adding repressor. Each point is the average of three filters. ●——●, without IPTG. O- - -O, IPTG added to a final concentration of 1 mM before adding repressor.

time point serves as a control to establish that without UV irradiation, IPTG completely eliminates repressor–operator complexes. Repressor must be present during irradiation; prior irradiation of the DNA does not lead to stable complex formation. Under these conditions, no stable complex is formed with BrdU-λh80 DNA. The BrdU-λh80 DNA was

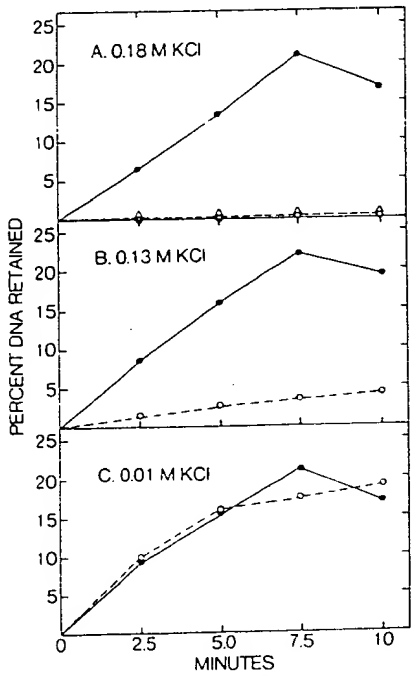


FIG. 2. Formation of IPTG-stable complexes between *lac* repressor and BrdU-DNA by UV radiation. *Lac* repressor (0.5 ng) was added to 50 ng of BrdU-DNA in 0.75 ml of buffer I adjusted to contain the indicated concentration of KCl. After 40 min to allow repressor to bind to operator, the samples were UV-irradiated at room temperature (25°) for the indicated times. IPTG was then added to a final concentration of 1 mM. After at least 10 min, 0.9 ml of buffer I containing 50 μg of sonicated salmon-sperm DNA was added, and 0.5-ml aliquots were filtered in triplicate through Millipore filters. DNA retention observed when UV irradiation preceded the addition of repressor (less than 5%) has been subtracted. (●——●), BrdU-λh80*dlac* [^{32}P]-DNA. (O- - -O), BrdU-λh80 [^{32}P]DNA. (△- - △), BrdU-λh80-*dlac* [^{32}P]DNA, 1 mM IPTG present *during* UV irradiation.

TABLE 1. *Effect of various reaction conditions on cross-linking of repressor to operator*

A		B	
Reaction condition	Percent control	Reaction condition	Percent control
Minus repressor	2	10^{-4} M IPTG	12
0°	26	10^{-3} M IPTG	1
25°	100	10^{-3} M methyl-β-D-thiogalactoside	10
37°	74	10^{-2} M melibiose	8
Minus dimethyl-sulfoxide	110	10^{-2} M lactose	131
0.01 M dithio-threitol	92	10^{-4} M phenyl-β-D-thiogalactoside	90
pH 7	75	10^{-4} M *o*-nitro-phenyl-β-D-fucoside	106
pH 8	84	10^{-2} M glucose	112
		10^{-2} M galactose	36

A. Repressor (2 ng) was added to 200 ng of BrdU-λh80*dlac* [^{32}P]DNA in 0.3 ml of buffer I, containing 0.18 M KCl and adjusted to the various conditions indicated. UV irradiation (10 min) and IPTG treatment were done as in the legend of Fig. 2. Before filtration the reaction mixture was diluted with 3.0 ml of buffer I containing 50 μg of sonicated salmon-sperm DNA. Samples (1 ml) were filtered in triplicate.

B. The basic procedure for these experiments is described in the legend of Fig. 2. Buffer I containing 0.18 M KCl and the indicated ligand was used. For each ligand, an experiment with no repressor present during UV irradiation was done to establish that the ligand alone caused no filter retention of DNA.

prepared identically to the BrdU-λh80*dlac* DNA (the phages were from a double lysogen and separated in CsCl) and had the same degree of BrdU substitution (90%) as measured by buoyant density. Sucrose gradient centrifugation experiments established that the molecular weights of the BrdU-λh80 and BrdU-λh80*dlac* DNAs were the same. Therefore, these data provide strong evidence for specific attachment of *lac* repressor to *lac* operator. Another argument for specificity will be developed below when the action of effector ligands is considered.

Nonspecific Attachment. In low salt no evidence for specific cross-linking to operator is seen. Fig. 2*C* shows that in 0.01 M KCl, IPTG-stable complexes form equally well with BrdU-λh80 and BrdU-λh80*dlac* DNA. Without UV treatment, filter retention only of BrdU-λh80*dlac* DNA is observed. We interpret these results as follows: The *lac* repressor does have measurable general affinity for DNA and this affinity for nonoperator DNA is much higher in low salt (7). Although the affinity of repressor for nonoperator DNA is much less than for operator, the effective concentration of nonoperator-binding sites is very high. In low salt, the probability of repressor being bound to BrdU-λh80 DNA is very high (see ref. 7, and note that the affinity of repressor for BrdU-substituted DNA is about 10 times greater than for unsubstituted DNA). Apparently this weakly bound repressor is not able to cause filter retention of the DNA. After UV treatment and the formation of a more stable complex, the DNA is retained on filters.

Effector Ligands. Many effector ligands, mostly galactosides, are known to interact with the *lac* repressor and affect its affinity for operator. Some are inducers and decrease bind-

TABLE 2. *Stability of repressor–DNA complexes formed during UV irradiation*

Treatment after UV	Ratio of treated to control: Nonoperator (λh80 DNA)	Ratio of treated to control: Operator (λh80*dlac* DNA)
10^{-3} M IPTG[a]	1	1
1 M KCl[b]	0.95	0.95
80°, 30 min[c]	1.04	0.33
0.2 N NaOH[d]	0.82	—[d]
Pronase[e]	0	0

The procedure through irradiation was as described in the legend of Fig. 2. For the experiments with nonoperator [^{32}P]-DNA (BrdU-λh80), buffer I was used. For experiments where binding was to operator, BrdU-λh80*dlac* [^{32}P]DNA was used, and the buffer contained 0.18 M KCl. After UV irradiation (7.5 min), various treatments were given before filtration.

[a] At least 10 min before filtration, IPTG was added to a final concentration of 10^{-3} M. The control received no IPTG.

[b] KCl was added to a final concentration of 1 M. After at least 20 min at 25°, 3 ml of buffer I containing 50 μg of salmon-sperm DNA was added and 1-ml samples were filtered. The control was with water added in place of the KCl solution.

[c] λh80 DNA was sonicated and 50 ng of repressor was used. After UV irradiation, 400 μg of BSA was added (to protect from adsorption to the walls of the test tube) and the reaction mixture heated at 80° for 30 min. The control was not heated. λh80*dlac* DNA was not sonicated and only 0.5 ng of repressor was used.

[d] When nonoperator binding was studied, λh80 DNA was sonicated and 50 ng of repressor was used. After UV irradiation, NaOH was added to a final concentration of 0.2 N. The solution was incubated at 25° for 10 min and then neutralized with HCl. For the control, NaCl was added instead of NaOH. When operator binding was studied, the λh80*dlac* DNA could not be sonicated and such high backgrounds (no repressor) were obtained after denaturation as to render the experiment meaningless. Experiments where the DNA was renatured overnight at 65° were also unsuccessful because of high backgrounds.

[e] Pronase (20 μg) was added and the reaction mixture incubated at 37° for 10 min. The control got no Pronase, but was incubated at 37° for 10 min.

ing affinity; others increase affinity and are known as anti-inducers (12). IPTG, an inducer, is known to cause slight conformational changes in the *lac* repressor (15–17). Under conditions where specific binding to BrdU-λh80*dlac* DNA is seen, the presence of IPTG during irradiation completely eliminates the formation of stable complex (Fig. 2A and Table 1). It was conceivable that IPTG was acting, not by causing a conformational change in the repressor, but rather in some nonspecific way, perhaps by reacting with the free radicals produced during UV irradiation. Therefore, we checked the effect of other galactosides. As illustrated in Table 1, only ligands known to inhibit repressor binding to operator are effective. Anti-inducers such as glucose, *o*-nitrophenylfucoside, and phenylthiogalactoside (12) do not inhibit stable complex formation. Lactose, a disaccharide which recently has been shown to be an anti-inducer (18), does not inhibit, whereas melibiose, a disaccharide that acts as an inducer (12), greatly reduces the formation of stable complexes. These results establish that the effect of these ligands is mediated through the *lac* repressor.

In contrast, Fig. 3 shows that in low salt, where nonspecific interactions predominate, the presence of IPTG before and

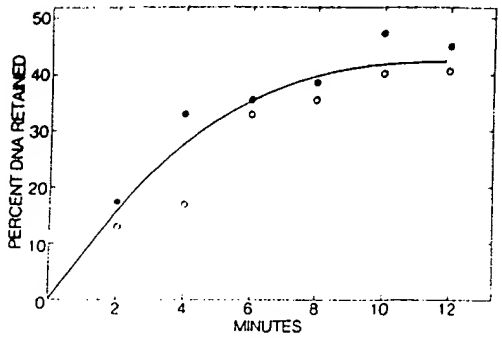


FIG. 3. The effect of IPTG on the photochemical attachment of *lac* repressor to wild-type BrdU-λh80 DNA. *Lac* repressor (1.0 ng) was added to 50 ng of BrdU-λh80 [^{32}P]DNA in 0.75 ml of buffer I. In one set of reaction mixtures, 1 mM IPTG was present. After 20 min at room temperature, the reaction mixtures were UV irradiated for the indicated times. To those samples with no ligand present during UV irradiation, IPTG was then added to a concentration of 1 mM. After an additional 10 min, 0.2-ml samples were filtered, in triplicate, through Millipore filters. (●——●) 1 mM IPTG present before and during UV treatment. (O- - -O) 1 mM IPTG added after UV treatment.

during irradiation does not affect the formation of stable complexes. This result is in keeping with our earlier observations that IPTG does not affect the binding of repressor to nonoperator DNA (7). Apparently, the conformational changes induced in the repressor by galactosides only affect binding to operator. Since in 0.18 M KCl, IPTG does eliminate stable complex formation, it follows that, under these conditions, attachment is to the *lac* operator.

Chemistry and Efficiency of Attachment. Markovitz found that UV irradiation induces the formation of DNA polymerase–DNA complexes that are resistant to high salt, phenol, heat, and 0.1 M NaOH (3); he concluded that a covalent bond between DNA and protein had been established. Photoinduced protein–DNA complexes also are known to be resistant to SDS (2, 25). Under conditions where repressor is binding nonspecifically to BrdU-substituted DNA, we have obtained similar results (Table 2). The complexes also are stable to SDS (Table 3). These results strongly suggest that UV treatment covalently attaches repressor to DNA.

There is no reason to think that the mechanism of photochemical attachment of repressor to operator DNA is fundamentally different from attachment to nonoperator DNA. However, experiments to establish this point have proven more difficult, because under conditions where specific attachment of repressor to operator occurs, only one repressor protein is bound for each BrdU-λh80*dlac* DNA molecule (30×10^6 molecular weight). The filter assay requires that this protein cause the DNA to be retained on the nitrocellulose filters. Experiments where strand separation occurs (0.2 M NaOH and boiling temperatures) have not been successful. UV irradiation is known to introduce single strand breaks in BrdU-DNA, so after strand separation, the majority of DNA fragments would not be expected to have repressor peptides attached. Treatment at 80° causes a drop in DNA filter retention to a value about one-third that of the control. A denatured subunit attached to DNA may not be as effective in causing the DNA to be retained on the filters as the native tetramer. Although the above experiments were ambiguous, others were more definitive. The data in Table 3 provide

TABLE 3. *SDS and salt stability of photoinduced repressor–DNA complexes*

Reaction condition	DNA	Percent DNA in nonaqueous phase: No UV	Percent DNA in nonaqueous phase: + UV
Nonspecific (0.01 M KCl)	λh80	0.8	62
Specific (0.18 M KCl)	λh80*dlac*	0.3	1.4
		0.5	8.2

For the experiment under nonspecific conditions, 200 ng of repressor was mixed with 400 ng of BrdU-λh80 [^{32}P]DNA in 1.5 ml of buffer I without dimethylsulfoxide. After 10 min of UV treatment, a modification of the procedure of Smets and Cornelis (25) was applied. BSA, SDS, and NaCl were added to a final concentration of 70 μg/ml, 0.2%, and 1 M, respectively; then an equal volume of $CHCl_3$:isoamyl alcohol (12:1) was added and the mixture gently shaken at 25° for 10 min. The water phase and $CHCl_3$ phase were separated and counted. The interphase was collected by filtration through Whatman GF/C glass filters. Before counting, the filters were washed with 1 N HCl containing 0.05 M sodium pyrophosphate, and then with ethanol. For the experiments under specific conditions, the same procedure was followed, except that only 8 ng of repressor was used and buffer I contained 0.18 M KCl.

strong evidence for SDS-stable cross-linking of repressor to operator. UV irradiation in the presence of repressor increases more than 10-fold the amount of DNA trapped in $CHCl_3$ and the protein–SDS interphase. Most important is the complete resistance of the photochemical complexes to high salt and inducer concentrations (agents that would quickly and completely eliminate normal repressor–operator complexes). Therefore, we think that photochemical attachment to operator occurs as it does to nonoperator DNA with the formation of extremely stable and probably covalent bonds.

Before UV irraidation, repressor causes a maximum of about 40% of BrdU-λh80*dlac* DNA to be retained on filters (Fig. 1). Fig. 2 shows that after UV irradiation and the formation of IPTG-resistant complexes, a maximum of about 20% of the DNA is retained. Therefore, from the data shown, it is apparent that the efficiency of complex formation is at least 50%. After 7.5 min. of UV treatment, we estimate that the sample has received a dose of 8×10^3 ergs/mm^2. Markovitz found that about 50×10^3 ergs/mm^2 was necessary to covalently attach DNA polymerase to poly(dA-dT) or normal *Escherichia coli* DNA (3). The difference in energy is in keeping with the increased sensitivity of BrdU-DNA to UV irradiation (2, 20).

As illustrated by the data shown in Table 1, the photochemical attachment of repressor to operator is much less at 0° than at 25°. This result has been obtained reproducibly and can only be partially compensated for by longer irradiation times. At 37°, background (no repressor) becomes higher and more variable. To obtain reproducible results, BSA must be present, presumably to protect repressor. However, the BSA must be heat treated (see below). Dimethylsulfoxide is not essential and can be eliminated. High concentrations of dithiothreitol do not interfere with photochemical attachment to operator.

Lac repressor binds strongly to poly(dA-dT) (7), and even more tightly to poly(dA-BrdU) (21). However, we found that

TABLE 4. *Photochemical attachment of the catabolite gene activator protein to BrdU-DNA*

Ligand	Exp. no.	Percent DNA retained: No UV, Treatment before filtering: None	No UV: KCl (1 M)	+ UV: None	+ UV: KCl (1 M)	+ UV: cGMP (3 mM)
None	1	10	0	64	60	—
	2	19	0	42	41	39
cAMP 0.3 mM	1	71	1	53	38	—
	2	45	1	44	26	29
cGMP 0.3 mM	1	—	—	—	—	—
	2	6	0	7	4	3

The reaction mixture contained the indicated ligand and 0.1 μg of BrdU-λh80*dlac* [^{32}P]DNA in 0.7 ml of buffer I. Enough CAP was added to cause 90% of the DNA to be retained on filters under our standard (no UV) condition (23). UV irradiation was for 10 min at 25° at a distance of 11 cm. After UV treatment, either KCl (1 M) or 3′:5′-cyclic GMP (3 mM) was added and the mixture was incubated at 25° for 20 min. Sonicated salmon-sperm DNA (50 μg) was added and then 2.5 ml of buffer I was added, and 1-ml samples were filtered in triplicate. In the case of no treatment before filtering, KCl or cGMP was omitted. Controls without CAP were done and subtracted as background. Neither cyclic AMP or cyclic GMP affected the background.

the photochemical attachment of repressor to poly(dA-BrdU) required higher UV doses than attachment to operator or to sonicated BrdU-λh80 DNA. A UV dose of about 50×10^3 ergs/mm^2 was required for 50% retention of [^{3}H]poly(dA-BrdU)–repressor complex on filters. Smith has observed that the rate of photochemical addition of [^{35}S]cysteine to poly(dA-dT) is considerably less than to calf-thymus DNA (19).

Photochemical attachment of repressor to normal λh80*dlac* DNA has not been successful. Initial experiments were done with intact λh80*dlac* DNA (30×10^6 daltons). Later we prepared DNA fragments of about 1×10^6 daltons, each of which contained the *lac* operator (22). With these operator enriched fragments, even 60×10^3 ergs/mm^2 gave no IPTG-resistant complexes.

Other Proteins. In this laboratory, we have studied the DNA binding properties of another regulatory protein, the catabolite gene activator protein (CAP, CR, or CGA protein) (23). The DNA-binding activity of CAP is stimulated by cAMP, but is eliminated by cGMP or by high salt (Table 4 and refs. 23 and 24). Binding specificity has not been demonstrated (23, 24). As shown in Table 4, UV treatment leads to the formation of a CAP–DNA complex that is stable to high salt and cGMP.

We also have confirmed that UV treatment will cause DNA polymerase and RNA polymerase to form salt resistant complexes with BrdU-DNA. All four DNA-binding proteins are effective in causing DNA filter retention at concentrations of 0.01 μg/ml or less (with or without covalent attachment). Other non-DNA-binding proteins (trypsin, ovalbumin, and BSA) will cause filter retention after UV treatment, but at least one 100-fold higher concentrations are needed (1 μg/ml or more). At 50 μg/ml, even BSA will cause filter retention unless it is heat treated (see *Methods*).

DISCUSSION

Markovitz (3) has shown that UV radiation covalently attaches DNA polymerase to poly(dA-dT) and to normal *E. coli* DNA. UV irradiation of BrdU-substituted DNA leads to debromination and the consequent production of highly reactive uracilyl radicals (2, 20). Therefore, it is reasonable to think that protein bound to DNA would be more readily attached to BrdU-DNA than to normal DNA. Smith (2) and Smets and Cornelis (25) have shown, in fact, that UV treatment of cells with BrdU-substituted DNA decreases the amount of DNA that can be extracted. They interpreted this as due to the formation of protein-DNA cross-links. After this paper was in preparation, we learned that Weintraub (26) has also recently obtained evidence for the cross-linking of proteins to BrdU-substituted DNA. He has found that a variety of proteins, including histones and RNA polymerase, can be attached to BrdU-substituted DNA from mammalian cells. If specific attachment occurs, involving the correct sites on the DNA and on the protein, then UV-induced cross-linking promises to be a very useful tool. However, in none of these studies was any evidence obtained for specific attachment.

We report here that the *lac* repressor can be photochemically attached to BrdU-substituted DNA and that in high salt (0.18 M KCl) the reaction is specific for *lac* operator, i.e., attachment occurs to BrdU-λh80*dlac* DNA but not to BrdU-λh80 DNA. Inducers of the *lac* operon (i.e., IPTG) prevent photochemical attachment of repressor to operator if they are present during UV irradiation, but not if added later. In low salt (0.01 M KCl), specificity is not observed; cross-linking occurs to BrdU-λh80 DNA as well as to BrdU-λh80-*dlac*, and IPTG has no effect. By analogy to previous work and from the stability of the repressor–DNA photoproduct we think that covalent bonds are formed.

We find BrdU-substitution to be essential; no attachment to normal λh80*dlac* is obtained even with much higher UV doses. There are large differences between normal and BrdU-substituted DNA in the types and numbers of photoproducts (20). These differences may be critical for the attachment of of sequence specific proteins. BrdU-substituted DNA may be advantageous, not only because of its greater photochemical reactivity, but also because the *lac* repressor binds tighter to BrdU-substituted DNA (8).

Cysteine adds photochemically to DNA (19) and Smith has shown that cysteine reacts with uracil to form 5-*S*-cysteine-6-hydrouracil (27) or with thymine to form 5-*S*-cysteine-6-hydrothymine (28). Eleven other amino acids photochemically add to uracil with cysteine, phenylalanine, tyrosine, histidine, lysine, and arginine being the most reactive (28). Polylysine also has been cross-linked by UV radiation to DNA (26). Since many amino acids can react, it seems likely that most DNA-binding proteins will be cross-linked by UV irradiation. We find that another DNA-binding regulatory protein, the catabolite gene activator protein (23, 24), also can be attached stably to DNA. We also have confirmed (26) that RNA polymerase can be cross-linked to BrdU-DNA.

Specific covalent attachment of DNA-binding proteins to their DNA substrate is obviously of great potential usefulness for identification of the DNA-binding sites of proteins and possibly in the isolation of the DNA region covered by the proteins. For mammalian cells especially, it may be useful to attach covalently chromosomal proteins to their specific sites by UV irradiation prior to disruption of the cell or nucleus. Perhaps less obvious is that covalent attachment may be useful for the *demonstration* of specific binding, which often is a major problem with DNA-binding proteins. For many proteins, binding specificity may be greatest in high salt. However, in high salt, DNA–protein complexes are detectable in sucrose gradients only if impracticably high concentrations of reactants are used; and the same is true for retention on nitrocellulose filters. By the methods described here, it is now possible to fix permanently the protein to DNA under conditions of maximum specificity.

We are grateful for the excellent technical assistance of D. Lin, J. Roberts, and K. Alchian. This work was supported by grants from the National Institutes of Health (HD-04420) and the National Science Foundation (GB-26517).

1. Smith, K. C. (1962) *Biochem. Biophys. Res. Commun.* 8, 157–163.
2. Smith, K. C. & Hanawalt, P. C. (1969) *Molecular Photobiology: Inactivation and Recovery* (Academic Press, New York and London), pp. 57–84.
3. Markovitz, A. (1972) *Biochim. Biophys. Acta* 281, 522–534.
4. Müller-Hill, B., Beyreuther, K. & Gilbert, W. (1971) *Methods in Enzymology*, eds. Grossman, L & Moldave, K. (Academic Press, New York), Vol. 21, pt. D, pp. 483–487.
5. Gilbert, W. & Müller-Hill, B. (1966) *Proc. Nat. Acad. Sci. USA* 56, 1891–1898.
6. Riggs, A. D., Suzuki, H. & Bourgeois, S. (1970) *J. Mol. Biol.* 48, 67–83.
7. Lin, S. & Riggs, A. D. (1972) *J. Mol. Biol.* 72, 671–690.
8. Lin, S. & Riggs, A. D. (1972) *Proc. Nat. Acad. Sci. USA* 69, 2574–2576.
9. Hackett, P. & Hanawalt, P. (1966) *Biochim. Biophys. Acta* 123, 356–363.
10. Gilbert, W. & Müller-Hill, B. (1967) *Proc Nat. Acad Sci. USA* 58, 2415–2421.
11. Riggs, D. D., Bourgeois, S., Newby, R. F. & Cohn, M. (1968) *J. Mol. Biol.* 34, 365–368.
12. Riggs, A. D., Newby, R. F. & Bourgeois, S. (1970) *J. Mol. Biol.* 51, 303–314.
13. Riggs, A. D., Bourgeois, S. & Cohn, M. (1970) *J. Mol. Biol.* 53, 401–417.
14. Jobe, A., Riggs, A. D. & Bourgeois, S. (1972) *J. Mol. Biol.* 64, 181–199.
15. Matthews, K. S., Matthews, H. R., Thielmann, H. W. & Jardetzky, O. (1973) *Biochim. Biophys. Acta* 295, 159–165.
16. Oshima, Y., Matsuura, M. & Horiuchi, T. (1972) *Biochem. Biophys. Res. Commun.* 47, 1444–1449.
17. Laiken, S. L., Gross, C. A. & von Hippel, P. H. (1972) *J. Mol. Biol.* 66, 143–155.
18. Jobe, A. & Bourgeois, S. (1973) *J. Mol. Biol.* 75, 303–313.
19. Smith, K. C. & Meun, D. H. C. (1968) *Biochemistry* 7, 1033–1037.
20. Setlow, R. B. & Setlow, J. K. (1972) *Annu. Rev. Biophys. Bioeng.* 1, 293–346.
21. Lin, S. & Riggs, A. D. (1971) *Biochem. Biophys. Res. Commun.* 45, 1542–1547.
22. Bourgeois, S. & Riggs, A. D. (1970) *Biochem. Biophys. Res. Commun.* 38, 348–354.
23. Riggs, A. D., Reiness, G. & Zubay, G. (1971) *Proc. Nat. Acad. Sci. USA* 68, 1222–1225.
24. Nissley, P., Anderson, W. B., Gallo, M. & Pastan, I. (1972) *J. Biol. Chem.* 247, 4264–4269.
25. Smets, L. A. & Cornelis, J. J. (1971) *Int. J. Radiat. Biol.* 19, 445–457.
26. Weintraub, H. (1973) *Cold Spring Harbor Symp. Quant. Biol.* 38, in press.
27. Smith, K. C. & Aplin, R. T. (1966) *Biochemistry* 5, 2125–2130.
28. Smith, K. C. (1969) *Biochem. Biophys. Res. Commun.* 34, 354–357.

Proc. Nat. Acad. Sci.
Vol. 71, No. 3, pp. 947–951, March 1974

Photochemical Attachment of *lac* Repressor to Bromodeoxyuridine-Substituted *lac* Operator by Ultraviolet Radiation

(catabolite gene activator protein/protein–DNA interaction/nitrocellulose-filter assay)

SYR-YAUNG LIN AND ARTHUR D. RIGGS

City of Hope National Medical Center, Duarte, California 91010

Communicated by Matthew Meselson, October 27, 1973

ABSTRACT **The transducing phage λh80*dlac* carries the *lac* operator, whereas wild-type λh80 does not. We find that in high salt (0.18 M KCl), ultraviolet radiation causes the formation of a very stable complex between repressor and 5-bromodeoxyuridine (BrdU)-substituted λh80*dlac* but not to BrdU-λh80 DNA. Studies with inducers of the *lac* operon confirm the specificity of attachment. In low salt (0.01 M KCl), ultraviolet radiation will also attach repressor nonspecifically to BrdU-λh80 DNA. The stability of the complex suggests that covalent bonds are formed. We also report that another regulatory protein, the catabolite gene activator protein, can be attached similarly to DNA.**

Smith first noted that ultraviolet (UV) radiation cross-links protein to DNA, both *in vivo* and *in vitro* (1). The experimental evidence for cross-linking was that after UV treatment, DNA was not extractable from sodium dodecyl sulfate (SDS)–protein precipitates. This work has been reviewed (2). Proteins known to bind to DNA were not studied. Recently, Markovitz (3) demonstrated that UV irradiation results in covalent bond formation between DNA polymerase and DNA. Stimulated by the work of Markovitz, we tried to demonstrate the specific cross-linking of *lac* repressor to *lac* operator in λh80*dlac* DNA. These experiments were not successful until 5-bromodeoxyuridine (BrdU)-substituted λh80*dlac* DNA was used. We report here the photochemical attachment of *lac* repressor specifically to BrdU-substituted *lac* operator.

METHODS

We prepared *lac* repressor (i^{superq}) from strain M96 following the procedure of Müller-Hill, Beyreuther, and Gilbert (4). To ensure purity, additional chromatography on DEAE-Sephadex was done (5). The preparation was free of impurities detectable by SDS–acrylamide gel electrophoresis and all DNA-binding activity (including photochemical cross-linking) sedimented in a sucrose gradient as *lac* repressor. The nitrocellulose filter assay for repressor–DNA complexes has been described in detail (6, 7). Because of somewhat lower background and better reproducibility, we are now using type HAMK filters from the Millipore Corp. The basic procedures for preparing BrdU-substituted λh80*dlac* [^{32}P]DNA and λh80 [^{32}P]DNA are published (8). For this work the thymine-requiring double lysogen, JG108 ($\lambda h_{80}C_{I857}S_{c68}dlac$, $\lambda h_{80}C_{I857}S_{c68}$), was grown in medium containing 10 μg/ml of BrdU and 0.2 μg/ml of thymidine for 30 min prior to heat induction. This procedure leads to about 90% substitution BrdU for thymidine as estimated by buoyant density measurements in CsCl (9).

For most experiments, ultraviolet light treatment was at distance of 11 cm from a short wavelength mineral light (Ultraviolet Products, model UVS-11). The sample (0.75 m was in 0.5 × 2-inch polyallomer tubes situated directly below the UV lamp. Irradiation was usually done at room temperature (25°) in buffer I, which contains: 10 mM KCl, 10 mM Tris·HCl (pH 7.4), 0.1 mM EDTA, 0.1 mM dithiothreitol 5% (v/v) dimethylsulfoxide, and 50 μg/ml of BSA. The BSA was heat treated at 70° for 2 hr at pH 9.0. UV dosage was measured with an ultraviolet meter (Ultraviolet Products, model J-225). Test tubes with the bottom cut out were used to estimate the dose actually received by the sample.

RESULTS

The specific binding of *lac* repressor to *lac* operator has been firmly established (10, 11) and studied in detail using nitrocellulose filters to asay for repressor-operator complex (6, 12–14). Repressor binding to operator is eliminated by isopropyl-β-D-thiogalactoside (IPTG), a good inducer of the *lac* operon. IPTG at 10^{-3} M causes preformed repressor–operator complexes to dissociate in a few seconds, even in low ionic strength buffers (ref. 13, and our unpublished data). The binding of repressor to operator is also very sensitive to salt concentration and preformed repressor–operator complexes dissociate quickly in high salt (13). *Lac* repressor has a relatively weak, but nonetheless measurable, affinity for DNA not containing the *lac* operator (7). Repressor binding to nonoperator DNA is sensitive to ionic strength, but is not affected by IPTG (7).

The results above were obtained using normal, unsubstituted DNA. However, as shown in Fig. 1, the binding of repressor to BrdU-substituted DNA is basically similar. Specificity for operator is easily demonstrated because IPTG eliminates the binding (Fig. 1 and ref. 8) and no binding is observed if DNA without the *lac* operon (BrdU-λh80 [^{32}P]-DNA) is used (data not shown). An important difference between normal and BrdU-substituted operator is that the rate of dissociation of *lac* repressor is ten times slower from the latter (8). Recent work (Lin and Riggs, unpublished) has established that the equilibrium affinity of *lac* repressor for both operator and nonoperator BrdU-substituted DNA is increased about one order of magnitude.

Specific attachment. Fig. 2A shows that, in 0.18 M KCl, UV irradiation leads to the formation of IPTG-resistant complexes between repressor and BrdU-λh80*dlac* DNA. The zero

Abbreviations: BSA, bovine-serum albumin; BrdU, 5-bromodeoxyuridine; CAP, catabolite gene activator protein; IPTG, isopropyl-β-D-thiogalactoside; SDS, sodium dodecyl sulfate; UV, ultraviolet.

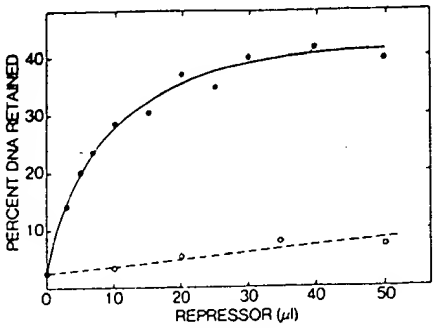


FIG. 1. Binding of *lac* repressor to BrdU-substituted λh80-*dlac* [^{32}P]DNA. Various amounts of repressor were added to 0.4 ml of buffer I, containing 25 ng of BrdU-substituted λh80-*dlac* [^{32}P]DNA. The reaction mixtures were incubated at room temperature for at least 30 min before filtration on Millipore filters. In some tubes, IPTG was added to a final concentration of 10^{-3} M before adding repressor. Each point is the average of three filters. ●——●, without IPTG. O- - -O, IPTG added to a final concentration of 1 mM before adding repressor.

time point serves as a control to establish that without UV irradiation, IPTG completely eliminates repressor–operator complexes. Repressor must be present during irradiation; prior irradiation of the DNA does not lead to stable complex formation. Under these conditions, no stable complex is formed with BrdU-λh80 DNA. The BrdU-λh80 DNA was

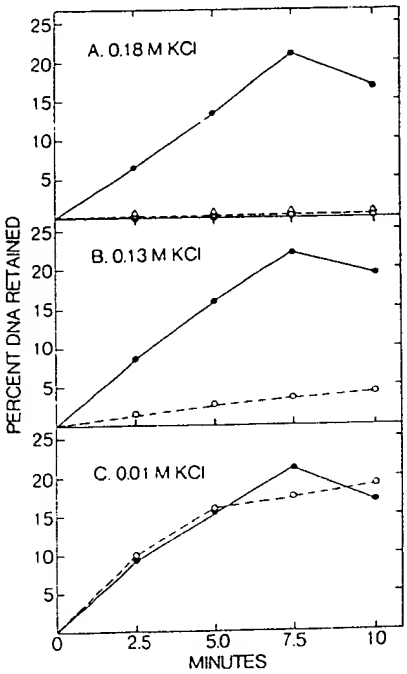


FIG. 2. Formation of IPTG-stable complexes between *lac* repressor and BrdU-DNA by UV radiation. *Lac* repressor (0.5 ng) was added to 50 ng of BrdU-DNA in 0.75 ml of buffer I adjusted to contain the indicated concentration of KCl. After 40 min to allow repressor to bind to operator, the samples were UV-irradiated at room temperature (25°) for the indicated times. IPTG was then added to a final concentration of 1 mM. After at least 10 min, 0.9 ml of buffer I containing 50 μg of sonicated salmon-sperm DNA was added, and 0.5-ml aliquots were filtered in triplicate through Millipore filters. DNA retention observed when UV irradiation preceded the addition of repressor (less than 5%) has been subtracted. (●——●), BrdU-λh80*dlac* [^{32}P]-DNA. (O- - -O), BrdU-λh80 [^{32}P]DNA. (Δ- - -Δ), BrdU-λh80-*dlac* [^{32}P]DNA, 1 mM IPTG present *during* UV irradiation.

TABLE 1. *Effect of various reaction conditions on cross-linking of repressor to operator*

A		B	
Reaction condition	Percent control	Reaction condition	Percent control
Minus repressor	2	10^{-1} M IPTG	12
0°	26	10^{-2} M IPTG	1
25°	100	10^{-3} M methyl-β-D-thiogalactoside	10
37°	74	10^{-2} M melibiose	8
Minus dimethylsulfoxide	110	10^{-2} M lactose	131
0.01 M dithiothreitol	92	10^{-4} M phenyl-β-D-thiogalactoside	90
pH 7	75	10^{-4} M o-nitrophenyl-β-D-fucoside	106
pH 8	84	10^{-2} M glucose	112
		10^{-2} M galactose	36

A. Repressor (2 ng) was added to 200 ng of BrdU-λh80*dlac* [^{32}P]DNA in 0.3 ml of buffer I, containing 0.18 M KCl and adjusted to the various conditions indicated. UV irradiation (10 min) and IPTG treatment were done as in the legend of Fig. 2. Before filtration the reaction mixture was diluted with 3.0 ml of buffer I containing 50 μg of sonicated salmon-sperm DNA. Samples (1 ml) were filtered in triplicate.

B. The basic procedure for these experiments is described in the legend of Fig. 2. Buffer I containing 0.18 M KCl and the indicated ligand was used. For each ligand, an experiment with no repressor present during UV irradiation was done to establish that the ligand alone caused no filter retention of DNA.

prepared identically to the BrdU-λh80*dlac* DNA (the phages were from a double lysogen and separated in CsCl) and had the same degree of BrdU substitution (90%) as measured by buoyant density. Sucrose gradient centrifugation experiments established that the molecular weights of the BrdU-λh80 and BrdU-λh80*dlac* DNAs were the same. Therefore, these data provide strong evidence for specific attachment of *lac* repressor to *lac* operator. Another argument for specificity will be developed below when the action of effector ligands is considered.

Nonspecific Attachment. In low salt no evidence for specific cross-linking to operator is seen. Fig. 2*C* shows that in 0.01 M KCl, IPTG-stable complexes form equally well with BrdU-λh80 and BrdU-λh80*dlac* DNA. Without UV treatment, filter retention only of BrdU-λh80*dlac* DNA is observed. We interpret these results as follows: The *lac* repressor does have measurable general affinity for DNA and this affinity for nonoperator DNA is much higher in low salt (7). Although the affinity of repressor for nonoperator DNA is much less than for operator, the effective concentration of nonoperator-binding sites is very high. In low salt, the probability of repressor being bound to BrdU-λh80 DNA is very high (see ref. 7, and note that the affinity of repressor for BrdU-substituted DNA is about 10 times greater than for unsubstituted DNA). Apparently this weakly bound repressor is not able to cause filter retention of the DNA. After UV treatment and the formation of a more stable complex, the DNA is retained on filters.

Effector Ligands. Many effector ligands, mostly galactosides, are known to interact with the *lac* repressor and affect its affinity for operator. Some are inducers and decrease bind-

TABLE 2. *Stability of repressor-DNA complexes formed during UV irradiation*

Treatment after UV	Ratio of treated to control	
	Nonoperator (λh80 DNA)	Operator (λh80*dlac* DNA)
10^{-3} M IPTG[a]	1	1
1 M KCl[b]	0.95	0.95
80°, 30 min[c]	1.04	0.33
0.2 N NaOH[d]	0.82	—[d]
Pronase[e]	0	0

The procedure through irradiation was as described in the legend of Fig. 2. For the experiments with nonoperator [^{32}P]-DNA (BrdU-λh80), buffer I was used. For experiments where binding was to operator, BrdU-λh80*dlac* [^{32}P]DNA was used, and the buffer contained 0.18 M KCl. After UV irradiation (7.5 min), various treatments were given before filtration.

[a] At least 10 min before filtration, IPTG was added to a final concentration of 10^{-3} M. The control received no IPTG.

[b] KCl was added to a final concentration of 1 M. After at least 20 min at 25°, 3 ml of buffer I containing 50 μg of salmon-sperm DNA was added and 1-ml samples were filtered. The control was with water added in place of the KCl solution.

[c] λh80 DNA was sonicated and 50 ng of repressor was used. After UV irradiation, 400 μg of BSA was added (to protect from adsorption to the walls of the test tube) and the reaction mixture heated at 80° for 30 min. The control was not heated. λh80*dlac* DNA was not sonicated and only 0.5 ng of repressor was used.

[d] When nonoperator binding was studied, λh80 DNA was sonicated and 50 ng of repressor was used. After UV irradiation, NaOH was added to a final concentration of 0.2 N. The solution was incubated at 25° for 10 min and then neutralized with HCl. For the control, NaCl was added instead of NaOH. When operator binding was studied, the λh80*dlac* DNA could not be sonicated and such high backgrounds (no repressor) were obtained after denaturation as to render the experiment meaningless. Experiments where the DNA was renatured overnight at 65° were also unsuccessful because of high backgrounds.

[e] Pronase (20 μg) was added and the reaction mixture incubated at 37° for 10 min. The control got no Pronase, but was incubated at 37° for 10 min.

ing affinity; others increase affinity and are known as anti-inducers (12). IPTG, an inducer, is known to cause slight conformational changes in the *lac* repressor (15–17). Under conditions where specific binding to BrdU-λh80*dlac* DNA is seen, the presence of IPTG during irradiation completely eliminates the formation of stable complex (Fig. 2A and Table 1). It was conceivable that IPTG was acting, not by causing a conformational change in the repressor, but rather in some nonspecific way, perhaps by reacting with the free radicals produced during UV irradiation. Therefore, we checked the effect of other galactosides. As illustrated in Table 1, only ligands known to inhibit repressor binding to operator are effective. Anti-inducers such as glucose, *o*-nitrophenylfucoside, and phenylthiogalactoside (12) do not inhibit stable complex formation. Lactose, a disaccharide which recently has been shown to be an anti-inducer (18), does not inhibit, whereas melibiose, a disaccharide that acts as an inducer (12), greatly reduces the formation of stable complexes. These results establish that the effect of these ligands is mediated through the *lac* repressor.

In contrast, Fig. 3 shows that in low salt, where nonspecific interactions predominate, the presence of IPTG before and

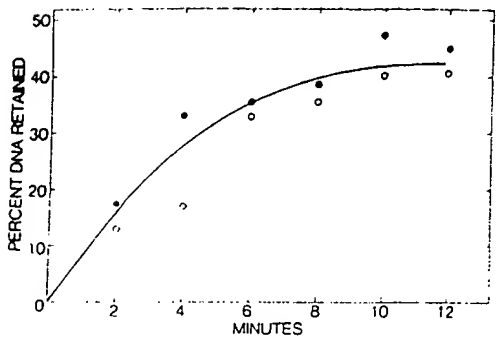


FIG. 3. The effect of IPTG on the photochemical attachment of *lac* repressor to wild-type BrdU-λh80 DNA. *Lac* repressor (1.0 ng) was added to 50 ng of BrdU-λh80 [^{32}P]DNA in 0.75 ml of buffer I. In one set of reaction mixtures, 1 mM IPTG was present. After 20 min at room temperature, the reaction mixtures were UV irradiated for the indicated times. To those samples with no ligand present during UV irradiation, IPTG was then added to a concentration of 1 mM. After an additional 10 min, 0.2-ml samples were filtered, in triplicate, through Millipore filters. (●——●) 1 mM IPTG present before and during UV treatment. (O- - -O) 1 mM IPTG added after UV treatment.

during irradiation does not affect the formation of stable complexes. This result is in keeping with our earlier observations that IPTG does not affect the binding of repressor to nonoperator DNA (7). Apparently, the conformational changes induced in the repressor by galactosides only affect binding to operator. Since in 0.18 M KCl, IPTG does eliminate stable complex formation, it follows that, under these conditions, attachment is to the *lac* operator.

Chemistry and Efficiency of Attachment. Markovitz found that UV irradiation induces the formation of DNA polymerase–DNA complexes that are resistant to high salt, phenol, heat, and 0.1 M NaOH (3); he concluded that a covalent bond between DNA and protein had been established. Photoinduced protein–DNA complexes also are known to be resistant to SDS (2, 25). Under conditions where repressor is binding nonspecifically to BrdU-substituted DNA, we have obtained similar results (Table 2). The complexes also are stable to SDS (Table 3). These results strongly suggest that UV treatment covalently attaches repressor to DNA.

There is no reason to think that the mechanism of photochemical attachment of repressor to operator DNA is fundamentally different from attachment to nonoperator DNA. However, experiments to establish this point have proven more difficult, because under conditions where specific attachment of repressor to operator occurs, only one repressor protein is bound for each BrdU-λh80*dlac* DNA molecule (30×10^6 molecular weight). The filter assay requires that this protein cause the DNA to be retained on the nitrocellulose filters. Experiments where strand separation occurs (0.2 M NaOH and boiling temperatures) have not been successful. UV irradiation is known to introduce single strand breaks in BrdU-DNA, so after strand separation, the majority of DNA fragments would not be expected to have repressor peptides attached. Treatment at 80° causes a drop in DNA filter retention to a value about one-third that of the control. A denatured subunit attached to DNA may not be as effective in causing the DNA to be retained on the filters as the native tetramer. Although the above experiments were ambiguous, others were more definitive. The data in Table 3 provide

TABLE 3. *SDS and salt stability of photoinduced repressor–DNA complexes*

Reaction condition	DNA	Percent DNA in nonaqueous phase: No UV	Percent DNA in nonaqueous phase: + UV
Nonspecific (0.01 M KCl)	λh80	0.8	62
Specific (0.18 M KCl)	λh80	0.3	1.4
	λh80*dlac*	0.5	8.2

For the experiment under nonspecific conditions, 200 ng of repressor was mixed with 400 ng of BrdU-λh80 [^{32}P]DNA in 1.5 ml of buffer I without dimethylsulfoxide. After 10 min of UV treatment, a modification of the procedure of Smets and Cornelis (25) was applied. BSA, SDS, and NaCl were added to a final concentration of 70 μg/ml, 0.2%, and 1 M, respectively; then an equal volume of $CHCl_3$:isoamyl alcohol (12:1) was added and the mixture gently shaken at 25° for 10 min. The water phase and $CHCl_3$ phase were separated and counted. The interphase was collected by filtration through Whatman GF/C glass filters. Before counting, the filters were washed with 1 N HCl containing 0.05 M sodium pyrophosphate, and then with ethanol. For the experiments under specific conditions, the same procedure was followed, except that only 8 ng of repressor was used and buffer I contained 0.18 M KCl.

strong evidence for SDS-stable cross-linking of repressor to operator. UV irradiation in the presence of repressor increases more than 10-fold the amount of DNA trapped in $CHCl_3$ and the protein–SDS interphase. Most important is the complete resistance of the photochemical complexes to high salt and inducer concentrations (agents that would quickly and completely eliminate normal repressor–operator complexes). Therefore, we think that photochemical attachment to operator occurs as it does to nonoperator DNA with the formation of extremely stable and probably covalent bonds.

Before UV irraidation, repressor causes a maximum of about 40% of BrdU-λh80*dlac* DNA to be retained on filters (Fig. 1). Fig. 2 shows that after UV irradiation and the formation of IPTG-resistant complexes, a maximum of about 20% of the DNA is retained. Therefore, from the data shown, it is apparent that the efficiency of complex formation is at least 50%. After 7.5 min. of UV treatment, we estimate that the sample has received a dose of 8×10^3 ergs/mm^2. Markovitz found that about 50×10^3 ergs/mm^2 was necessary to covalently attach DNA polymerase to poly(dA-dT) or normal *Escherichia coli* DNA (3). The difference in energy is in keeping with the increased sensitivity of BrdU-DNA to UV irradiation (2, 20).

As illustrated by the data shown in Table 1, the photochemical attachment of repressor to operator is much less at 0° than at 25°. This result has been obtained reproducibly and can only be partially compensated for by longer irradiation times. At 37°, background (no repressor) becomes higher and more variable. To obtain reproducible results, BSA must be present, presumably to protect repressor. However, the BSA must be heat treated (see below). Dimethylsulfoxide is not essential and can be eliminated. High concentrations of dithiothreitol do not interfere with photochemical attachment to operator.

Lac repressor binds strongly to poly(dA-dT) (7), and even more tightly to poly(dA-BrdU) (21). However, we found that

TABLE 4. *Photochemical attachment of the catabolite gene activator protein to BrdU-DNA*

Ligand	Exp. no.	Percent DNA retained: No UV; Treatment before filtering: None	No UV: KCl (1 M)	+ UV: None	+ UV: KCl (1 M)	+ UV: cGMP (3 mM)
None	1	10	0	64	60	—
	2	19	0	42	41	39
cAMP 0.3 mM	1	71	1	53	38	—
	2	45	1	44	26	29
cGMP 0.3 mM	1	—	—	—	—	—
	2	6	0	7	4	3

The reaction mixture contained the indicated ligand and 0.1 μg of BrdU-λh80*dlac* [^{32}P]DNA in 0.7 ml of buffer I. Enough CAP was added to cause 90% of the DNA to be retained on filters under our standard (no UV) condition (23). UV irradiation was for 10 min at 25° at a distance of 11 cm. After UV treatment, either KCl (1 M) or 3′:5′-cyclic GMP (3 mM) was added and the mixture was incubated at 25° for 20 min. Sonicated salmon-sperm DNA (50 μg) was added and then 2.5 ml of buffer I was added, and 1-ml samples were filtered in triplicate. In the case of no treatment before filtering, KCl or cGMP was omitted. Controls without CAP were done and subtracted as background. Neither cyclic AMP or cyclic GMP affected the background.

the photochemical attachment of repressor to poly(dA-BrdU) required higher UV doses than attachment to operator or to sonicated BrdU-λh80 DNA. A UV dose of about 50×10^3 ergs/mm^2 was required for 50% retention of [^{3}H]poly-(dA-BrdU)–repressor complex on filters. Smith has observed that the rate of photochemical addition of [^{35}S]cysteine to poly(dA-dT) is considerably less than to calf-thymus DNA (19).

Photochemical attachment of repressor to normal λh80-*dlac* DNA has not been successful. Initial experiments were done with intact λh80*dlac* DNA (30×10^6 daltons). Later we prepared DNA fragments of about 1×10^6 daltons, each of which contained the *lac* operator (22). With these operator enriched fragments, even 60×10^3 ergs/mm^2 gave no IPTG-resistant complexes.

Other Proteins. In this laboratory, we have studied the DNA binding properties of another regulatory protein, the catabolite gene activator protein (CAP, CR, or CGA protein) (23). The DNA-binding activity of CAP is stimulated by cAMP, but is eliminated by cGMP or by high salt (Table 4 and refs. 23 and 24). Binding specificity has not been demonstrated (23, 24). As shown in Table 4, UV treatment leads to the formation of a CAP–DNA complex that is stable to high salt and cGMP.

We also have confirmed that UV treatment will cause DNA polymerase and RNA polymerase to form salt resistant complexes with BrdU-DNA. All four DNA-binding proteins are effective in causing DNA filter retention at concentrations of 0.01 μg/ml or less (with or without covalent attachment). Other non-DNA-binding proteins (trypsin, ovalbumin, and BSA) will cause filter retention after UV treatment, but at least one 100-fold higher concentrations are needed (1 μg/ml or more). At 50 μg/ml, even BSA will cause filter retention unless it is heat treated (see *Methods*).

DISCUSSION

Markovitz (3) has shown that UV radiation covalently attaches DNA polymerase to poly(dA-dT) and to normal *E. coli* DNA. UV irradiation of BrdU-substituted DNA leads to debromination and the consequent production of highly reactive uracilyl radicals (2, 20). Therefore, it is reasonable to think that protein bound to DNA would be more readily attached to BrdU-DNA than to normal DNA. Smith (2) and Smets and Cornelis (25) have shown, in fact, that UV treatment of cells with BrdU-substituted DNA decreases the amount of DNA that can be extracted. They interpreted this as due to the formation of protein–DNA cross-links. After this paper was in preparation, we learned that Weintraub (26) has also recently obtained evidence for the cross-linking of proteins to BrdU-substituted DNA. He has found that a variety of proteins, including histones and RNA polymerase, can be attached to BrdU-substituted DNA from mammalian cells. If specific attachment occurs, involving the correct sites on the DNA and on the protein, then UV-induced cross-linking promises to be a very useful tool. However, in none of these studies was any evidence obtained for specific attachment.

We report here that the *lac* repressor can be photochemically attached to BrdU-substituted DNA and that in high salt (0.18 M KCl) the reaction is specific for *lac* operator, i.e., attachment occurs to BrdU-λh80*dlac* DNA but not to BrdU-λh80 DNA. Inducers of the *lac* operon (i.e., IPTG) prevent photochemical attachment of repressor to operator if they are present during UV irradiation, but not if added later. In low salt (0.01 M KCl), specificity is not observed; cross-linking occurs to BrdU-λh80 DNA as well as to BrdU-λh80-*dlac*, and IPTG has no effect. By analogy to previous work and from the stability of the repressor–DNA photoproduct we think that covalent bonds are formed.

We find BrdU-substitution to be essential; no attachment to normal λh80*dlac* is obtained even with much higher UV doses. There are large differences between normal and BrdU-substituted DNA in the types and numbers of photoproducts (20). These differences may be critical for the attachment of of sequence specific proteins. BrdU-substituted DNA may be advantageous, not only because of its greater photochemical reactivity, but also because the *lac* repressor binds tighter to BrdU-substituted DNA (8).

Cysteine adds photochemically to DNA (19) and Smith has shown that cysteine reacts with uracil to form 5-*S*-cysteine-6-hydrouracil (27) or with thymine to form 5-*S*-cysteine-6-hydrothymine (28). Eleven other amino acids photochemically add to uracil with cysteine, phenylalanine, tyrosine, histidine, lysine, and arginine being the most reactive (28). Polylysine also has been cross-linked by UV radiation to DNA (26). Since many amino acids can react, it seems likely that most DNA-binding proteins will be cross-linked by UV irradiation. We find that another DNA-binding regulatory protein, the catabolite gene activator protein (23, 24), also can be attached stably to DNA. We also have confirmed (26) that RNA polymerase can be cross-linked to BrdU-DNA.

Specific covalent attachment of DNA-binding proteins to their DNA substrate is obviously of great potential usefulness for identification of the DNA-binding sites of proteins and possibly in the isolation of the DNA region covered by the proteins. For mammalian cells especially, it may be useful to attach covalently chromosomal proteins to their specific sites by UV irradiation prior to disruption of the cell or nucleus. Perhaps less obvious is that covalent attachment may be useful for the *demonstration* of specific binding, which often is a major problem with DNA-binding proteins. For many proteins, binding specificity may be greatest in high salt. However, in high salt, DNA–protein complexes are detectable in sucrose gradients only if impracticably high concentrations of reactants are used; and the same is true for retention on nitrocellulose filters. By the methods described here, it is now possible to fix permanently the protein to DNA under conditions of maximum specificity.

We are grateful for the excellent technical assistance of D. Lin, J. Roberts, and K. Alchian. This work was supported by grants from the National Institutes of Health (HD-04420) and the National Science Foundation (GB-26517).

1. Smith, K. C. (1962) *Biochem. Biophys. Res. Commun.* 8, 157–163.
2. Smith, K. C. & Hanawalt, P. C. (1969) *Molecular Photobiology: Inactivation and Recovery* (Academic Press, New York and London), pp. 57–84.
3. Markovitz, A. (1972) *Biochim. Biophys. Acta* 281, 522–534.
4. Müller-Hill, B., Beyreuther, K. & Gilbert, W. (1971) *Methods in Enzymology*, eds. Grossman, L & Moldave, K. (Academic Press, New York), Vol. 21, pt. D, pp. 483–487.
5. Gilbert, W. & Müller-Hill, B. (1966) *Proc. Nat. Acad. Sci USA* 56, 1891–1898.
6. Riggs, A. D., Suzuki, H. & Bourgeois, S. (1970) *J. Mol. Biol.* 48, 67–83.
7. Lin, S. & Riggs, A. D. (1972) *J. Mol. Biol.* 72, 671–690.
8. Lin, S. & Riggs, A. D. (1972) *Proc. Nat. Acad. Sci. USA* 69, 2574–2576.
9. Hackett, P. & Hanawalt, P. (1966) *Biochim. Biophys. Acta* 123, 356–363.
10. Gilbert, W. & Müller-Hill, B. (1967) *Proc Nat. Acad Sci. USA* 58, 2415–2421.
11. Riggs, D. D., Bourgeois, S., Newby, R. F. & Cohn, M. (1968) *J. Mol. Biol.* 34, 365–368.
12. Riggs, A. D., Newby, R. F. & Bourgeois, S. (1970) *J. Mol. Biol.* 51, 303–314.
13. Riggs, A. D., Bourgeois, S. & Cohn, M. (1970) *J. Mol. Biol.* 53, 401–417.
14. Jobe, A., Riggs, A. D. & Bourgeois, S. (1972) *J. Mol. Biol.* 64, 181–199.
15. Matthews, K. S., Matthews, H. R., Thielmann, H. W. & Jardetzky, O. (1973) *Biochim. Biophys. Acta* 295, 159–165.
16. Oshima, Y., Matsuura, M. & Horiuchi, T. (1972) *Biochem. Biophys. Res. Commun.* 47, 1444–1449.
17. Laiken, S. L., Gross, C. A. & von Hippel, P. H. (1972) *J. Mol. Biol.* 66, 143–155.
18. Jobe, A. & Bourgeois, S. (1973) *J. Mol. Biol.* 75, 303–313.
19. Smith, K. C. & Meun, D. H. C. (1968) *Biochemistry* 7, 1033–1037.
20. Setlow, R. B. & Setlow, J. K. (1972) *Annu. Rev. Biophys. Bioeng.* 1, 293–346.
21. Lin, S. & Riggs, A. D. (1971) *Biochem. Biophys. Res. Commun.* 45, 1542–1547.
22. Bourgeois, S. & Riggs, A. D. (1970) *Biochem. Biophys. Res. Commun.* 38, 348–354.
23. Riggs, A. D., Reiness, G. & Zubay, G. (1971) *Proc. Nat. Acad. Sci. USA* 68, 1222–1225.
24. Nissley, P., Anderson, W. B., Gallo, M. & Pastan, I. (1972) *J. Biol. Chem.* 247, 4264–4269.
25. Smets, L. A. & Cornelis, J. J. (1971) *Int. J. Radiat. Biol.* 19, 445–457.
26. Weintraub, H. (1973) *Cold Spring Harbor Symp. Quant. Biol.* 38, in press.
27. Smith, K. C. & Aplin, R. T. (1966) *Biochemistry* 5, 2125–2130.
28. Smith, K. C. (1969) *Biochem. Biophys. Res. Commun.* 34, 354–357.

US005578442A

United States Patent [19]

Desai et al.

[11] Patent Number: 5,578,442

[45] Date of Patent: Nov. 26, 1996

[54] **GRAFT COPOLYMERS OF POLYCATIONIC SPECIES AND WATER-SOLUBLE POLYMERS, AND USE THEREFOR**

[75] Inventors: **Neil P. Desai**; **Patrick Soon-Shiong**; **Paul A. Sandford**; **Roswitha E. Heintz**, all of Los Angeles, Calif.

[73] Assignee: **VivoRx, Inc.**, Santa Monica, Calif.

[21] Appl. No.: **856,137**

[22] Filed: **Mar. 23, 1992**

[51] **Int. Cl.**[6] **A01N 1/02**; C12N 11/10; C12N 5/00

[52] **U.S. Cl.** **435/1.1**; 435/178; 435/182; 435/240.1; 435/240.22

[58] **Field of Search** 435/1, 41, 240.1, 435/240.22, 962, 178, 182; 264/4.1, 4.32, 4.7; 525/54.1, 54.2

[56] **References Cited**

U.S. PATENT DOCUMENTS

4,663,286	5/1987	Tsang	435/178
5,084,350	1/1992	Chang	428/402.2
5,219,564	6/1993	Zalipsry	424/78.17
5,232,984	8/1993	Hubbell	525/54.1
5,380,536	1/1995	Hubbell et al.	424/497

FOREIGN PATENT DOCUMENTS

WO91/07951 6/1991 WIPO .

OTHER PUBLICATIONS

Ruegg and Hefti, "Growth of Dissociated Neurons in Culture Dishes Coated with Synthetic Polymeric Amines", Neuroscience Letters, vol. 49:319–324 (1984).

Epstein and Lunney, "A Cell Surface ELISA in the Mouse using Only Poly-L-Lysine as Cell Fixative", Journal of Immunological Methods vol. 76:63–72 (1985).

Harris, Milton J., "Laboratory Synthesis of Polyethylene Glycol Derivatives", macromol. Chem. Phys. vol. C25(3):325–373 (1985).

Nagaoka and Nakao, "Clinical application of antithrombogenic hydrogel with long poly(etylene oxide) chains", Biomaterials vol. 11:119–121 (1990).

Zheng et al., Prolonged Pancreas Preservation Using a Simplified UW Solution Containing Polyethylene Glycol, vol. 51:63–66 (1991).

Desai and Hubbell, "Biological responses to polyethylene oxide modified polyethylene terephthalate surfaces", Journal of Biomedical Materials Research vol. 25:829–843 (1991).

Desai and Hubbell, "Solution technique to incorporate polyethylene oxide and other water soluble polymers into surfaces of polymeric biomaterials", Biomaterials vol. 12:144–152 (1991).

Ruegg, U. T., Growth of Dissociated Neurons in Culture Dishes . . . Neuroscience Letters 49 (1984) 319–324.

Desai, N. P., Biological Responses to Polyethylene Oxide . . . J. of Biomed Materials Rsch, vol. 25, 829–843 1991.

Zheng, T., Prolonged Pancrease Preservation Using A . . . Transplantation, vol. 51 63–66 No. 1 Jan. 1991.

Primary Examiner—Ralph J. Gitomer

Attorney, Agent, or Firm—Pretty, Schroeder, Brueggemann & Clark; Stephen E. Reiter

[57] **ABSTRACT**

In accordance with the present invention, there are provided methods to render cells non-adhesive and/or non-immunogenic with respect to macromolecules typically encountered in culture media or in physiological media. The invention method comprises contacting cells with an effective amount of a composition comprising a polycationic species having water-soluble polymer chains grafted thereon.

18 Claims, No Drawings

GRAFT COPOLYMERS OF POLYCATIONIC SPECIES AND WATER-SOLUBLE POLYMERS, AND USE THEREFOR

The present invention relates to methods for rendering cells non-adhesive. In another aspect, the present invention relates to methods for rendering cells non-immunogenic. In yet another aspect, the present invention relates to methods for the stabilization of liposomes. In a further aspect, the present invention relates to methods for the in vitro generation of neural networks.

BACKGROUND OF THE INVENTION

Water-soluble polymers, such as polyethylene glycols (PEGs), have been investigated extensively in recent years for use as biocompatible, protein repulsive, noninflammatory, and nonimmunogenic modifiers for drugs, proteins, enzymes, and surfaces of implanted materials. These characteristics have variously been attributed to a combination of properties of such polymers, e.g., nonionic character, water solubility, backbone flexibility, and volume exclusion effect in solution or when immobilized on a surface.

While extensive efforts have been made to render foreign substances, such as drugs, proteins, and the like, non-immunogenic employing water-soluble polymers such as PEG, the use of such polymers to render an individual cell non-immunogenic has not been considered in the art. If such polymers could be attached directly to a cell surface, then it is possible, due to the exclusion of proteins and macromolecules from the vicinity of the cell surface, that the cell as a whole may be rendered non-immunogenic. The ability to accomplish such attachment would be invaluable for a variety of treatment protocols.

It is known that mammalian cell membranes have a variety of negatively charged species on their exterior. For example, negatively charged proteoglycans (PGA), glycosaminoglycans (GAG), such as chondroitin sulfate and heparin sulfate, and negatively charged lipids have all been identified on cell exteriors. Not surprisingly, polycation species such as polylysine and polyornithine interact with negatively charged cell surfaces to form a strong ionic linkage. Unfortunately, polycations (such as polylysine and polyornithine) are known to be cytotoxic, even at fairly low concentrations. Polylysine, for example, has been used as a cell fixative, and has been shown to cause cell aggregation (e.g., with human platelets).

While water-soluble polymers, having found use in a variety of biological applications, would be ideal for use in treating cells to render them non-immunogenic, their generally non-ionic nature renders them substantially unable to bind to cell membranes. Thus, for example, treatment of cells with unmodified PEG was unable to confer a non-adhesive or protein repellant character on such cells.

BRIEF DESCRIPTION OF THE INVENTION

In accordance with the present invention, we have developed methods to render cells non-adhesive and/or non-immunogenic with respect to macromolecules typically encountered in culture media or in physiological media.

The methods of the present invention can be used for a wide variety of purposes, e.g., for the treatment of cells used for implantation (thereby avoiding the need for immunosuppressive therapy), for the preservation of organs outside the body while awaiting transplant, for modifying surfaces of materials which are to be exposed to various components of physiological media, for the stabilization of liposomes (and prevention of their uptake by the reticuloendothelial system), and the like.

DETAILED DESCRIPTION OF THE INVENTION

In accordance with the present invention, there is provided a method to render cells non-adhesive, said method comprising contacting said cells with an effective amount of a composition comprising a polycationic species having water-soluble polymer chains grafted thereon.

As employed herein, reference to rendering cells "non-adhesive" means, in an in vitro setting, that cells do not stick to wells (e.g., glass, plastic, and the like), or other surfaces with which they come in contact. Instead, non-adhesive cells, as contemplated herein, spread and grow, yet remain in suspension. In an in vivo setting, "non-adhesive" refers to cells which do not adhere to biologically-encountered macromolecules or proteinaceous matrix (e.g., collagen matrix). As used herein, "non-adhesive" also refers to cells which have been rendered non-immunogenic, i.e., cells which are substantially non-susceptible to an immune response mediated by biological macromolecules.

"Contacting" of cells or tissues with graft copolymer compositions contemplated for use in the practice of the present invention is typically carried out in vitro at room temperature for a time in the range of about 0.01 up to 1 hour or longer in suitable physiological buffer (i.e., pH in the range of about 7.2–7.4; osmolarity of about 290 mOsm/kg) containing a concentration of at least about 0.005% of graft copolymer, with respect to the concentration of the polycationic species used for the preparation of the cell surface (e.g., polylysine). It is presently preferred to treat cells with a solution of graft copolymer containing a concentration of graft copolymer in the range of about 0.05 up to 1.0%, with concentrations of graft copolymer in the range of about 0.1 up to 0.5% being especially preferred. Those of skill in the art recognize that as the molecular weight of the polycationic species is increased, a lower concentration (determined on the same basis as set forth above) of the graft copolymer is required to produce the same beneficial effect.

As employed herein, an "effective amount" of graft copolymer compositions contemplated for use in the practice of the present invention is an amount sufficient to render said cells non-adhesive to biological macromolecules, while leaving the cells viable (as determined, for example, by suitable staining techniques). In the case of specialized cells, such as islets, it is desirable for the treated cells to retain their unique function as well as viability (i.e., the ability of islets to respond to exposure to glucose by secretion of insulin). Typically, an excess of graft copolymer is used with respect to the negative charges present on the surface of the cells to be treated. The quantity of graft copolymer required will vary depending on the cell type being treated and the concentration of cells to be treated. Typically, in the range of about 10^2–10^8 cells/ml will be treated. For example, up to about 10^8 bacterial cells/ml, up to about 100,000 fibroblasts/ml, or up to about 50,000 islets/ml will be treated.

Copolymer compositions contemplated for use in the practice of the present invention comprise a polycationic species having water-soluble polymer chains grafted thereon. Polycationic species contemplated for use in the practice of the present invention are polycationic species having sufficient charge density to allow binding of the above-described graft copolymer to cells, and include:

polymers containing primary amine groups, secondary amine groups, tertiary amine groups or pyridinyl nitrogen(s), such as polyethyleneimine, polyallylamine, polyetheramine, polyvinylpyridine, and the like,

polysaccharides having a positively charged functionality thereon (e.g., chitosan),

polyamino acids, such as:

poly-L-histidine, poly-im-benzyl-L-histidine,
poly-D-lysine, poly-DL-lysine, poly-L-lysine,
poly-ε-CBZ-D-lysine, poly-ε-CBZ-DL-lysine,
poly-ε-CBZ-L-lysine,
poly-DL-ornithine, poly-L-ornithine,
poly-δ-CBZ-DL-ornithine,
poly-L-arginine,
poly-DL-alanine-poly-L-lysine;
poly (-L-histidine, L-glutamic acid)-poly-DL-alanine-poly-L-lysine;
poly(L-phenylalanine, L-glutamic acid)-poly-DL-alanine-poly-L-lysine;
poly(L-tyrosine, L-glutamic acid)-poly-DL-alanine-poly-L-lysine;

random copolymers of:

L-arginine with tryptophan, tyrosine, or serine;
D-glutamic acid with D-lysine;
L-glutamic acid with lysine, ornithine, or mixtures thereof;

and the like, as well as mixtures of any two or more thereof.

Presently preferred polycations for use in the practice of the present invention include polylysine (i.e., poly-D-lysine (PDL), poly-DL-lysine, poly-L-lysine (PLL), poly-ε-CBZ-D-lysine, poly-ε-CBZ-DL-lysine, or poly-ε-CBZ-L-lysine), polyornithine (i.e., poly-DL-ornithine, poly-L-ornithine or poly-δ-CBZ-DL-ornithine), and the like.

Polycationic species having a wide range of molecular weights can be employed in the practice of the present invention. Polycations having a MW in the range of about 200 up to 1,000,000 are suitable, with molecular weights in the range of about 1000 up to 100,000 preferred. Presently most preferred polycationic species for use in the practice of the present invention will have molecular weights in the range of about 5,000 to 50,000.

Optionally, the polycationic species employed in the practice of the present invention can be further modified with one or more functional groups capable of undergoing free radical polymerization. Suitable functional groups for this purpose include unsaturated species capable of free radical polymerization, such as, for example, acrylate groups, vinyl groups, methacrylate groups, and the like. When cells or tissues are treated with such modified polycationic species, the graft copolymer can be further subjected to free radical polymerization conditions, thereby stabilizing the association of graft copolymer with the cell surface. In addition, the further crosslinking of the graft copolymer forms a highly stabilized, immunoprotective coating of water-soluble polymer about the treated cell or tissue.

Free radical polymerization of the above-described modified polycationic species can be carried out in a variety of ways, for example, initiated by irradiation with suitable wavelength electromagnetic radiation (e.g., visible or ultraviolet radiation) in the presence of a suitable photoinitiator, and optionally, cocatalyst and/or comonomer. Alternatively, free radical polymerization can be initiated by thermal decomposition of a suitable free radical catalyst, such as benzoyl peroxide, azobisisobutyronitrile, and the like.

Photoinitiators contemplated for use in the practice of the present invention include such ultraviolet (UV) initiators as 2,2-dimethyl phenoxyacetophenone, benzophenones and ionic derivatives (for water solubility), benzils and ionic derivatives thereof, thioxanthones and ionic derivatives thereof; and visible photoinitiators such as ethyl eosin, eosin, erythrosin, rose bengal, thionine, methylene blue, riboflavin, and the like.

Cocatalysts are typically used when the excited state of the photoinitiator is quenched too rapidly to efficiently promote polymerization. In such a situation, a cocatalyst (also referred to in the art as a "cosynergist", "activator", "initiating intermediate" or "quenching partner") will generally be employed. Cocatalysts contemplated for use in the practice of the present invention include triethanolamine, methyl diethanolamine, triethylamine, arginine, and the like.

Water-soluble polymeric species contemplated for use in the practice of the present invention are water-soluble polymers capable of rendering polycations non-immunogenic and include non-ionic, water-soluble polymers such as polyethylene glycol (PEG), polyvinyl alcohol (PVA), poly(hydroxyethyl methacrylate) (pHEMA), poly(acrylamide), poly(vinyl pyrrolidone) (PVP), poly(ethyl oxazoline), polysaccharides (such as, for example, starch, glycogen, guar gum, locust bean gum, dextran, levan, inulin, cyclodextran, agarose, and the like); as well as ionic, water-soluble polymers such as polyacrylic acid (PAA) or polysaccharides (such as, for example, xanthan gum, carageenan, hyaluronic acid, heparin, chitosan, pectin, and the like); as well as copolymers of any two or more of said water-soluble polymeric species. Presently preferred water soluble polymers employed in the practice of the present invention are polyalkylene oxides, such as polyethylene glycol (PEG).

Water-soluble polymeric species having a wide range of molecular weights can be employed in the practice of the present invention. Polymeric species having a MW in the range of about 200 up to 1,000,000 are suitable, with molecular weights in the range of about 500 up to 100,000 preferred. Presently most preferred polymeric species for use in the practice of the present invention will have molecular weights in the range of about 1000 to 50,000.

Optionally, the water-soluble polymeric species employed in the practice of the present invention can be further modified with one or more functional groups capable of undergoing free radical polymerization. Suitable functional groups for this purpose include unsaturated species capable of free radical polymerization, such as, for example, acrylate groups, vinyl groups, methacrylate groups, and the like. When cells or tissues are treated with such modified water-soluble polymeric species, the graft copolymer can be further subjected to free radical polymerization conditions, thereby stabilizing the association of graft copolymer with the cell surface. In addition, the further crosslinking of the graft copolymer forms a highly stabilized, immunoprotective coating of water-soluble polymer about the treated cell or tissue.

Free radical polymerization of the above-described modified water-soluble polymeric species can be carried out in the same manner as described above with respect to free radical polymerization of modified polycationic species.

Graft copolymers contemplated for use in the practice of the present invention are those wherein the polycationic species has grafted thereon at least one water-soluble polymer chain per chain of said polycationic species, up to a maximum of one grafted chain per repeat unit of said polycationic species. For example, when the molecular weight of the polycationic species falls in the range of about 20,000, it will typically have grafted thereon at least about 5 chains of said water-soluble polymer chain per chain of

polycationic species; with in the range of about 10–20 chains of said water-soluble polymer chain per chain of said polycationic species being the presently most preferred level of grafting. Those of skill in the art recognize that with polycationic species having higher molecular weights, higher levels of grafting will be desirable, and that the above values for grafting levels should be increased accordingly. Similarly, with respect to the water-soluble component of invention graft copolymers, the use of higher molecular weight species will allow one to achieve substantially the same result while grafting fewer (water-soluble) chains per chain of polycationic species.

Preparation of the graft copolymers of the present invention can be carried out employing chemical techniques known by those of skill in the art. For example, the free hydroxyl groups of the water-soluble component can be activated to render such groups susceptible to nucleophilic displacement. Thus, the free hydroxyl groups of the water-soluble component can be subjected to esterification, etherification, amidation, urethane formation, and the like. Such reactions involve the generation of such intermediates as carbonates, sulfonates, xanthates, epoxides, aliphatic aldehydes, carboxymethyl azides, succinimidyl succinates, and the like. The activated water-soluble component can then be coupled to a suitable polycationic species, for example, by nucleophilic displacement.

Cell types contemplated for use in the practice of the present invention include islets, fibroblasts, thyroid cells, parathyroid cells, adrenal cells, neuronal cells, dopamine secreting cells, hepatocytes, nerve growth factor secreting cells, adrenaline/angiotensin secreting cells, norepinephrine/metencephalin secreting cells, human T-lymphoblastoid cells sensitive to the cytopathic effects of HIV, and the like.

Also included within the scope of the present invention are cells having a modified cell surface which is substantially non-adhesive with respect to macromolecules encountered in physiological environments.

In accordance with another embodiment of the present invention, there is provided a process to remove copolymer compositions contemplated for use in the practice of the present invention from cells treated as described above, said process comprising contacting such cells with an effective amount of an anionic species.

Anionic species contemplated for use in this embodiment of the present invention include monomeric or polymeric anions. Any soluble anionic species capable of reversing the association of polycationic species with negatively charged cell surface can be employed for this purpose. Presently preferred anionic species are polyanionic species, such as, for example, heparin, heparin sulfate, chondroitin sulfate, soluble alginates (e.g., sodium alginate, potassium alginate, ammonium alginate, and the like), bovine serum albumin, hyaluronic acid, pectin, carageenan, oxidized cellulose, and the like.

"Contacting" of treated cells to remove invention copolymer therefrom is carried out at room temperature for a time in the range of about 0.01 up to 1 hour or longer in physiological buffer solution containing anionic species at a sufficiently high ionic strength to reverse the association of polycationic species with negatively charged cell surface.

An effective amount of anionic species to employ in accordance with this embodiment of the present invention depends on the specific anionic species employed. Generally, the concentration of anionic species employed will be sufficient to reverse polycation binding to cells or tissues, but not so high as to be toxic to the biological material being treated. Concentrations employed are typically in excess of the amount of anion actually needed to disrupt binding of polycation to cell surface. Thus, for example, presently preferred treating solutions contain about 2.5 Units/ml of heparin or 2 mg/ml of bovine serum albumin.

In accordance with yet another embodiment of the present invention, there is provided a method to render cells non-immunogenic, said method comprising contacting said cells with an effective amount of a composition comprising a polycationic species having water-soluble polymer chains grafted thereon.

"Contacting" of cells with graft copolymer compositions to render cells non-immunogenic is typically carried out as described above with respect to rendering cells non-adhesive.

The process of the present invention can be used for rendering non-immunogenic any cell, tissue, organ, or system of organs, and the like, that may be used for transplant or the like.

Also included within the scope of the present invention are cells having a modified cell surface which is substantially non-immunogenic with respect to mediators of immune response, e.g., biological macromolecules such as proteins, enzymes, and the like.

In accordance with another embodiment of the present invention, there is provided a process to remove copolymer compositions contemplated for use in the practice of the present invention from cells treated as described above, said process comprising contacting treated cells with an effective amount of an anionic species, as described above.

In accordance with still another embodiment of the present invention, there is provided a method to preserve cells and/or tissues which are subjected to long periods of storage before being used for therapeutic applications, said method comprising contacting said cells and/or tissues with an effective amount of a composition comprising a polycationic species having water-soluble polymer chains grafted thereon.

"Contacting" of cells and/or tissues with graft copolymer compositions to preserve same is typically carried out as described above with respect to rendering cells non-adhesive and/or non-immunogenic.

In accordance with a still further embodiment of the present invention, there is provided a method for associating water-soluble polymer with a cell surface, said method comprising:

grafting water-soluble polymer onto a polycationic resin to produce a copolymer of said water-soluble polymer and said polycation, and thereafter

contacting said cell surface with an effective amount of said copolymer.

If desired, the copolymer can be substantially removed from the cell surface employing the above-described removal process.

In accordance with a further embodiment of the present invention, there is provided a method for the stabilization of liposomes having negatively charged surfaces, said method comprising contacting said liposomes with an effective, stabilizing amount of a composition comprising a polycationic species having water-soluble polymer chains grafted thereon.

"Contacting" of liposomes for the stabilization thereof is carried out at room temperature for a time in the range of about 0.01 up to 1 hour or longer in physiological buffer.

An effective amount of graft copolymer for use in this embodiment of the present invention is an amount sufficient to render such liposomes essentially non-detectable in vivo, thereby reducing uptake of the liposome by the reticuloen-

dothelial system (and increasing liposome circulation times in vivo). Suitable quantities of graft copolymer will render the liposomes substantially non-adhesive to biological materials, while leaving the liposome intact, and without adversely affecting the function and/or activity of the contents thereof, if any. Typically, a concentration of graft copolymer sufficient to neutralize the negative charges on the surface of the liposome will be employed. Concentrations in the range of at least about 0.05% of graft copolymer, with respect to the concentration of the polycationic species used to treat the surface of said liposome will be employed; with concentrations of graft copolymer in the range of about 0.1 up to 0.5% being presently preferred.

One can readily determine the stability of a liposome using a functional assay, such as the following. In an in vitro setting, the stability of liposome-encapsulated hemoglobin in an un-modified liposome could be compared to the stability of hemoglobin encapsulated in a liposome stabilized in accordance with the present invention (i.e., the result of treating an un-modified liposome with a sufficient quantity of graft copolymer described above to stabilize the liposome). The release of hemoglobin into the surrounding buffer media over time would then be assayed, with an extended time-frame for release of hemoglobin indicating enhanced liposome stability.

In accordance with yet another embodiment of the present invention, there is provided a method for producing neural networks on a substrate, said method comprising:

masking that portion of said substrate which defines the desired network,

rendering the unmasked portion of said substrate non-adhesive by the above-described method of the invention,

removing the mask, then

allowing cells to spread and grow on said substrate, wherein cells grow only on the portion of the substrate which has not been treated with graft copolymer.

Substrates contemplated for use in the above-described method include tissue culture substrates, such as collagen, tissue culture polystyrene, microporous dextran substrate, and the like.

Masking contemplated by the above-described method can be accomplished in a variety of ways, such as, for example, by covering a portion of the substrate with an agent which does not serve as a substrate for cell growth (e.g., a piece of tape, or the like).

The masking agent employed can readily be removed by merely reversing the process employed for applying the mask to the substrate.

Conditions required for cells to spread and grow on the substrate are standard cell culture conditions.

The resulting neural networks can be used for a variety of purposes, such as, for example, for studying the transmission of nerve impulses, for connection between a nerve cell and an electrical circuit, and the like.

The invention will now be described in greater detail by reference to the following non-limiting examples.

EXAMPLES

EXAMPLE I

Synthesis of a Graft copolymer of Poly-L-Lysine and Polyethylene Glycol

Twenty grams (20 g) of PEG (molecular weight 10,000 g/mol, having the structure HO-PEG-OH) were dried in a vacuum oven at 80° C. for 24 hours and dissolved in 100 ml of methylene chloride that had been dried by molecular sieves (4A). Then, 3.24 g of 1,1-carbonyldiimidazole (CDI, 5 fold excess, to ensure the activation of 100% of PEG end groups) were added to the solution and stirred overnight at room temperature in an argon atmosphere. The CDI-activated PEG was then precipitated with an excess of anhydrous diethyl ether and dried overnight under vacuum. Five grams (5 g) of the CDI-activated PEG were dissolved in 20 ml of 5 mM sodium borate buffer (pH 9). In order to prevent crosslinking of poly-L-lysine (PLL) with the 100% CDI-activated PEG, 50% of the PEG end groups were inactivated by adding 30.2 µl of ethanolamine to the buffer solution and stirring for 4–6 hours at room temperature. This results in a mono-activated CDI-derivative of PEG, having the structure CDI-PEG-OH. Alternatively, a monomethoxy PEG could be used to avoid this partial deactivation step, but monomethyl PEGs are presently available commercially only up to molecular weight 5000.

Following the above-described partial deactivation step, 50 mg of PLL (M.W. 20,100 g/mol) were added to the reaction mixture and stirred for 24 hours at room temperature. The solution was then dialyzed for 24 hours against deionized water and freeze dried to obtain a powder. This procedure produced a PEG graft copolymer (PLL-PEG) having a concentration of approximately 10–20 PEG chains per PLL chain.

EXAMPLE II

Demonstration of Cell Binding Properties of PLL-PEG to Fibroblasts: Effect on Cells in Suspension

The cell binding effects of PLL-PEG copolymer produced as described in Example I were tested on cultures of human foreskin fibroblasts (HFF). These cells are anchorage dependent and ordinarily die within 4 to 10 hours if they do not adhere and spread on a surface. Thus, a flask of confluent HFF was harvested with trypsin-EDTA, then the resultant cells in suspension were split into 6 batches, each containing approximately 170,000 cells. Each batch was centrifuged to obtain cell pellets. Six different solutions were used for cell treatment:

(A) Fibroblast culture media: Dulbecco's modified Eagles' medium (D-MEM) containing 10% fetal bovine serum;

(B) 10 mM HEPES buffered saline (HBS), pH 7.4;

(C) HBS containing 0.1% (w/v) PLL;

(D) HBS containing 0.5% PEG (M.W. 10,000);

(E) HBS containing 0.1% PLL and 0.5% PEG; and

(F) HBS containing 0.3% PLL-PEG (based on PLL concentration).

All solutions were sterilized by filtration through 0.22 micron filters prior to use. The cell pellets were resuspended in 2 ml of solutions A, B, C, D, E or F for approximately 10 minutes. The tubes were then centrifuged (200×g for 5 minutes), the solutions aspirated and replaced with fibroblast culture medium, and the cells plated onto culture dishes. The plated cells were observed periodically to verify adherence and spreading. The cells were also stained with trypan blue (TB) to test viability. Table I summarizes the observations over 5 days following the seeding.

TABLE I

TIME AFTER SEEDING	HFF TREATMENT SOLUTIONS A (fibroblast culture medium)	B (buffered saline)	C (PLL)	D (PEG)	E (PLL + PEG)	F (PLL-PEG copolymer)
1 hr	Normal spreading	Normal spreading	No adherence; Cell clumping	Normal spreading	No adherence; Cell clumping	No adherence; No clumping
% viability	95	95	0	90	0	80
24 hr	Normal spreading	Normal spreading	No adherence; Cell clumping	Normal spreading	No adherence; Cell clumping	No adherence; No clumping
% viability	100	100	0	95	0	70
48 hr	Confluent monolayer	Confluent monolayer	No adherence; Cell clumping	Confluent monolayer	No adherence; Cell clumping	No adherence; No clumping
% viability	100	100	0	95	0	60
120 hr	Confluent monolayer	Confluent monolayer	No adherence; Cell clumping; Few spread Cells	Confluent monolayer	No adherence; Cell clumping; Few spread Cells	No adherence; No clumping; Few spread Cells
% viability	100	100	<1	95	<3	60

Treatments A, B, and D showed essentially the same results, with most of the HFF showing normal spreading and viability.

Free PLL was found to be toxic at the concentrations used (treatments C and E). Essentially all cells subjected to treatments C and E took up TB and did not spread on the tissue culture substrate. The cells subjected to treatments C and E also showed extensive aggregation.

Free PEG had no appreciable effect on cell function (treatment D). PEG also had no appreciable ameliorating effect in conjunction with PLL (treatment E).

Incubation with the graft PLL-PEG copolymer of the present invention (treatment F) however, had a remarkable effect on the HFF. In stark contrast to treatment with free PLL, treatment with the copolymer PLL-PEG (at 3 times higher concentration than used for treatments C and E) produced cells that showed no adherence to the substrate, no aggregation in suspension, but a high percent viability. This viability was maintained for well over 24 hours with the HFF still in suspension. This behavior is quite unusual for anchorage dependent cells.

A distinct morphological difference in cells treated with PLL and PLL-PEG was evident. PLL treated cells in suspension showed a rough or ragged surface while those treated with PLL-PEG copolymer of the present invention are smooth and spherical, much like freshly trypsinized cells.

These results indicate that treatment with the PLL-PEG copolymer of the invention is noncytotoxic to HFF. In addition, interaction of the PEG-grafted polycation with the exterior of the cell prevents the cell from adhering to a substrate. Thus the cytotoxicity of PLL is markedly reduced by PEG grafting.

Five days after the initial treatment, a few of the cells treated with PLL-PEG copolymer begin to show some spreading on the surface of the culture dish. This observation implies that the PLL-PEG copolymer may either have desorbed from the cell surfaces, or cell division may have occurred (which would dilute the concentration of PLL-PEG copolymer on the cell membrane).

EXAMPLE III

Assessment of Efficacy of PLL and PLL-PEG Treatments at Various Dilutions

A similar experiment as outlined in Example II was conducted to test the effects of PLL and PLL-PEG copolymer at various dilutions. Solutions C and F were serially diluted with 10 mM HEPES buffered saline (HBS) to 1/5, 1/25, and 1/125 of their original concentrations, and human foreskin fibroblasts (HFF) incubated in these solutions for 10 minutes. Additional treatments included PEG 20M (a PEG composition having a molecular weight of about 20,000, comprised of two lower molecular weight PEGs (one having a MW ~8,000 and the other having a MW of ~10,000) linked together by a hydrophobic, bifunctional bisphenol-epichlorohydrin linker; available from Union Carbide, Danbury, Conn.) and PEG 20,000 (a substantially linear PEG having a molecular weight of ~20,000; available from Fluka, Ronkonkoma, N.Y.) at 0.5% in HBS. A control treatment with fibroblast culture media was also run. Results are summarized in Table II, below.

In the Table, the following abbreviations are used:

"adh." for adhesion,

"aggreg." for aggregated, and

"subst." is the abbreviation for substrate.

P-0 refers to cells treated with 0.1% of PLL, and P-5, P-25 and P-125 refer to cells treated with 1/5, 1/25, and 1/125 dilutions thereof, respectively. Similarly, G-0 refers to cells treated with 0.3% of PLL-PEG copolymer, and G-5, G-25 and G-125 refer to cells treated with 1/5, 1/25, and 1/125 dilutions thereof, respectively.

TABLE II

TIME AFTER SEEDING	HFF TREATMENT SOLUTIONS: Control: No PEG	Control: 20M PEG	Control: 20,000 PEG	PLL treatment: P-0	PLL treatment: P-5	PLL treatment: P-25	PLL treatment: P-125	PLL-PEG copolymer treatment: G-0	PLL-PEG copolymer treatment: G-5	PLL-PEG copolymer treatment: G-25	PLL-PEG copolymer treatment: G-125
0 hr		Minor adh. to substr.		Clumped	Clumped	Clumped	Clumped; adh. to subst.	No adh.	No adh.	Minor adh. to subst.	Minor adh. to subst.
3 hr		100% adh. to subst.		Clumped; aggreg.; no adh. to subst.	Clumped; aggreg.; no adh. to subst.	Clumped; 5–10% adhered to subst.	Clumped; 5–10% adhered to subst.	No adh.	50% adh.	75% adh. to subst.	100% adh. to subst.
24 hr		100% adhesion		No adh; Extensive clumping	No adh; Extensive clumping	Clumped; ~10% adh. to subst.	Clumped; ~10% adh. to subst.	No adh.; no clumping	~60% adh.;	~80% adh.	~100% adhesion
% viability		100%		<10%	<10%	<10%	<10%	>70%	>70%	>70%	>70%

Observation of the cells immediately after seeding showed all PLL treatments (abbreviated P) to cause clumping of cells. A small number of cells showed adherence in the P-125 treatment. The graft copolymer (PLL-PEG, abbreviated G) treatment showed a decrease in efficacy at the lower concentrations. At dilutions of 25 and 125 (G-25 and G-125), adherence of cells was noted, though not quantified. Treatments with the PEG 20M and PEG 20,000 showed no appreciable difference from the control.

Three hours following the initial seeding, the following observations were made. The PLL treated cells P-0 (0.1% PLL) and P-5 were clumped and aggregated, with none of the cells showing adherence to the substrate. P-25 and P-125 also showed clumping, but approximately 5–10% of cells adhered to the substrate, indicating PLL cytotoxicity at very low concentrations.

Cells treated with PLL-PEG showed an increased adhering tendency with increasing dilutions. G-0 (0.3% PLL-PEG) showed no adhesion and individual free-floating cells. G-5, G-25, and G-125 showed approximately 50%, 75% and 100% adherence, respectively, at 3 hours. G-125 was very similar to the PEGs and the control.

After 24 hours, P-0 and P-5 showed no adherence to substrate, and extensive clumping. P-25 and P-125 also showed clumping, but approximately 10% of the cells were adhered to the substrate, indicating a lower level of toxicity for P-25 and P-125, compared to the higher concentrations used in samples P-0 and P-5.

After 24 hours, G-0 showed no adherence to substrate and no clumping; while G-5, G-25 and G-125 showed increasing levels of adherence of approximately 60%, 80% and 100%, respectively. The PEG treatments and the control were also 100% adhered.

TB staining at 24 hours showed all PLL treatments to have less than 10% viability, while the treatments with PLL-PEG copolymer showed a viability of greater than 70%. Thus the attachment of PEG to PLL substantially alleviates the PLL toxicity; this effect is apparent at very low concentrations (P-125=0.0008% PLL; G-125=0.0024%).

EXAMPLE IV

Effect of PLL and PLL-PEG on Confluent Monolayers of Fibroblasts

In order to assess, in a more realistic (although in vitro situation), the effects of PLL and PLL-PEG copolymer of the invention on cells which would normally be present in a flattened spread morphology (and not in a rounded morphology), confluent monolayers of HFF were treated with solutions P-0, P-5, G-0, G-5, PEG 20M, and a control (fibroblast culture medium). The cells were exposed to these solutions for 10 minutes, followed by a rinse with HBS, then fibroblast culture medium was returned to the culture dishes.

Short-term observation 15 minutes after treatment showed the P-0 treated cells sloughing off the culture substrate, with approximately 90% of all cells in suspension at 20 minutes.

About 2–5% of cells treated with P-5 were detached from the surface within the same 15 minute period.

HFF treated with solutions G-0, G-5 and PEG 20M showed no appreciable difference from the control cells.

These results indicate that PLL (at 0.1%) is clearly toxic to HFF, while similar concentrations of PLL modified with PEG show no harmful effects to confluent monolayers of cells. It is noteworthy that the P-5 treatment showed only mild toxicity to spread, confluent fibroblasts, indicating that they may be less susceptible to toxic macromolecules in this state rather than in suspension.

EXAMPLE V

Reversal of PLL-PEG Binding to Cells with Polyanions

It was possible, by addition of heparin sulfate or chondroitin sulfate, to reverse the effect of PLL and PLL-PEG on HFF. Thus, addition of 2.5 U/ml of heparin to the fibroblast culture medium soon after treatment with PLL caused disaggregation of the HFF clumps and resulted in cells that were able to adhere to tissue culture substrates. If, however, the addition of heparin was postponed until several hours after the PLL treatment, reversibility was not possible because the cells had succumbed to PLL toxicity.

This however, was not the case with the PLL-PEG copolymer if the present invention. The nonadhesive, nonaggregating nature conferred upon the fibroblasts by treatment with PLL-PEG copolymer was found to be reversible at least 48 hours after the initial treatment, clearly indicating that these anchorage dependent cells were still alive, despite the fact that they were not adhered to a substrate.

EXAMPLE VI

Resistance of PLL-PEG Treated Cells to specific Antibodies as Indicators of Conferred Immune Protection

Fibroblasts have receptors for the protein vitronectin on their surfaces. Vitronectin is a cell adhesion molecule (CAM). This receptor (called αV-β3) can be targeted with an antibody, anti αV-β3, a rabbit polyclonal. A fluorescently conjugated secondary antibody to anti αV-β3 (e.g., rhodamine conjugated anti IgG, goat anti-rabbit) would permit the visualization of these receptors on the cell surface.

Untreated HFF, PLL treated HFF, and PLL-PEG treated HFF were incubated with anti αV-β3 polyclonal antibody, followed by incubation with the secondary antibody, then observed at the appropriate excitation wavelengths under a microscope. It was observed that the untreated and PLL treated cells showed strong fluorescence, while the PLL-PEG treated cells fluoresced at a much lower level. This observation indicates that the approach of the antibody to the cell is hindered by the presence of PEG.

PLL by itself was found not to affect the receptor-ligand interaction.

Based on the above-described experiments, it is likely that the prevention of protein binding to these cells will render them immunologically unrecognizable.

EXAMPLE VII

Transplantation of PLL-PEG Treated Allogeneic Islets in Rats as a Model for Immunoprotectivity

Rat islets were isolated employing techniques known in the art [see, for example, Lacy and Kostianovsky in Diabetes 16:35 (1967)]. The isolated islets were treated with 0.3% PLL-PEG as described above (see Example II), and transplanted by injection into the peritoneal cavity of diabetic rats. Diabetes was induced by treatment with streptozotocin. Controls were injected with untreated rat islets. Blood glucose levels of these rats were monitored at first on an hourly basis, and then on a daily basis for several weeks. It was found that the control rats had a reversal of diabetes (indicated by normal glucose levels) for 3–4 days following which the graft failed due to rejection. On the other hand, the rats injected with the PLL-PEG copolymer treated islets showed a continuous reversal of diabetes for several weeks, indicating that the treatment of these cells with PLL-PEG copolymer was effective in immunoprotecting the islets.

EXAMPLE VIII

Crosslinkable Graft Copolymers

A variation on the above theme for the surface treatment of cells is one in which the PLL-PEG graft copolymer has on its structure polymerizable groups such as the acrylate group. The presence of this group on the graft copolymer facilitates polymerization or crosslinking following the absorption of the copolymer onto the cell surface through ionic interactions. The resultant covalently crosslinked network is significantly more stable than the ionically attached graft copolymer. Thus the immunoprotective properties conferred upon the cell by absorption of PLL-PEG on its surface are no longer transient as may be expected through an ionic interaction, but are permanent due to the formation of intermolecular and intramolecular covalent crosslinks formed with the PLL-PEG.

Synthesis of these polymerizable copolymers could have two possible strategies. One involves the synthesis of a PEG that is heterobifunctional, i.e., one end is functionalized with CDI (1,1-carbonyldiimidazole; or other electrophilic derivative) and the other with acryloyl chloride (the reaction of PEG with acryloyl chloride is described below). This technique allows the synthesis of a PLL-PEG graft copolymer in which the free end of PEG contains a polymerizable double bond. The second strategy involves the preparation of PLL-PEG as described above, and the subsequent reaction of the copolymer with acryloyl chloride to add polymerizable groups. In this case the addition of polymerizable groups to the copolymer is nonspecific, i.e., the substitution occurs on the free end of the PEG as well as on the amines on polylysine.

The reaction of PEG with acryloyl chloride proceeds to completion in about 24 hours when carried out at 50° C. For example, mono-CDI functionalized PEG (i.e., CDI-PEG-OH, prepared as described in Example I) was reacted with an equimolar amount of acryloyl chloride in dry dichloromethane solvent. The reaction was carried out in a round-bottom flask under an inert atmosphere at constant reflux for 24 hours. The resulting product was purified by precipitation with diethyl ether, then dried in a vacuum oven.

Alternatively, PLL-PEG could be treated with acryloyl chloride. In this situation, acrylate substitution would occur on both the PEG chains and the PLL backbone (via the amine groups thereof).

Photopolymerization is the method of choice for covalent crosslinking of the graft copolymer following attachment to the cell surface. Following attachment of the graft copolymer to the cell surface the treated cells are transferred to a physiological buffer solution containing ethyl eosin (EE, 0.1 μM to 0.1 mM), triethanolamine (TEA, 0.1 mM to 0.1M), and optionally a comonomer (e.g. 1-vinyl 2-pyrrolidinone (VP) at a concentration in the range of about 0.001 to 1.0%, when used). This solution containing islets is well mixed and exposed to a mercury lamp (100 watt) with a bandpass filter (500–560 nm) for approximately 3 minutes. This causes crosslinking of the copolymer on the surface of the cell resulting in the immunoprotective layer. The cells are then transferred to culture.

An alternative technique involves the incubation of the copolymer treated cells with a solution of EE (0.1 μM to 0.1 mM) in physiological buffer for approximately two minutes. In this step the EE complexes with the positively charged polycation on the cell surface. After rinsing in buffer the cells are transferred to a physiological buffer solution containing TEA (conc. as above), and a comonomer e.g. VP (optional). This solution containing islets is well mixed, polymerized as before, and transferred to culture.

EXAMPLE IX

PLL-PEG Solutions in Organ Preservation Media

As noted above, PEG 20M has been used in the preservation of organs. The basis of its activity, though not clearly understood, is believed to be the binding of PEG to cell surface molecules through nonspecific hydrophobic interactions. The PLL-PEG copolymer of the present invention, however, interacts directly through ionic interactions with cell-surface moieties bearing a negative charge. Thus, tissues and organs may be flushed with a solution containing the PLL-PEG copolymer prior to transplantation to, in effect, 'coat' the tissues with PEG, thereby providing an immunoprotective and organ-protective effect.

EXAMPLE X

Stabilization of Liposomes with PLL-PEG for Longer Circulation Times and Increased Biocompatibility

Lipid vesicles or liposomes have been investigated extensively as systems for drug delivery (Gregoriadis, 1987). The commonly used phospholipids that comprise liposomes, such as phosphatidyl choline, phosphatidyl serine, dilaurylphosphatidic acid, and phosphatidylglycerol are negatively charged at physiological pH. The interaction of polycations such as PLL with the negatively charged phospholipids has been studied quite extensively with regard to conformational changes induced in PLL and consequent stability [Fukushima et al., *Biophysical Chemistry* 34:83 (1989); Houbre et al., *Biophysical Chemistry* 30:245 (1988)]. Stability of liposomes in physiological conditions is a major focus of researchers investigating drug delivery. Although PLL may be used to stabilize lysosomes in vitro, PLL coated liposomes in vivo are likely to be rapidly overgrown or ingested by macrophages due to the adhesive nature of PLL, thus making them ineffective for the controlled release of drugs. In addition, liposomes may also be destroyed by uptake by the reticuloendothelial system. The addition of the graft copolymers of the present invention to the surface of the liposome is likely to prevent this uptake.

The replacement of PLL by the PLL-PEG copolymer of the present invention, however, promises to provide a liposome that is stable not only due to interactions between negatively charged phospholipid and positively charged PLL, but also because the PLL-PEG copolymer will prevent interactions with proteins, and therefore prevent interactions with cells such as macrophages. This should result in liposomes with long circulation times which can therefore deliver drugs in a controlled fashion.

EXAMPLE XI

Patterned Surfaces for Neural Networks

Investigators in neurology have tried to generate in vitro networks of neurons on culture dishes. A problem has been to generate patterned surfaces that are preferentially adherent to cells in order to design 'biological circuits.' By creating a mask of the pattern desired, and applying it to the culture substrate, followed by treatment of the surface with PLL-PEG copolymer, one can selectively leave the desired pattern adhesive to cells, while the rest of the available surface is rendered nonadhesive to cells.

While the invention has been described in detail with reference to certain preferred embodiments thereof, it will be understood that modifications and variations are within the spirit and scope of that which is described and claimed.

That which is claimed is:

1. A method to render cells non-adhesive, said method comprising directly contacting a surface of said cells with an effective amount of a composition comprising a polycationic species having water-soluble polymer chains grafted thereon.

2. A method according to claim 1 wherein said water-soluble polymer is selected from polyethylene glycol (PEG), polyvinyl alcohol (PVA), poly(hydroxyethyl methacrylate) (pHEMA), polyacrylic acid (PAA), poly(acrylamide), poly (vinyl pyrrolidone) (PVP), poly(ethyl oxazoline) (PEOX), polysaccharides, or copolymers of any two or more thereof.

3. A method according to claim 1 wherein said polycationic species has grafted thereon at least one water-soluble polymer chain per chain of said polycationic species.

4. A method according to claim 3 wherein said water-soluble polymer is polyethylene glycol.

5. A method according to claim 1 wherein either the water-soluble polymer, or the polycationic species, or both contain at least one functional group which is susceptible to free radical polymerization.

6. A method according to claim 5 wherein said composition is further subjected to free radical polymerization conditions.

7. A method according to claim 1 wherein said polycationic species is selected from one or more of:

polyethyleneimine, polyallylamine, polyetheramine, polyvinylpyridine,

polysaccharides having a positively charged functionality thereon,

polyamino acids selected from:

poly-L-histidine, poly-im-benzyl-L-histidine,
poly-D-lysine, poly-DL-lysine, poly-L-lysine,
poly-ε-CBZ-D-lysine, poly-ε-CBZ-DL-lysine,
poly-ε-CBZ-L-lysine,
poly-DL-ornithine, poly-L-ornithine,
poly-δ-CBZ-DL-ornithine,
poly-L-arginine,
poly-DL-alanine-poly-L-lysine;
poly(-L-histidine, L-glutamic acid)-poly-DL-alanine-poly-L-lysine;
poly(L-phenylalanine, L-glutamic acid)-poly-DL-alanine-poly-L-lysine; or
poly(L-tyrosine, L-glutamic acid)-poly-DL-alanine-poly-L-lysine; or

random copolymers of:

L-arginine with tryptophan, tyrosine, or serine;
D-glutamic acid with D-lysine; or
L-glutamic acid with lysine, ornithine, or mixtures thereof.

8. A method according to claim 1 wherein said polycationic species is selected from polylysine or polyornithine.

9. A method according to claim 1 wherein said cells to be rendered non-adhesive are selected from islets, thyroid cells, adrenal cells, dopamine secreting cells, hepatocytes, or human T-lymphoblastoid cells sensitive to the cytopathic effects of HIV.

10. The cells produced by the method of claim 1.

11. A method to render cells non-immunogenic, said method comprising directly contacting a surface of said cells with a composition comprising a polycationic species having water-soluble polymer chains grafted thereon.

12. A method according to claim 11 wherein said polycationic species has grafted thereon at least one water-soluble polymer chain per chain of said polycationic species.

13. A method according to claim 12 wherein said water-soluble polymer is polyethylene glycol.

14. A method according to claim 11 wherein said cells to be rendered non-immunogenic are selected from islets, thyroid cells, adrenal cells, dopamine secreting cells, hepatocytes, or human T-lymphoblastoid cells sensitive to the cytopathic effects of HIV.

15. The cells produced by the method of claim 11.

16. A method for associating water-soluble polymer with a cell surface, said method comprising:

grafting water-soluble polymer onto a polycationic resin to produce a copolymer, and thereafter

directly contacting said cell surface with an effective amount of said copolymer.

17. A method according to claim **16** wherein said copolymer comprises a polycation having grafted thereon at least one water-soluble polymer chain per chain of said polycationic resin.

18. Cells having a modified cell surface which is non-adhesive with respect to mediators of immune response, wherein the surface of said cells has been modified by directly contacting said surface with a composition comprising a polycationic species having water-soluble polymer chains grafted thereon.

* * * * *

PCT WORLD INTELLECTUAL PROPERTY ORGANIZATION
International Bureau

INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification 6 : C07K 1/10, 1/13, A61K 49/00, 47/48, 9/127 — A1

(11) International Publication Number: **WO 95/06058**

(43) International Publication Date: 2 March 1995 (02.03.95)

(21) International Application Number: PCT/GB94/01844

(22) International Filing Date: 23 August 1994 (23.08.94)

(30) Priority Data:
9317618.8 24 August 1993 (24.08.93) GB

(71) Applicant *(for all designated States except US)*: ROYAL FREE HOSPITAL SCHOOL OF MEDICINE [GB/GB]; University of London, Rowland Hill Street, London NW3 2PF (GB).

(72) Inventors; and

(75) Inventors/Applicants *(for US only)*: FRANCIS, Gillian, Elizabeth [GB/GB]; Molecular Cell Pathology, Royal Free Hospital School of Medicine, Rowland Hill Street, London NW3 2PF (GB). FISHER, Derek [GB/GB]; Molecular Cell Pathology, Royal Free Hospital School of Medicine, Rowland Hill Street, London NW3 2PF (GB). DELGADO, Cristina [GB/GB]; Molecular Cell Pathology, Royal Free Hospital School of Medicine, Rowland Hill Street, London NW3 2PF (GB). MALIK, Farooq [GB/GB]; Molecular Cell Pathology, Royal Free Hospital School of Medicine, Rowland Hill Street, London NW3 2PF (GB).

(74) Agents: CRESSWELL, Thomas, Anthony et al.; J.A. Kemp & Co., 14 South Square, Gray's Inn, London WC1R 5LX (GB).

(81) Designated States: JP, US, European patent (AT, BE, CH, DE, DK, ES, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE).

Published
With international search report.
Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.

(54) Title: POLYMER MODIFICATION

(57) Abstract

A process for producing adducts of a polymer and a target material which process comprises the steps of (a) reacting either (i) an activating compound of formula (I) X-AM with a polymer of formula (II) $(C)_c$ POL - G_g so as to form (ii) a sulphonate ester-activated polymer of formula (III) $(C)_c$ POL - $(AM)_g$; (b) reacting the sulphonate ester-activated polymer of formula (III) or (III') with the target material and (c) recovering the adduct of the polymer and the target material, in which process: (i) the polymer of formula (II) is dry as determined by benzene distillation, (ii) the reaction of the compound of formula (I) or (I') with the polymer of formula (II) is conducted in an organic solvent which is inert to the reagents and to the product of formula (III) or (III') and is anhydrous as obtainable using molecular sieves of 0.3nm; (iii) the reaction of the compound of formula (I) or (I') with the polymer of formula (II) is conducted in a reaction vessel from which water is excluded; (iv) the sulphonate ester-activated polymer of formula (III) or (III') so produced is recovered and either used directly in step (b) or stored, prior to use in step (b), in the presence of a desiccating agent more hygroscopic than the product of formula (III) or (III'); and (v) the reaction of the sulphonate ester-activated polymer with the target material is conducted in a non-denaturing medium and non-denaturing temperature with respect to the target material.

FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AT	Austria	**GB**	United Kingdom	**MR**	Mauritania
AU	Australia	**GE**	Georgia	**MW**	Malawi
BB	Barbados	**GN**	Guinea	**NE**	Niger
BE	Belgium	**GR**	Greece	**NL**	Netherlands
BF	Burkina Faso	**HU**	Hungary	**NO**	Norway
BG	Bulgaria	**IE**	Ireland	**NZ**	New Zealand
BJ	Benin	**IT**	Italy	**PL**	Poland
BR	Brazil	**JP**	Japan	**PT**	Portugal
BY	Belarus	**KE**	Kenya	**RO**	Romania
CA	Canada	**KG**	Kyrgystan	**RU**	Russian Federation
CF	Central African Republic	**KP**	Democratic People's Republic of Korea	**SD**	Sudan
CG	Congo			**SE**	Sweden
CH	Switzerland	**KR**	Republic of Korea	**SI**	Slovenia
CI	Côte d'Ivoire	**KZ**	Kazakhstan	**SK**	Slovakia
CM	Cameroon	**LI**	Liechtenstein	**SN**	Senegal
CN	China	**LK**	Sri Lanka	**TD**	Chad
CS	Czechoslovakia	**LU**	Luxembourg	**TG**	Togo
CZ	Czech Republic	**LV**	Latvia	**TJ**	Tajikistan
DE	Germany	**MC**	Monaco	**TT**	Trinidad and Tobago
DK	Denmark	**MD**	Republic of Moldova	**UA**	Ukraine
ES	Spain	**MG**	Madagascar	**US**	United States of America
FI	Finland	**ML**	Mali	**UZ**	Uzbekistan
FR	France	**MN**	Mongolia	**VN**	Viet Nam
GA	Gabon				

Polymer Modification

The present invention relates to a process for direct covalent bonding of polymer moieties to target molecules in order to improve or modify the biological properties of the target molecules. The invention also relates to certain products which may be produced by this process and to intermediates useful in the process as well as to methods of use of the products of the process.

Covalent attachment of polyethylene glycol(PEG) and other polymers to proteins is well known to convey many benefits which improve the pharmacological and some physiological properties of proteins (reviewed in Nucci et al (1991) Advanced Drug Delivery Reviews, 6, 133-151; Zalipsky & Lee (1992) Biomedical Applications of Polyethylene Glycol Chemistry (ed. by J.M. Harris), Plenum, New York; Fuertges & Abuchowski, Journal of Controlled Release, 11, 139-148 1990).

There are many methods for achieving covalent coupling of polymers like PEG to proteins. All consist of a method of activating the polymer by attachment of a group or groups herein called an "activating moiety" or by coverting a terminal moiety of the polymer into an "activating moiety" and a second step where the polymer couples to the target molecule, usually via a residual portion of the "activating moiety" herein called the "coupling moiety".

Typical targets are proteins which contain one or more reactive groups on which the attachment of the coupling moiety or polymer itself can take place, such as primary and secondary amino groups, thiol groups and aromatic hydroxy groups. Alternatively, the protein molecule has been modified so that it contains suitable groups. Similar techniques are applied in coupling PEG and other polymers to other types of target molecule.

Examples of known techniques are:

Cyanuric Chloride Methods: USP 4 179 337 Davis et al; USP 4 301 144 Iwashita & Ajisaka; USP 4 261 973 Lee & Sehon; EP-A-0 098 110 Hiratani; USP 4 495 285 Shimitzu; USP 4 609 546 Hiratani; WO 86/04145 Tomasi; EP-A-0 210 761 Miyata et al; WO 90/06952 Ishikawa et al; GB 2 238 959A Sehon et al; Abuchowski et al (1977a), Journal of Biological Chemistry, **252**, 3578-3581, Abuchowski et al (1977b), Journal of Biological Chemistry, **252**, 3582-3586.

Succinimidyl Active Ester Methods: Boccu et al (1983) Z. Naturforsch, **38c** 94-99; Abuchowski et al (1984) Cancer Biochem. Biophys., **7**, 175-186; Leonard et al (1984) Tetrahedron, **40**, 1585-1590; USP 4 412 989 Iwashita et al; WO 86/04145 Tomasi; WO 87/00056 Katre & Knauf; EP-A-0 247 860 Katre et al; EP-A-0-260 098 Inada et al; WO 89/06546 Shadle et al; Katre et al (1987) Proc. Natl. Acad. Sci. USA, **84**, 1487-1491.

Carbonyldiimidazole Method: Beauchamp et al (1983) Analytical Biochemistry, **131**, 25-33; EP-A-0 154 432 Sawai et al.

Phenylchloroformate Methods: Veronese et al (1985) Appl. Biochem. Biotechnol., **11**, 141-152; WO 89/06546 Shadle et al; WO 90/15628 Groves et al.

PEG-Succinate Mixed Anhydride Methods: Ahlstedt et al (1983) Int. Arch. Allergy Appl. Immunol., **71**,228-232; Richter and Akerblom (1983) Int. Arch. Allergy Appl. Immunol, **70**, 124-131; Richter & Akerblom (1984) Int. Arch. Allergy Appl. Immunol, **74**, 36-39; Lee and Sehon (1978) Immunol. Rev, **41**, 200-247; USP 4 261 973 Lee and Sehon.

Organic Sulphonyl Halide Methods: USP 4 415 665 Mosbach & Nilsson; Delgado et al (1990) Biotechnology and

Applied Biochemistry, 12, 119-128; WO 90/04650 Francis et al; WO 90/04606 Delgado et al; WO 90/04384 Fisher.

PEG-Aldehyde Methods: Harris et al (1989) Separations Using Aqeous Phase Systems. Applications in Cell Biology and Biotechnology (ed. by D. Fisher and I.A. Sutherland), p.203. Plenum Press, London; Harris et al (1991) Water-Soluble Polymers (ed. by S.W. Shalaby, C.L. McCormick and G.B. Butler), American Chemical Society, Washington, D.C. USP 4 002 531 Royer; EP-A-0-251 304 Minami et al; WO 90/05534 Capon et al.

PEG-Maleimide and Related Methods: Goodson & Katre (1990) Biotechnology, 8, 343-346.

Phenylglyoxal Method: EP-A-0 340 741 Maeda et al.

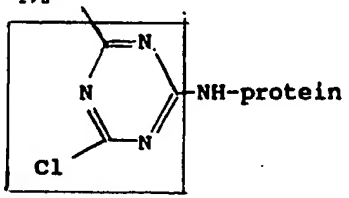
Succinimide Carbonate Method: WO 90/13540 Zalipsky; WO 91/07190 Nho et al;

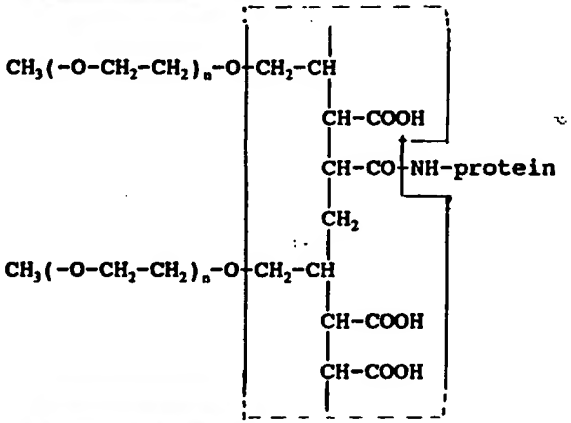
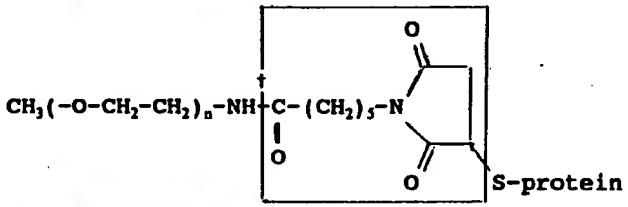
Cyanogen Bromide Method: USP 4 301 144 Iwashita & Ajisaka.

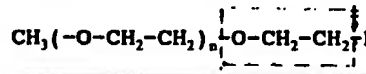
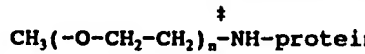
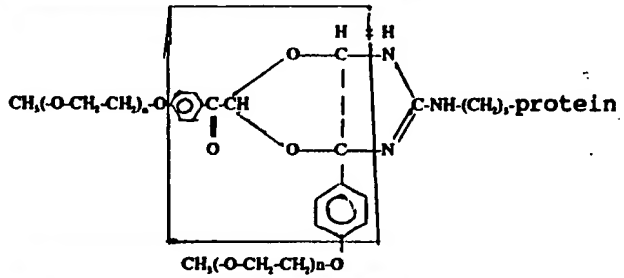
Poly-PEG Maleic Acid Anhydride Method: Yoshimoto et al (1987) Biochemical and Biophysical Research Communications, 148, 876-882.

The key features of the methods are summarised in Table 1.

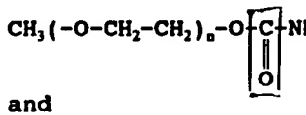
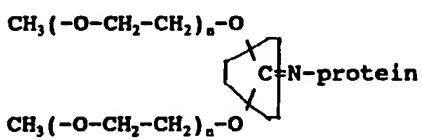
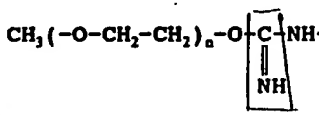
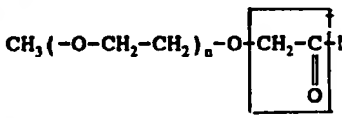
Table 1

Method	Coupling Moiety (Boxed) and general structure of adduct	Bond	Co-Product	Recommended Coupling Reaction
Cyanuric Chloride	$CH_3(-O-CH_2-CH_2)_n-O$ 		HCl	1h, RT[2],pH 9.2(3) 1h, RT, pH 9.8 (4) 1h, 37°C, pH10(5)
Succinimidyl active ester (succinimidyl succinate)	$CH_3(-O-CH_2-CH_2)_n-O-C(=O)-CH_2-CH_2-C(=O)-NH$-protein	†amide bond *ester bond	N-hydroxy-succinimide	30 min, pH 7(6) 1h, RT, pH8.25(7) 30min, RT, pH9(8)
PEG-succinate mixed anhydride	$CH_3(-O-CH_2-CH_2)_n-O-C(=O)-CH_2-CH_2-C(=O)-NH$-protein	† amide bond * ester bond	ester plus ester-modified protein	30 min, RT plus overnight 0°C pH 8.7 (9)
Phenylchloro-formates	$CH_3(-O-CH_2-CH_2)_n-O-C(=O)-NH$-protein	carbamate	substituted phenol[1]	1-5h,pH8.3-9.3(10)
Carbonyldiimi-dazole	$CH_3(-O-CH_2-CH_2)_n-O-C(=O)-NH$-protein	carbamate	imidazole	24-72h, 4°C,pH8.5 (11,12)

Method	Coupling Moiety (Boxed) and general structure of adduct	Bond	Co-Product	Recommended Coupling Reaction
Succinimide carbonate		carbamate	N-hydroxy-succinimide	30min,pH9.3 (13)
Poly(PEG-MA) anhydride		†amide bond		2h,25°C,pH8.5 (14)
PEG-maleimide		†amide bond		several hours,RT, pH5-7 (15) 2hr, RT, pH5.5 (16)

Method	Coupling Moiety (Boxed) and general structure of adduct	Bond	Co-Product	Recommended Coupling Reaction
PEG-acetaldehyde	no coupling moiety present or ethylene oxide unit 	‡ secondary amine	oxidised cyano-borohydride	Not indicated (17)
Sulphonic halogenide	no coupling moiety present 	‡secondary amine	sulphonic acid	1h,RT,pH 7.5 (18)
Phenyl glyoxal		‡secondary amine		pH8.5,7hr,RT (19)

5

Method	Coupling Moiety (Boxed) and general structure of adduct	Bond	Co-Product	Recommended Coupling Reaction
Cyanogen bromide	This process potentially provides three products  and  and 	carbamate imido carbonate -	NH_3 NH_3 None	16h,0°C,pH7.5 (20)
Amine acylation		† amide	PEG-carboxylate	3h,65°C, benzene (21)

Method	Coupling Moiety (Boxed) and general structure of adduct	Bond	Co-Product	Recommended Coupling Reaction
PEG-propion-aldehyde	$CH_3(-O-CH_2-CH_2)_n$-[S-$(CH_2)_3$-S-$(CH_2)_3$]‡-NH-protein or $CH_3(-O-CH_2-CH_2)_n$-[O-CH_2-CH_2-CH_2]‡-NH-protein	‡ secondary amine	oxidised cyano-borohydride	1H, RT, pH9 (22)

Notes

1. cf. 2,4,5-trichlorophenol from MPEG 2,4,5-trichlorophenylcarbonate; p-nitrophenol from MPEG-p-nitrophenylcarbonate.
2. Room temperature
3. Abuchowski (1977a)
4. Pyatak et al. (1980) Res, Commun. Chem. Pathol. Pharmacol., 29, 113-127.
5. Yoshimoto, et al. (1986) Jpn. J. Can. Res., 77, 1264-1270.
6. Abuchowski (1984).

Notes to Table 1 cont'd

7. Leonard (1984).

8. Katre (1987).

9. Wie et al. (1981) Int. Arch. Allergy Applied Immunol., 64,84

10. Veronese (1985).

11. Beauchamp (1983) and EP-A-O 154 432

12. Pizzo (1991) Advanced Drug Delivery Reviews, 6, 153-166.

13. Zalipsky (1992).

14. Yoshimoto (1987).

15. Aldwin and Nitecki, (1987) Analytical Biochemistry, 164, 494-501.

16. Goodson and Katre (1990).

17. Harris (1989).

18. Delgado (1990).

19. Maeda et al. (1989) EP-A-0340741

20. Iwashita et al. (1981) US-A-4301144

21. Sears (1983) EP-A-0072111

22 Harris et al. New polyethylene glycols for biomedical applications, in Shalaby SW, McCormick CL, Butler GB (eds): Water-soluble Polymers, Washington D.C., American Chemical Society, 1991.

Methods previously disclosed suffer from one or more of the following defects:

1. Substantial loss of biological activity (e.g.

20-95% loss of bio-activity) is frequently seen with the cyanuric chloride and carbonyldiimidazole methods and occasionally with phenylchloroformate and succinimidyl active ester methods.

2. The coupling of PEG (or other polymers) to proteins (or other target molecules) is, with few exceptions, in a manner which leaves part of the activating moiety, the coupling moiety, between the polymer and the target molecule. Of the above methods, only the organic sulphonyl halide methods and a PEG-acetaldehyde method (one of the PEG aldehyde methods [Harris (1989), Harris (1991)]) couple PEG directly without coupling moieties (see Table 1). With the exception of some PEG acetaldehyde methods where the coupling moiety is ethylene oxide (and thus indistinguishable from PEG itself) and the direct coupling methods above, all other coupling methods incorporate a coupling moiety distinct from the polymer and the target and are regarded herein as "indirect" coupling methods.

The incorporation of a coupling moiety generates further problems depending on the nature of the coupling moiety, thus

(i) some coupling moieties provide reactive groups capable of linking further molecules to the polymer-target construct via the coupling moiety (e.g. the triazine ring of the cyanuric chloride method, Leonard, M. et al., Tetrahedron, 40: 1585 (1984));

(ii) some coupling moieties provide an immunogenic/antigenic group (e.g. the triazine ring of the cyanuric chloride method);

(iii) some coupling moieties are potentially

toxic or are themselves of unknown toxicity but derived from a compound known to be toxic (e.g. the triazine ring of the cyanuric chloride method and reagents in the phenylchloroformate method); and

(iv) some coupling moieties provide targets for enzymatic cleavage (see below).

3. Coupling in some instances is via an unstable bond liable to be cleaved by enzymes available in serum, plasma, cells or other biological materials or by procedures applied to the polymer-target product. This has two possible deleterious consequences,

(i) the polymer-target construct is degraded enzymatically or by the conditions required for subsequent reaction steps; the former occurs with methods generating amide and/or ester bonds (see Table 1); and

(ii) removal of the polymer alters the target molecule; this occurs with some succinimidyl active ester and mixed anhydride methods,

and either or both of these can occur.

4. Many methods recommend long coupling times and/or unphysiological pH, thus rendering some target molecules less active or inactive (cf. the carbonyl-diimidazole, cyanuric chloride, phenylchloroformate and some succinimidyl active ester methods (see Table 1)).

5. Many methods use activated polymer species and/or produce co-products which are toxic in a wide range

of bioassays and which are potentially toxic in vivo if not separated from the product (e.g phenylchloroformate, cyanuric chloride methods).

6. Many methods produce products highly contaminated with either activated or inactivated polymer, causing problems in analytical methods like FPLC and toxicity in some bioassay systems (cf. the organic sulphonyl halide [Delgado (1990)] and phenylchloroformate [Veronese (1985)] methods).

7. Some methods are unsuitable for use in aqueous solution, thus limiting the target molecules to those which will tolerate non-aqueous conditions (cf. the organic sulphonyl halide method using trifluoromethanesulphonyl chloride).

8. Some of the activated polymer constructs are unstable, for instance being subject to hydrolysis during either the activation or coupling reactions (cf. the phenylchloroformate method [Veronese (1985)]). The PEG-acetaldehyde is sensitive to decomposition under basic conditions and can give irreproducible results [Harris et al. (1991)].

The present inventors have previously described PEGylation by an organic sulphonyl halide method using 2,2,2-trifluoroethanesulphonylmonomethoxy PEG (TMPEG) as follows:

1. WO 90/04606 discloses a method for fractionation of PEG-proteins formed by the TMPEG method (discussed below) and an individual adduct, PEG-gm-CSF. The fractionation method is unrelated to the present invention. The PEG-protein products of the processes disclosed in this application, and specifically disclosed materials such as

the PEG-gm-CSF adduct, are excluded from the present invention.

2. PCT WO 90/04650 discloses a method to separate DNA/protein complexes using PEG adducts formed by the TMPEG in which PEG acts as an affinity ligand. These complexes are also excluded from the present invention.

3. PCT WO 90/04384 discloses the TMPEG method for attaching PEG to liposomes. Such PEGylated liposomes are excluded from the present invention. It should be noted that the objective of coupling PEG to lipsomes in this patent was to improve half life and liposome stability.

The TMPEG method mentioned above, for instance in WO-A-90/04606, comprises activation of monomethoxy PEG (MPEG) with 2,2,2-trifluoroethanesulphonyl chloride (tresyl chloride) to produce tresyl MPEG (TMPEG) which is subsequently reacted with the target protein molecule to produce monomethoxy products. The same technique is described in WO 90/04650 for coupling monomethoxy PEG moieties to DNA/protein complexes and in WO/04384 for coupling monomethoxy PEG moieties to liposomes. Further investigation of the TMPEG method has revealed that the reactivity of the activated polymer, TMPEG, is severely impaired necessitating the use of uneconomically large ratios of TMPEG to the target molecules and has exposed the rather poor yield of the final products and the low purity thereof, necessitating extensive purification and thereby further reducing the overall yield.

The present inventors have addressed these difficulties in further research and have identified a number of factors which, in combination, contribute to the poor performance of the TMPEG process. This has allowed development of an improved technique for producing PEG adducts. The technique has been extended to include additional technical developments permitting more facile

formation of complex adducts of PEG and other polymers and the formulation of adducts of a wider range of target molecules.

The present invention relates to an improved process for producing polymer:target molecule adducts which are directly covalently linked without any intervening coupling moiety residue from the activating group on the polymer and in which the link between polymer and target moieties is non-immunogenic, non-antigenic, non-toxic and non-biodegradable, this objective being achieved by careful control of the properties of certain of the reagents and the reaction conditions. The coupling step may be performed in aqueous media and occurs rapidly thus minimising damage to fragile target species.

Accordingly the invention provides a process for producing adducts of a polymer and a target material which process comprises the steps of

(a) reacting either

(i) an activating compound of formula (I)

X-AM (I)

wherein

-AM is an activating sulphonyl ester moiety optionally bearing a group for covalent bonding to a solid support, the solvolysis substituent constant of the group -AM being less than that of the trifluoromethane sulphonate group, and

X is a leaving group

or

(ii) reacting a solid support bearing moieties of formula (I')

X-AM'- (I')

wherein

-AM'- is activating sulphonyl ester moiety covalently bound to the solid support, the group -AM'- being such that the solvolysis substituent constant of the group -AM'- is less than that of the trifluoromethane sulphonate group, and

X is as defined above

with a polymer of formula (II)

$$(C)_c\ POL - G_g \qquad (II)$$

wherein

POL is a polymer moiety of valency c+g,

C is a capping group and c is zero or a positive number and

G is a terminal hydroxyl group reactive with the compound of formula (I) and g is a positive number

so as to form

(i) a sulphonate ester-activated polymer of formula (III)

$$(C)_c\ POL - (AM)_g \qquad (III)$$

wherein

C, POL, -AM, c and g are as defined above and the group(s) -AM are linked to termini of the polymer as sulphonate esters of terminal hydroxyl groups

or (ii) a solid support-bound, sulphonate ester-activated polymer of formula (III')

$$[(C)_c\ POL-\ (AM')_g]_z \qquad (III')$$

SS

wherein

C, POL, -AM'-, c and g are as defined above,

SS is a solid support and z is the number of sulphonate ester-activated polymer moieties on the solid support

and the groups -AM'- are linked to the termini of the polymer as sulphonate esters of terminal hydroxyl groups,

and, when -AM bears a group for covalent bonding to a solid support, reacting the sulphonate ester-activated polymer of formula (III) with a solid support to form a solid support-bound, sulphonate ester-activated polymer of formula (III') as defined above

(b) reacting the sulphonate ester-activated polymer of formula (III) or (III') with the target material and

(c) recovering the adduct of the polymer and the target material,

in which process:

(i) the polymer of formula (II) is dry as determined by benzene distillation,

(ii) the reaction of the compound of formula (I) or (I') with the polymer of formula (II) is conducted in an organic solvent which is inert to the reagents and to the product of formula (III) or (III') and is anhydrous as obtainable using molecular sieves of 0.3nm;

(iii) the reaction of the compound of formula

(I) or (I') with the polymer of formula (II) is conducted in a reaction vessel from which water is excluded;

(iv) the sulphonate ester activated polymer of formula (III) or (III') so produced is recovered and either used directly in step (b) or stored, prior to use in step (b), in the presence of a desiccating agent more hygroscopic than the product of formula (III) or (III'); and

(v) the reaction of the sulphonate ester-activated polymer with the target material is conducted in a non-denaturing medium and non-denaturing temperature with respect to the target material.

The compounds of formula (I) and solid supports bearing moieties of formula (I'), the polymer moiety POL in the polymers of formulae (II), (III) and (III'), the sulphonate ester-activating moieties -AM and -AM'-, the reactive groups X and G and the capping groups C will be described in more detail below. First, some variants of the overall process will be described:

In general the process of the invention is conducted in the liquid phase, using a compound of formula (I) in step (a), in solvents and reaction media as defined above. However it is also possible to conduct the reaction at a solid:liquid interface by using a solid support-bound, sulphonate ester-activated polymer of formula (III'). In this latter case the reaction can be conducted on, for instance, a column of solid support-bound sulphonate ester-activated polymer with other reagents and reaction media being passed through the column.

The objective of performing the reaction on a solid support is that although the target is exposed to a molar excess of sulphonate ester-activated polymer, only those polymer moieties which become attached to the target are eluted from the solid support and the potentially toxic co-product remains attached to the column. The flow rate and column length provide a means of controlling the degree of modification. Column media can also be selected to achieve differential elution of targets modified to different extents.

Binding of the sulphonate ester-activated polymer to the solid support is achieved via the activating ester-sulphonyl moiety -AM in one of two ways:

1. The process is conducted using a compound of formula (I) which is an activating sulphonyl compound having a binding substituent for later linking to the solid support. In this variant, the reaction between the compound of formula (I) and the polymer of formula (II) is conducted in the solution phase and is followed by the step of binding the product of formula (III) to the solid support. The reaction in step (b) between the solid support-bound, sulphonate ester-activated polymer of formula (III') and the target material is then performed at the solid:liquid interface.

2. The process is conducted using a solid support bearing activating sulphonyl moieties of formula (I') in step (a). In this case the reaction of the compound of formula (I') with the polymer material of formula (II) is conducted at the solid:liquid interface and directly forms the solid support-bound, sulphonate ester-activated polymer of formula (III'). The solid support bearing moieties of formula (I') is produced by reacting a compound of formula (I) or a precursor therefor which bears a group for covalent bonding to a solid support with the solid support

as a preliminary to step (a) of the present process. Step (b) is again conducted at the solid:liquid interface as in (1) above.

The benefit of conducting the reaction(s) at a solid:liquid interface is primarily seen in the greater purity of the products since unreacted sulphonate ester-activated polymer is left on the solid support as are the reaction products other than the polymer:target adduct.

The present invention therefore provides the following particular embodiments of the process:

1. A process as described above comprising the steps of reacting a compound of formula (I) with a polymer of formula (II) in the liquid phase to produce a sulphonate ester-activated polymer of formula (III) and reacting the sulphonate ester-activated polymer with the target material in the liquid phase.

2. A process as described above comprising the steps of reacting a compound of formula (I) wherein -AM is an activating sulphonyl moiety having one or more groups for covalent bonding to a solid support with a polymer of formula (II) in the liquid phase, coupling the thus-produced sulphonate ester-activated polymer to a solid support material <u>via</u> the binding groups of the moieties -AM and reacting the target material with the thus-produced solid support-bound, sulphonate ester-activated polymer. In this embodiment step (c) is achieved when the adduct is released from the solid support, eluted and thus recovered.

3. A process as described above comprising the steps of reacting a solid support bearing moiety of formula (I') with a polymer of formula (II) so as to form a solid support-bound, sulphonate ester-activated polymer of

formula (III') and reacting the solid support-bound, sulphonate ester-activated polymer with the target material.

In further variants of the process of the invention, which can be conducted in conjunction with any of the foregoing variants, the proportion of the groups -AM on the sulphonate ester-activated polymer which react with the (initial) target material is controlled such that in at least a proportion of the molecules of polymer:target adduct produced there remain unreacted activating sulphonyl moieties -AM. Such unreacted reactive groups -AM may then be reacted with one or more different further target materials so as to form materials polymer:[target]$_n$ wherein n is 2 or more and the initial and further target entities are different; or they are reacted with more of the initial target material so as to form materials polymer:[target]$_n$ wherein the target entities are all the same; or they are reacted with further unreacted groups in the initial target entity of the polymer:target adduct (for instance under conditions which hinder intermolecular reactions, such as high dilution) such that the polymer moieties are bonded at two or more positions to the target entity.

It will be appreciated that, since the polymer and/or the target materials may be multivalent, it is possible by the process of the invention to produce a variety of polymer:target structures. By way of example, a univalent polymer and univalent target produce 1:1 adducts; a bivalent target and a univalent polymer may form adducts wherein the target entities bear two polymer moieties whereas a bivalent polymer and a univalent target may produce species where two target entities are linked to a single polymer moiety; use of higher-valent polymers can lead to the formation of clusters of target entities bound to a single polymer moiety whereas higher-valent targets may become encrusted with a plurality of polymer moieties.

In general the target moieties are likely to have more than one reactive group which will react with the activated polymer and the possibility of forming complex structures must always be considered; when it is desired to form simple structures such as 1:1 adducts of polymer and target, or to use bivalent polymers to form target:polymer:target adducts, it will be necessary to use predetermined ratios of activated polymer and target material, predetermined concentrations thereof and to conduct the reaction under predetermined conditions (such as duration, temperature, pH etc.) so as to form a proportion of the described product and then to separate the described product from the other reaction products.

The necessary reaction conditions, proportions and concentrations of the reagents can be obtained by relatively simple trial-and-error experiments with appropriate scaling-up as necessary. It will be appreciated that molar proportions and the concentrations of individual reagents may need to be adjusted on scaling up compared with the optimal molar proportions and concentrations identified at the laboratory bench scale for production of a particular product; this may also require relatively simple trial-and-error experimentation. Purification and separation of the products is similarly achieved by conventional techniques well known to those skilled in the art.

The present invention therefore provides the following particular embodiments of the process:

1. A process as described above comprising, in step (b), reacting, in predetermined molar ratio and at predetermined concentrations, sulphonate ester-activated polymer having two moieties -AM with a first target material, so as to produce a sulphonate ester-activated 1:1 adduct of polymer and target material, then reacting the

1:1 adduct with a second target material so as to produce a target^1:polymer:target^2 adduct, wherein the first and second target materials may be the same or different, and then recovering the adduct in accordance with step (c).

2. A process as described above comprising, in step (b), reacting, in predetermined molar ratio and at predetermined concentrations, sulphonate ester-activated polymer having only one moiety -AM or -AM'- with a target material having more than one reactive group so as to form an adduct of the polymer and target having a preselected number of polymer molecules per molecule of target or, especially for macromolecular targets having a large number of reactive groups, so as to form an adduct in which a preselected proportion of the reactive groups have been reacted with and linked to polymer molecules, and then recovering the adduct in accordance with step (c). The preselected number may be, for instance from 1 to 10, preferably from 1 to 5, for example 1, 2, 3 or 4. The preselected proportion may be, for instance from 1 to 100 %, preferably from 5 to 95 %, for example, 10, 20, 30, 40, 50, 60, 70, 80, or 90%.

3. A process as described above comprising, in step (b), reacting, in predetermined molar ratio and at predetermined concentrations, sulphonate ester-activated polymer having two or more activating sulphonyl moieties -AM with a target material having two or more reactive groups so as to produce a sulphonate ester-activated 1:1 adduct of polymer and target then changing the reaction conditions to hinder intermolecular reactions whilst permitting intramolecular reactions between groups -AM on the polymer and reactive groups on the target so as to form adducts of polymer and target having two or more covalent bonds between the polymer and target moieties, and then recovering the adduct in accordance with step (c).

These process variants may each be used in conjunction with any of the process variants described earlier relating to liquid phase and solid:liquid phase interface reactions.

The reagents used in the process of the invention will now be described starting with the compounds of formula (I):

ACTIVATING COMPOUNDS OF FORMULA (I) and SOLID SUPPORTS BEARING MOIETIES OF FORMULA (I')

The leaving group X is intended to react with groups G on the polymer of formula (II) and, in the broadest sense, may be selected from any of the known leaving groups which will undergo such a reaction. However it is generally preferred that X is a halogen and most preferably X is chlorine.

Activating moieties, -AM and -AM'- are sulphonyl-type activating groups, and optionally have a binding substituent for subsequent linking to a solid support or are attached to a solid support. The groups -AM will be described below in general, followed by further information on binding substituents and linkage to solid supports.

The activating moieties -AM are moieties having the following properties:

1. They are sulphonyl groups; the derived sulphonate esters are a large class of compounds with a broad range of solvolytic activities.

2. They have appropriate electron withdrawing groups on the sulphur. The suitability of such groups can be estimated by linear free energy relationship plots. It has been observed [Crossland et al (1971) J.Amer.Chem.Soc.,

93, 4217-4219] that substituent constants may be applied to the reactivity of groups such as 2,2,2-trifluoroethane-sulphonate (tresylate), toluenesulphonate (tosylate), and methanesulphonate (mesylate) groups; there is a correlation observed in a Hammett plot between the rates of solvolysis of sulphonate ester and the nature of the substituent on the sulphur and although this correlation is only approximate, it allows the predication of gross effects of various sulphonyl substituents on solvolytic reaction rates. This technique provides a distinction between those sulphonate ester groups which are too highly reactive to be of use in the process of the present invention (i.e. those having a substituent constant or solvolysis rate equal to or greater than that of the trifluoromethane sulphonate (triflate) group) and those which are of use and provides a useful means of preliminary selection within the latter. Substituent constants must be less than the values for the trifluoromethyl group in trifluoromethanesulphonates, preferably they are equal to or greater than the values of the tosyl group in tosylates [Crossland et al (1971)]. This can for example be achieved by the inclusion of fluorine atoms in alkyl substituents as in 2,2,2-trifluoroethane-sulphonate (tresyl) esters. By selecting -AM from compounds having this range of substituent constants, one is selecting reagents with a predetermined range of reactivities. This gives a means of predicting: a) the rate of the coupling reaction and b) the tendency of -AM to undergo hydrolysis in aqueous solution. It is important that the two rates are below that of triflate and preferably equal to or above that of tosylate since, if the reactivity is too low, the coupling time will be long with potential damage to the target and if it is too high, hydrolysis will compete significantly with the coupling reaction and may preclude its occurring adequately in aqueous solution.

If the target molecule is one that can withstand

organic solvents these may be used for the coupling reaction. However, where the target molecule can withstand a slow coupling reaction then compounds with lower Hammett substituent constants than the range given above can be used.

3. They contain no groupings more susceptible to nucleophilic attack than the terminal carbon atom of the polymer moiety for instance PEG, or equivalent atom of any other polymer moiety (i.e. the carbon or equivalent atom bonded to the oxygen of the sulphonate group of the group -AM). The consequence of this is that no "coupling moiety" (i.e. residual part of the activating moiety) lies between the polymer and the target molecules.

4. The compounds from which the groups -AM are derived should preferably be stable.

5. To minimise toxic effects, the groups -AM and the compounds from which they are derived should preferably be of low toxicity <u>in vitro</u> and <u>in vivo</u>.

6. The compounds from which the groups -AM are derived should be readily separated from the product of formula (III).

Preferred groups -AM are:

2,2,2-trifluoroethanesulphonyl,
pentafluorobenzenesulphonyl,
fluorosulphonyl,
2,4,5-trifluorobenzenesulphonyl,
2,4-difluorobenzenesulphonyl,
2-chloro-4-fluorobenzenesulphonyl,
3-chloro-4-fluorobenzenesulphonyl,
4-amino-3-chlorobenzenesulphonyl,
4-amino-3-fluorobenzenesulphonyl,

o-trifluoromethylbenzenesulphonyl,
m-trifluoromethylbenzenesulphonyl,
p-trifluoromethylbenzenesulphonyl,
2-trifluoromethoxybenzenesulphonyl,
4-trifluoromethoxybenzenesulphonyl, and
5-fluoro-2-methylbenzenesulphonyl groups.

The most preferred group -AM is 2,2,2 trifluoroethane-sulphonyl.

It should be appreciated that the definition of the activated polymers used in the present invention excludes certain sulphonic acid esters of polymers which have previously been used in "active ester" methods of PEGylation such as the ester between the carboxylic acid of the polymer and the hydroxyl of 4-hydroxy-3-nitrobenzene sulphonic acid described in Katre et al.(1987).

The binding substituents for linking the group -AM to a solid support are suitably groups which can be coupled to conventional solid support materials, optionally via a conventional spacer moiety, by well known techniques. A preferred binding substituent is an aminophenyl group which can be coupled to a solid support via the amino substituent. Preferred compounds of formula (I) for binding to solid supports are therefore sulphonyl halides having an aminophenyl group bound to the sulphur atom, possibly via other moieties, such as 2',3',5',6'-tetra-fluoro-4-amino-phenyl-azobenzene-4'-sulphonic halides, especially the chloride.

Solid support materials which may be used in the process of the invention are entirely conventional and well known to those skilled in the art. It is preferred that the solid support is selected from silica, silconised glass, agarose, Sepharose, polystyrene divinyl benzene copolymer and polyacrylamide.

Compounds of formula (I) and solid supports bearing groups of formula (I') may be produced by conventional techniques well known to those skilled in the art. Many of these compounds are commercially available.

Compounds of formula (I) which are intended for linking to solid supports are also readily available or are produced by conventional techniques; they may be coupled to solid supports by conventional techniques optionally with introduction of spacer groups. Alternatively, in view of the reactivity of sulphonyl halides, it may be preferred to couple a precursor, such as a sulphonic acid, of the compound of formula (I) with the solid support or reagents for introducing a spacer group then to convert the bound precursor to the sulphonyl halide group.

An example of a compound of formula (I) bearing a group for covalent bonding to a solid support is tetrafluoro-4-amino-azobenzene-4'-sulphonyl chloride which can be generated in a three step procedure as described by Scouten et al (1991) Journal of Chromatography, **376**, 289-298 as follows:-

1. Tetrafluorosulphanilic acid can be prepared from tetrafluoroaniline.

2. Tetrafluoro-4-amino-azobenzene-4'-sulphonic acid is prepared from tetrafluorosulfanilic acid by diazotisation and reaction with aniline.

3. The sulphonic acid is converted to the sulphonyl chloride by drying with thionyl chloride and then grinding with phosphorus pentachloride and phosphorus oxychloride.

Coupling of compounds of formula (I) bearing moieties -AM having solid support binding groups or precursors thereof are coupled to a solid support, for instance by

reacting the compound of formula (I) with the solid support, with a spacer group on the solid support, or with reagents to introduce a spacer group and coupling the spacer group to the solid support. There are many possible compounds suitable for use in forming spacer groups. The spacer needs to be inert and not damaging to the target material in the context of the complete solid-supported reagent since, for instance, polymer modification may alter the properties of the solid support. The spacer needs to conserve the electron withdrawing groups giving -AM'- an appropriate substituent constant as defined for soluble -AM polymer constructs. It is particularly important to avoid groups susceptible to nucleophilic attack. The selection of the spacer will also depend on the support selected and the properties defined above. The group on the sulphonyl activating moiety -AM for covalent bonding to the solid support will be capable of reacting with a reactive group on the solid support or spacer and will be chosen depending on the nature of the chosen solid support and any spacer group.

For instance, solid supports bearing aldehyde groups are reacted with an amino group on the compound of formula (I) in the presence of a non-nucleophilic base such as lithium isopropylamide so as to form a Schiff's base, followed by reduction of the double bond, for instance using an appropriate borohydride.

Suitable precursors of the compounds of formula (I) are readily available or can be produced by conventional techniques. Suitable solid support materials are also readily available; those which do not have groups capable of linking the precursor of the compound of formula (I) may readily be modified by conventional techniques in order to introduce the necessary functionalities, for instance siliconised glass (prepared as described by Mohr and Pommerening (1985) Affinity Chromatography, Practical and Theoretical Aspects, Marcel Dekker, Inc, New York and

Basel) is activated using glutaraldehyde [Weston & Avrameas (1991) Biochemical and Biophysical Research Communications, 45, 1574-1580].

The compounds of formula (I) and solid supports bearing groups of formula (I') are readily hydrolysed and extremely labile and are preferably used when freshly prepared or, after preparation, are stored in air-tight containers such as glass ampoules prior to use.

POLYMERS OF FORMULA (II)

The polymers of formula (II) used in the present invention are all based on known and readily available polymers which generally already contain at least one group G, reactive with the group X of the compound of formula (I). As polymers are almost inevitably mixtures, the value of g will be an average for the material as a whole but is preferably nearly or, more preferably, exactly integral, preferably with a high degree of homogeneity. For polymers which have two or more reactive groups G it may be necessary or desirable to prevent reaction at a proportion of such groups by blocking them with a capping group C. The number of capping groups will also be an average for the material as a whole and is preferably nearly or, more preferably, exactly integral, or is zero when no capping groups are required. The polymers, reactive groups G and capping groups C will be further described below.

The polymers that can be used are selected from the following which are all readily available to those skilled in the art:

1. Homo- and heteropolymers, i.e. polymeric substances with repeating identical or non-identical subunits (homo-polymers and heteropolymers respectively) such as:

(i) Polyalkylene compounds; for example

a), polyalkylene oxides and glycols and their derivatives such as poly(oxymethylene), polyethyleneglycols and oxides and methoxypolyethyleneglycols and related homopolymers, such as polymethylethyleneglycol, polyhydroxypropyleneglycol, polypropyleneglycols and oxides, polymethylpropyleneglycol, and polyhydroxypropyleneoxide, which may be straight-chain or branched polymers (for example straight-chain polypropyleneglycols and branched-chain polypropyleneglycols) and derivatives of the above including ethers, for instance of polyethyleneglycol or polypropyleneglycol such as the monomethyl ethers, monocetyl ethers, mono-n-butyl ethers, mono-t-butylethers and monooleyl ethers, esters of polyalkyleneglycols with carboxylic acids such as the monobutyl esters and monostearyl esters, and dehydration condensation products of the polyalkyleneglycols with amines such as propylamine and stearyl amine;

b) polyvinyl compounds such as poly(vinylpyrrolidone), polyvinyl alcohol, poly(vinyl acetate) and the copolymer poly(vinyl acetate-co-vinyl alcohol),poly(vinyloxazolidone),poly(vinylmethyloxazolidone) and poly(vinyl methyl ether);

c) polyacrylic compounds such as poly (acrylic acid)s, poly(methacrylic acid)s, polyhydroxyethylmethacrylates, their amides such as poly(acrylamide) and poly(methacrylamide) and N-substituted derivatives of the amides such as poly(N,N-dimethylacrylamide), poly(N-isopropylacrylamide), poly(N-acetamidoacrylamide) and poly(N-acetamidomethacrylamide;

d) polyionic compounds such as poly(ethyleneimine), poly(ethylsulphonic acid), poly(silicic acid), poly(styrenesulphonic acid), poly(vinyl amine), poly(2-vinylpyridine) and its N-alkyl derivatives, poly-(4-vinylpyridine) and its N-alkyl derivatives, poly-(vinylsulphuric acid), poly(vinyl alcohol-co-vinyl

sulphuric acid), poly(diallyldimethylammonium chloride), poly[(dimethylimino) trimethylene(dimethylimino)hexamethylene dibromide)], poly(ethylenephosphonic acid), poly(maleic acid), poly(2-methacryloyloxyethane-1-sulfonic acid), poly(3-methacryloyloxypropane-1-sulfonic acid), poly(4-vinylbenzoic acid); poly(4-vinylbenzyltrimethylammonium), poly[3-(vinyloxy)propane-1-sulphonic acid)], poly(4-vinylphenol), (poly[p-hydroxystyrene]), poly(4-vinylphenyl sulphuric acid), poly(2-vinylpiperidine), poly(4-vinylpiperidine); poly(N-vinylsuccinamidic acid) and ionizable synthetic copolymers;

e) polyalkylene polyols such as polyoxyethylated glycerol, polyoxyethylated sorbitol (e.g polysorbates and polyoxyethylated glucose; and

f) non-ionic surfactants such as polyoxyethylenealkylphenols (including Tritons), polyoxyethylenemercaptans, polyoxyethylenealkylamines and polyoxyethylenealkylamides;

(ii) Polyamino acids or synthetic polypeptides such as, for example, polymers of D-glutamic acid and D-lysine, polylysine, polyalanine, polyglutamic acid, polyaspartic acid and polyproline;

(iii) Polysaccharides, crosslinked products thereof and polysaccharide containing material including branched or unbranched polysaccharides, comprising saccharide monomers such as glucose, mannose, galactose, fucose, fructose, xylose, arabinose, glucuronic acid, sialic acid (neuraminic acid), galacturonic acid, mannuronic acid, D-glucosamine and galactosamine, which may be homopolysaccharides or

heteropolysaccarides, such as

a) dextran and dextran derivatives including dextran sulphate, p-aminoethyl cross-linked dextran, and carboxymethyl dextran;

b) cellulose and cellulose derivatives including methyl cellulose and carboxymethyl cellulose;

c) starches (amylopectin and amylose) and dextrins derived from starch, hydroxyethyl starches, agarose, ficoll or its carboxy methyl derivatives;

d) glycosaminoglycan chains of proteoglycans such as hyaluronic acid, chondroitin sulphates, dermatan sulphate, heparin, heparin fragments, heparin oligosaccharides, heparan sulphate and keratan sulphate;

e) carbohydrate-containing side chains of glycoproteins and glycolipids such as gangliosides, globosides and sulphatides;

f) polymers of sugar alcohols such as polysorbitol and polymannitol; and

g) other polysaccharides such as glycogen, glucans (e.g. laminaran), glycosaminoglycans, polysaccharide sidechains of glycoproteins or glycolipids, algal polysaccharides (e.g. alginic acid or polymannuronic acid and sulphated polysaccharides such as carrageenan and agar), pectins, plant gums, seed mucilages such as guaran, bacterial and fungal polysaccharides (e.g. xanthans, gellan, alginate, scleroglucan, schizophyllan, curdlan and pullulan);

(iv) other organic polymers including polymers and copolymers of, for instance, amines, olefins, esters, acetal, polyamides, carbonates, ethers, phenylene sulphides, silicones, urea formaldehyde condensation products, phenol formaldehyde condensation products, urethanes,

melamine formaldehydes, epoxy resins, acrylic resins, allyl resins, polyacrylic acid and carbomers; and

(v) inorganic polymers especially those inorganic polymers containing organic moieties, for example, silicates.

2. Block copolymers, i.e. copolymers formed by combining appropriate blocks of the above polymers and include for instance block co-polymers of small alkoxymonomers, e.g. polyethylene/polypropyleneglycol (over 30 polyoxyethylene-polyoxypropylene copolymers are available on the market); block copolymers of ethylene and maleic anhydride; block copolymers of polyalkylene glycols and polyvinylpyrrolidone or polyvinyl alcohol; block copolymers of polyoxyethylene and polyoxy-propylene (Pluronics); block copolymers of the ethers, esters or dehydration condensation products of polymers of ethylene glycol and propylene glycol; and block copolymers of acrylamide and acrylic acid.

Typically the polymer will be water soluble. The polymer is preferably of very low toxicity in vivo and in vitro, since many applications involve administration to man or animals and/or exposure to cells in cell culture systems. The polymer length is not restricted in this invention, since it will depend on the principal use of the product (e.g. short lengths may be best for coupling two proteins together and longer polymers for improving plasma half life). With each application optimum polymer length must be selected either empirically or by reference to the desired application. The polymer's own inherent hydrophobicity is also important in some settings and will have to be evaluated on a case-by-case basis.

The reactive groups G are terminal hydroxyl groups. Depending upon the selected polymer such groups G may already be available for reaction or it may be necessary to introduce groups G by conventional techniques in a preliminary step. Generally groups G will be groups bonded to carbon atoms of the polymer. The groups G must be capable of reacting with the group X of the compounds of formula (I). The groups G will be selected such that they ultimately permit formation of the desired non-immunogenic, non-antigenic, non-toxic, non-biodegradable direct covalent link between the polymer and target. Preferred groups G are primary ($-CH_2OH$) or secondary (-CHOH) alcoholic hydroxyls for instance primary hydroxyls as found at the termini of polyalkylene glycols such as in PEG. Such hydroxyls react with sulphonyl halides and other activating compounds of formula (I) to form activating sulphonate ester moieties.

The use of capping groups C is an important feature of the reaction since this embodiment of the invention has special advantages discussed further below. The function of the capping groups C is to protect one or more reactive groups G of the polymer molecule from nucleophilic attack while leaving the activated polymer product susceptible to nucleophilic attack only at the carbon or equivalent atom adjacent to the groups -AM. C therefore must lack the properties of -AM and should preferably be an inert group with respect to reactivity with other molecules and should be of low toxicity. Suitable groups C are well known to those skilled in the art as are techniques for introducing such groups. A preferred group C is methyl.

Production of the polymers for use in the process of the invention may be achieved by conventional techniques although most materials will be obtained commercially, possibly then being modified to introduce the desired reactive groups G and/or capping groups C as mentioned

above.

A preferred polymer for use in accordance with the present invention is a PEG polymer $HO-(CH_2CH_2O)_x-H$ where x is large enough for the molecular weight to be in 150(x=3), 194(x=4), 238(x=5), 282(x=6) or above, for instance about 500, 1000, 2000, 3000, 4000, 5000, 6000 or 10000 which has two reactive groups G, i.e. the hydroxyl groups. The size of the polymer actually used will be selected according to the desired properties of the end product.

Another preferred polymer is MPEG (i.e. the polymer $MeO-(CH_2CH_2O)_x-H$ which has one capping group C, i.e. the methyl group and one reactive group G, i.e. the hydroxyl group) where x is 3, 4, 5 or 6 or is large enough to provide molecular weights of, for instance, about 500, 1000, 2000, 3000, 4000, 5000, 6000 or 10000. Branched PEGs can also be used.

Since conventional polymerisation techniques generally produce materials which are mixtures, in certain cases some purification may be required before the polymer is used in the process of the invention, for example, some preparations of MPEG are significantly contaminated with PEG. This would lead to the production of biactivated PEG and crosslinking on subsequent use and needs to be avoided for many applications. Such contaminated material can be identified on the basis of its size distribution (polymerisation occurs at both ends of the molecule for PEG hence the contaminant has circa twice the molecular weight). Size fractionation should therefore be used to remove this PEG from MPEG preparations prior to activation: gel permeation chromatography and other appropriate methods may be used. For example, the divalent PEG can be separated from the bulk MPEG using vesicle chromatography [Selisko et al (1993) J. Chromatogr. **641**, 71-79].

TARGET MATERIALS

Suitable target materials to which polymer can be attached in accordance with the present invention are all materials having biological activity which are useful in, for instance diagnosis or therapy and which are all well-known to those skilled in the art. They all contain at least one reactive group (hereinafter referred to as groups "N") containing an atom which is capable of mounting a nucleophilic attack on the carbon or equivalent atom of the polymer adjacent to the group AM. Examples of the reactive group include primary and secondary amino groups, thiol groups and aromatic hydroxy groups.

More specifically, potential targets include proteins, peptides, amino acids and their derivatives such as: antibodies and fragments thereof; cytokines and derivatives or fragments thereof, for example, the interleukins (IL) and especially the IL-1, IL-2, IL-3, IL-4, IL-5, IL-6, IL-7, IL-8, IL-9, IL-10 and IL-11 subtypes thereof; colony stimulating factors, for example granulocyte-macrophage colony stimulating factor, granulocyte-colony stimulating factor (alpha and beta forms) and macrophage-colony stimulating factor (also known as CSF-1); haemopoietins, for example erythropoietin, haemopoietin-alpha and kit-ligand (also known as stem cell factor or Steel factor); interferons (IFNS), for example IFNalpha, IFNbeta and IFNgamma; growth factors and bifunctional growth modulators, for example epidermal growth factor, platelet derived growth factor, transforming growth factor (alpha and beta forms), amphiregulin, somatomedin-C, bone growth factor, fibroblast growth factors, insulin-like growth factors, heparin binding growth factors and tumour growth factors; differentiation factors and the like, for example macrophage differentiating factor, differentiation inducing factor (DIF) and leukaemia inhibitory factor; activating factors, for example platelet activating factor and macrophage activation factor; coagulation factors such as

fibrinolytic/anticoagulant agents including heparin and proteases and their pro-factors, for example clotting factors VII, VIII, IX, X, XI and XII, antithrombin III, protein C, protein S, streptokinase, urokinase, prourokinase, tissue plasminogen activator, fibrinogen and hirudin; peptide hormones, for example insulin and calcitonin; enzymes such as superoxide dismutase, glucocerebrosidase, asparaginase and adenosine deaminase; vaccines, for example hepatitis-B vaccine, malaria vaccine, melanoma vaccine and HIV-1 vaccine; transcription factors and transcriptional modulators; carbohydrates, glycosoaminoglycans, glycoproteins and polysaccharides; lipids, for example phosphatidyl-ethanolamine, phosphatidylserine and derivatives thereof; sphingosine; steroids such as cholesterol and derivatives thereof; nucleotides, nucleosides, heterocyclic bases, DNA, RNA, synthetic and non-synthetic oligonucleotides including those with nuclease resistant backbones; vitamins; antibiotics; bacteristatic and bactericidal agents; antifungal, anthelminthic and other agents effective against infective agents including unicellular pathogens; small effector molecules such as noradrenalin, alpha adrenergic receptor ligands, dopamine receptor ligands, histamine receptor ligands, GABA/benzodiazepine receptor ligands, serotonin receptor ligands, leukotrienes and tri-iodothyronine; cytotoxic agents such as doxorubicin, methotrexate and derivatives thereof.

The target molecules may also be part of larger multi-molecular structures. These include cells or parts thereof, for instance erythrocytes, erythrocyte "ghosts" and leukocytes, liposomes such as multilamellar vesicles and unilamellar vesicles, micelles and micelle-like structures, and aggregates, microemulsions, coacervates, emulsions, suspensions of the foregoing.

It will be appreciated that when the target molecules are part of such structures there will generally be many

target molecules in each structure; treatment according to the invention will therefore produce a structure bearing many polymer moieties. Where the polymers are bi- or multi-valent, reaction with a multimolecular target may result in intermolecular cross-linking by the polymer between molecules of the same target structure and/or between molecules of different target structures as well as intramolecular bonding of the polymer to more than one position on the same molecule of a target structure.

It is evident from the inventors' investigation that much of the loss of biological activity frequently observed with prior polymer coupling methods is due to inappropriate coupling reactions (i.e. reactions taking place at sites which disable the target's biological activity), coupling conditions and/or contaminating toxic material reducing responses in bioassays. The present process provides a means of generating adducts of polymer and target with highly conserved biological activity for the majority of molecules, or even enhanced biological activity. In the event of unusually substantial loss of biological activity, a search must be made using fractionated material with different degrees of substitution and appropriate mapping (e.g. peptide mapping) to identify the group or groups N the modification of which by polymer is responsible for lost activity. The situation can then be remedied either by modifying the group N to abrogate coupling of polymer at that site or by shielding N with an appropriate non-covalent bond (examples include hydrogen bonding of base pairs for DNA and protein/protein binding like receptor ligand interactions). Two alternative strategies are available depending on the nature of the critical N group, in particular whether there are significant differences in the susceptibility of the group compared to the other such groups (either being more or less susceptible) to coupling to the polymer. If the group N is less susceptible the coupling conditions (usually the coupling ratio) can be

altered so that the critical group N is rarely modified. If it is more susceptible, a two step procedure where short polymer molecules are first linked to more accessible (susceptible) sites (i.e. including the group(s) N) then long polymer molecules are linked to the remaining sites may prove acceptable, the outcome depending on the nature of the problem at the N site with respect to biological activity.

Targets lacking a reactive group may be modified so as to create one or more reactive groups; this is within the ability of those skilled in the art and can be achieved by well-known techniques.

Some target structures (e.g. RNA and single stranded DNA) pose special problems because they provide too many "N" groups to which the polymer would attach in a standard reaction. There the groups N may be temporarily protected by involvement in an appropriate conformation precluding the nucleophilic attack, as for example in the hydrogen bonding associated with base pairing of DNA (see below).

An embodiment of the present process involves site-specific modification of DNA, RNA and synthetic oligonucleotide targets (or of any molecule containing an amino or other reactive group which can participate in interactions such as hydrogen bonding with another molecule or compound) by precluding the nucleophilic attack on the activated polymer species by reactive groups on the target. The bases adenine (A), cytosine (C) and guanine (G) [but not uracil (U) or thymine (T)] provide suitable targets in DNA, RNA and synthetic oligonucleotides for modification with polymer moieties according to the invention and thus these are special targets with the problem that there are too many available reactive groups to which the polymer can be attached. As shown below, single stranded DNA is rapidly and very heavily modified by activated PEG (TMPEG).

By using various restriction fragment DNA cleavage sites as a model system, the present inventors have shown

that selected bases A, C or G can be modified by the expedient of leaving short stretches (e.g. 2-4 bases) single stranded. Adenine bases appear to be the most susceptible to such modification. Blunt ended double stranded DNA is not readily coupled under the conditions described, indicating that hydrogen bonding between base pairs is sufficient to preclude interaction of the amino groups of A, C and G bases with the activated polymers.

Site-specific DNA modification by polymer can be achieved by the expedient of including one or more A, C or G bases in a short single stranded section of DNA by appropriate restriction enzyme digestion or by hybridising oligonucleotides of dissimilar lengths with the DNA to protect bases which are not to be modified or by exploiting the natural strand asymmetry of polymerase chain reaction products which have a one base-pair overhang, or by exploiting localised regions of single strandedness achieved by natural or artificial localised melting of the double helix.

THE PROCESS

The process of the present invention relies upon conducting steps (a) and (b) in accordance with certain constraints as defined above. In particular, step (a) must be conducted using dry polymer, dry solvents and with water being excluded from the reaction vessel. Dryness of the polymer may be determined by benzene distillation as described below. If the polymer is not sufficiently dry, interfering side reactions occur making it difficult to obtain economical amounts of the final adduct. Likewise, wet solvents and ingress of water during the reaction will also cause interfering side reactions. Suitably dry solvents are obtained using molecular sieves (0.3nm) as described below. Exclusion of water from the reaction vessel can be achieved by conventional techniques.

Benzene distillation

The principal exploited here is that the water-benzene azeotrope has a boiling point of 65°C and that after water has been removed from a sample, the distilling temperature rises to that of pure benzene (i.e 79 to 80°C). In addition, the water-benzene azeotrope is cloudy and benzene is clear so that the change from cloudy to clear distillate confirms that drying is complete. If a suitably dry sample is heated in benzene the distillation temperature will be that of pure benzene and the distillate will be clear from the first.

0.3 nm Molecular sieves

Solvents may be dried by any conventional method provided that they are dried to the extent obtainable by use of 0.3 nm molecular sieves. Thus, for instance, when 0.3 nm molecular sieves are used an amount of molecular sieve is added to and left in contact with the solvent for several hours (preferably about 10 hours or more) and at about room temperature (ca 20°C), the amount of molecular sieves used suitably represents a twenty fold excess over the recommended amount to adsorb the anticipated water content in the solvent, according to the manufacturer's instructions, for instance about 100g of molecular sieve per litre of substantially dry solvent.

It is also a requirement that the solvent should be inert to the reagents and the activated polymer. Suitable inert solvents include halogenated alkanes such as dichloromethane and other organic solvents with low hydrophilicity and low hygroscopicity; such solvents are well known to those skilled in the art. Halogenated alkanes, especially dichloromethane, are preferred.

The activated polymer is preferably used directly following its production in accordance with step (a) as this affords the minimum opportunity for degradation

leading to formation of other reactive species which will interfere with subsequent reactions. If the product is to be stored prior to use, for instance when formed in bulk for use in smaller quantities at a later date, it must be stored so as to avoid hydrolysis, i.e. in the presence of a more hygroscopic desiccant. Sulphonyl halides are highly hygroscopic and will dry many common desiccants such as silica gel and thus become hydrolysed. The preferred desiccant for drying and storage of the activated polymer is phosphorus pentoxide.

The reaction of the activated polymer with the target material in step (b) takes place in a non-denaturing medium; for many biological materials this will of necessity be an aqueous medium. There are also many target materials which are stable under non-aqueous conditions and for these it is quite acceptable to conduct step (b) in organic solvents which are inert to the reagents. Ultimately the choice of reaction medium will be dependant on the stability of the target material and final adduct in that medium. Selection of pH, salt concentration, protein concentration and other requirements for stability will be determined on a case-by-case basis. Those skilled in the art will have no difficulty with this. The same applies in relation to determination of non-denaturing temperatures.

When the process of the invention involves the use of a solid support coupled to the activated polymer, the reactions involved in coupling the activating moiety to the solid support will also be conducted under dry conditions, i.e. dry reagents as determined by benzene distillation and dry solvents as determined using molecular sieves of 0.3 nm, will be employed whenever sulphonyl halide groups are present.

It is preferred that the reaction of step (a) is conducted in the presence of a base such as a tertiary amine, preferred bases include those which are easily removed by washing, such as pyridine, and volatile bases

which may be removed by evaporation. At present the preferred base is pyridine. However certain bases, especially pyridine, may react deleteriously with the target material and these should be removed prior to step (b). This may be achieved by conventional means.

It is preferred that the reagents for step (a) are mixed at reduced temperature, preferably at 0°C for instance by chilling with ice and that the reaction mixture is then allowed to warm to ambient temperature, for instance about 20°C.

These preferred features may be adopted in any combination but most preferably all of these preferred features are adopted.

When the polymer of formula (II) has more than one group G and/or one or more capping groups C, it has been found that contamination with related products of formula (II')

$$(C)_{c'}\ POL\text{-}G_{g'} \qquad (II')$$

wherein C, POL and G are as defined above and c' and g' are zero or positive numbers such that c'+g' = c+g but g' is different to g, can lead to undesirable inhibition of the intended reaction and formation of unwanted by-products which therefore complicates the purification and recovery of the eventual adduct. In the case where the polymer of formula (III) is a polyalkylene oxide with one capping group (eg MPEG), c is 1 and g is 1. Contaminants of formula (II') in which c' is 2 and g' is 0 will be unreactive and thus not detrimental but contaminants in which c' is 0 and g' is 2 will cause cross-linking of target materials; preferably such contaminants are avoided in production of the compounds of formula (II) or are removed prior to use of the compound in step (a) of the present process. When the polymer of formula (II) is a material in which c' + g' > 2 there are many possible contaminants; again those

wherein g′ is 0 are unreactive and of little concern whereas those wherein g′ > 1 and g′ > g, especially those wherein g′ > g, cause unwanted side reactions and are preferably removed from the reagent before use.

Whilst the reaction of step (b) will proceed in the presence of large amounts of such contaminants, it is preferred that the amount of all compounds of formula (II′) present in the compound of formula (II) is less than 35%, for instance less than 25%, more preferably less than 20%, for instance, 15, 10 or 5% and yet more preferably below 1% by weight based on the total weight of the compound of formula (II) and all compounds of formula (II′). This may be achieved by purifying the starting materials used in forming the polymer, controlling the polymerisation and subsequent process steps required to form the compound of formula (II) and/or by purifying the compound of formula (II) before use in the process of the invention.

In a preferred aspect of the invention the compound of formula (II) is MPEG in which POL is a divalent residue $-O-(CH_2CH_2O)_x-$ (for instance the residue of PEG 5000), c is 1 and C is methyl and g is 1 and G is hydroxyl. This material is produced by polymerisation from methoxyethanol and ethylene glycol and tends to contain a large proportion of material where polymerisation has initiated from ethylene glycol rather than the methoxyethanol such that chain extension occurs in both directions and a PEG product of approximately twice the molecular weight of the MPEG is present as a major contaminant; this may readily be removed by gel permeation chromatography at an appropriate molecular weight cut-off.

Purity can be checked by nmr and chromatography. Contamination by materials where g′ > g is particularly to be avoided when 1:1 target:polymer adducts are to be produced, since the presence of such contaminants will lead to the production of aggregated materials.

When the reaction of target and activated polymer is

to be performed at a solid:liquid interface, the activated polymer may, in one variant of the process, be linked to a solid support after reacting a compound of formula (I) having a suitable linking group with the polymer. The linking reaction may be effected as described above in connection with the production of compounds of formula (I) linked to a solid support. Thus, for instance, a tetrafluoro-4-amino-azobenzene-4'-sulphonyl derivative of the polymer is reacted with a solid support bearing aldehyde groups (for instance siliconised glass treated with glutaraldehyde) in the presence of a non-nucleophilic base, such as lithium isopropylamide, followed by borohydride reduction of the potentially labile double bond.

It is particularly preferred that the process of the invention is conducted using tresyl chloride as the compound of formula (I) and MPEG, for instance MPEG 5000, as the polymer of formula (II). For MPEG of molecular weight up to 5000 or 6000, purity can be checked by nmr but for higher molecular weight material the methyl signal is swamped and chromatographic techniques must be adopted. These are well known to those skilled in the art.

In this preferred aspect, the product of formula (III) is TMPEG. Ideally this is used immediately but, if not, storage of TMPEG is critical and activity is not well maintained unless it is properly stored. When desiccated over phosphorus pentoxide and stored at 4°C, activity is maintained for at least 1 year. Degradation of TMPEG (either during production or on storage) is detectable on the basis of a change in the FPLC profiles of exposed peptide targets (see Example 1). It produces less substitution of the target at a given molar ratio (a loss of resolution and right shift of the elution profile accompanies the former if FPLC loads are not corrected for the amount of PEG loaded). Substantial aging of TMPEG prepared as previously described is documented in Figure 8

in WO90/04606. Since degradation produces coproduct, degraded TMPEG preparations are also more acidic.

PEG itself is known to oxidise on storage to a brown discoloured product. The TMPEG preparation process removes the antioxidants present in commercially supplied PEG. Oxidation has been observed in several stored TMPEG preparations and it is recommended that, if prolonged storage is anticipated, an appropriate antioxidant should be included. This new method for preparing and storing the TMPEG has significant advantages over previously described methods in terms of the activity, reproducibility between preparations and stability of individual preparations.

In an especially preferred aspect the present invention provides a process comprising the steps of

(a) reacting dry MPEG (as determined by benzene distillation) containing less than 10% by weight of PEG (as determined by nmr and/or chromatography) with tresyl chloride in dry dichloromethane (as determined using 0.3 nm molecular sieves) in the presence of pyridine in a reaction vessel from which water is excluded, so as to form TMPEG, recovering the TMPEG so formed and either storing it over phosphorus pentoxide or using it directly in step (b),

(b) reacting the TMPEG so formed, optionally after storage, with a target material such as erythropoietin (EPO) in aqueous medium and about 20°C and

(c) recovering the Target:MPEG adduct (eg EPO:MPEG) so formed.

More preferably the molar ratio of tresyl chloride to

MPEG is 2:1 or more, most preferably about 2.5:1.

The process of the present invention may be supplemented by one or more separation and/or purification steps at any stage as necessary or desirable. Separation and purification may be achieved by appropriate techniques well known in the art selected having regard to the need to maintain the activity of the reagents and products and to avoid use of toxic or interfering materials. In some cases, for instance where the polymer is a polyalkylene glycol, aqueous biphasic polyalkylene glycol solutions may be used to effect separation and/or purification of the activated polymer and/or polymer:target adduct.

THE PRODUCTS

The present invention further provides polymer:target adducts obtainable by the process of the invention other than the known polymer:target adducts having polymer and target moieties directly linked by stable, non biodegradable covalent bonds which are described in the references discussed above.

The invention also extends to such products for use in therapeutic and diagnostic methods of treatment of the human or animal body and to the use of such products in the manufacture of medicaments for use in therapeutic and diagnostic methods of treatment of the human or animal body and to pharmaceutical compositions comprising products of the invention together with pharmaceutically acceptable diluents or carriers.

Many of the prior methods of coupling polymers to targets are unsuitable for coupling more than one target molecule to each polymer molecule since most methods use polymers having only one group capable of reacting with the target. In contrast, the process of the present invention enables the production of constructs such as the following which form particular embodiments of the present invention:

1. Liposomes bearing linear polymeric linking groups bound to the surface of the liposome at one terminal of the polymer and bearing a receptor ligand, receptor molecule, antibody, antigen or other molecule of therapeutic or diagnostic interest at the other terminal.

2. Constructs where a plurality of identical target molecules are linked to a single polymer moiety; for instance a linear polymer having two reactive termini is linked to two target molecules to enhance the biological activity thereof or a branched polymer having three or more reactive termini or a polymer having reactive pendant groups is linked to three or more target molecules.

3. Constructs as in 2. above wherein the target molecules are different; such constructs may be intended to have synergistic effect when the target molecules interact with each other or with other substrates.

4. Constructs wherein the polymer moiety is linked to a target molecule at two or more positions either by reaction of both termini of a linear polymer with different sites on the target molecule or by reaction of pendant reactive groups, or the termini of a branched polymer, at two, three or more sites on the target molecule.

The products of the present invention preferably comprise any one of the polymer materials set out above and any one or more of the target materials set out above. Particularly preferred products of the invention are adducts of a polyalkylene glycol, especially polyethylene glycol and polypropylene glycol with the former being most preferred, with any one or more of the target materials set out above, with erythropoietin (EPO) being particularly preferred.

The production of adducts wherein two or more

different target species are coupled to a multivalent polymer presents special difficulties which can be overcome by the process of the present invention. For this situation an appropriate procedure for producing a product comprising two different targets involves the following steps:

1. A first target, Target (A), is exposed to activated polymer (AM-Polymer-AM) with the latter in gross excess such that essentially only 1:1 Target(A):polymer adducts are formed and 2:1 or higher Target(A):polymer adduct formation is minimised. This can be followed by FPLC or other appropriate methods to separate and, if necessary, purify the adduct, provided that this is sufficiently rapid to avoid hydrolysis of the remaining activating moieties. If the target has many derivatisable groups, it may be necessary to fine-tune the coupling ratio, reaction time and/or pH, so that 2:1 or lower Target(A):polymer adducts are not formed or, if formed are discarded. Alternatively a mixture of monovalent and multivalent activated polymer species may be used in a ratio selected such that it is statistically likely that only one of the polymer molecules attached to any target molecule will be the multivalent form (targets which are by chance only modified with the univalent form will be wasted).

2. Either:

a) the Target(A):polymer adduct is first separated from the AM-polymer-AM then reacted with the second target, Target(B), preferably at equimolar ratio or, if this reacts too slowly, with the adduct in excess; or

b) the reaction product of step 1 is reacted

with Target(B), preferably at a molar ratio of 1:2 with respect to the amount of activating moieties remaining in order to reduce the formation of Target(B):polymer:Target(B) constructs. This is much simpler than (a) but more wasteful in terms of Target(B) which is therefore selected as the cheaper of the targets.

After a sufficient reaction time (derived empirically), the excess -AM is neutralised with a monovalent neutralising agent e.g. with glycine, and the products are purified to discriminate the combinatorial possibilities. This may be possible on the basis of molecular weight if target(A) and target(B) differ significantly in size or via differential labelling of the targets. Alternately, since the major contaminant will be Target(B):polymer:Target(B) at this stage, an affinity purification method, with affinity ligand to Target(A), should enrich for hybrids. Similar measures may be adopted to construct more complex adducts.

A particular advantage of the present invention is that the process enables the coupling of polymer moieties to oligonucleotides and nucleic acids (DNA and RNA) at defined positions. EP-A-0 292 128 (Seger 1988) deals with "improved DNA probes" and uses PEG, amongst other molecules, to link DNA to reporter groups for hybridisation. However the PEG is linked to the 5'-phosphate of the DNA and there is no indication of a method which would link the PEG without leaving a coupling moiety. This ability to modify DNA, RNA and synthetic oligonucleotides with polymer will influence the solubility and alter biodistribution and has applications in both the in vitro and therapeutic or diagnostic (in vivo) use of nucleotides.

Further improvements offered by the invention include the ability to maximise the biological activity retention and/or to increase the activity of the target molecule, minimise the toxicity of the product, minimise the reaction time at physiological pH, reduce contamination of the product and improve the stability of the activated polymer.

The invention will be illustrated with reference to the accompanying figures of the drawings in which:

Fig.1 shows the results of separations of MPEG 5000 obtained commercially.

Fig.2 is a plot of age of TMPEG used and % of gm-CSF left unmodified by reaction with aged TMPEG produced according to the invention.

Fig.3 is a plot of the relative activities of PEGylated gm-CSF prepared by the process of the invention and by a previously described process.

Fig.4 plots the activity of EPO and PEG-EPO.

Fig.5 is a gel showing DNA fragments variously treated with TMPEG, MPEG or buffer.

Fig.6 shows log concentrations of gm-CSF and various PEG-gmCSF adducts in blood and tissue of mice.

Fig.7 shows the results of fractionation of gm-CSF and PEG-gm-CSF before and after ageing.

Fig.8 shows FPLC profiles for EPO PEGylated with various molar ratios of TMPEG:lysine.

Fig.9 shows biological activity of unmodified and PEGylated EPO.

The present invention will now be illustrated by the following Examples which are not intended to limit the scope of the invention in any way:

EXAMPLES

Examples 1a and b and Comparative Examples 1a and b

(a) Purification of MPEG

MPEG-5000 (Union Carbide) was subjected to permeation gel chromatography on Superose 12 (Fig. 1a). The material has a clearly biphasic size distribution with an estimated 22.9% high molecular weight contaminant (9280Da) and a low molecular weight component (5460Da). The good agreement between proportions of the two peak areas and the NMR estimate of PEG versus MPEG in the same preparation suggest that all the PEG is accounted for by the high molecular weight species. To confirm this and to devise an appropriate purification procedure, vesicle chromatography [Ehwald (1991)] was used. Analytical and preparative scale preparations gave different efficiencies of separation. Analytical scale separation was performed using vesicular packing material P1(5) equilibrated in 0.05M NaH_2PO_4 buffer pH 5.5 (column bed volume 22 ml). The MPEG preparation (Union Carbide Mw 5000), 0.5ml of a 20mg/ml solution in PBS was loaded onto the column. The column was eluted with PBS using a flow rate of 0.08 ml/min and 0.5 ml fractions were collected. The elution profile is shown in Fig.1b; circa 8% of the material was eluted in the excluded fraction (high molecular weight) and 92% in the permeable fraction (low molecular weight fraction). In preparative scale (using 6.5L bed volume and 15g/500ml MPEG in 0.01M NaH_2PO_4 pH 5.5 and an elution rate of 20.5 ml/min) the excluded fraction (PEG) was 11.2 % (Fig.1c). Rechromatography on Superose 12 of the two pooled fractions (shaded and hatched areas of Fig.1c) taken from the preparative scale fractionation on Superose 12 was used to determine the extent to which the two materials were separated (Fig. 1d, squares - permeable fraction, crosses - excluded fraction). NMR analysis of the permeable fraction gave an estimated ratio of PEG:MPEG of 11:89 mole:mole, which is in good agreement with the area

under the curve estimate of the residual high molecular weight contaminant in the permeable fraction on the elution profile on Superose 12 (Fig.1d, squares). NMR analysis could not be performed on the excluded fraction because of its much higher molecular weight. Further rounds of vesicle chromatography, at analytical scale, gave a comparable reduction in the high molecular weight material (the permeable fraction yielded a smaller "excluded" peak on rechromatography, circa 4% in the high molecular weight excluded fraction, using a second round of vesicle chromatography, Fig. 1e).

(b) Preparation of TMPEG

Tresyl chloride was used when freshly prepared or after storage in airtight ampoules. MPEG-5000 (Mr 5000, 18g, 3.5 mmol) was dried with benzene (B.P. 79-80°C) by distillation of the water-benzene azeotrope and then the benzene. The water-free MPEG was then immediately dissolved in dichloromethane (45 ml, ANALAR, previously dried over molecular sieve 3Å, 100 g per litre of solvent, overnight at room temperature). Activation of MPEG-5000 with tresyl chloride was carried out at a molar ratio of 2.5:1 (tresyl chloride to available hydroxyl groups in MPEG). The MPEG/dichloromethane mixture was then cooled on ice (to circa 3°C) and pyridine (1 ml, 12.4 mmol) followed by tresyl chloride (1 ml, 9 mmol), both precooled on ice were added dropwise with constant stirring using a magnetic stirrer. The reaction was allowed to continue (for 2 hr) at room temperature with constant stirring before the removal of dichloromethane by evaporation under reduced pressure. The solid obtained (TMPEG) was redissolved in methanol-hydrochloric acid mixture (1000:0.3 v/v) and allowed to precipitate overnight at reduced temperature (-20°C). The precipitate was recovered by centrifugation (at 1100 x g, for 10 minutes) at reduced temperature (0°C) and the supernatant was spectrophotometrically checked for pyridine content (λmax 255nm). This procedure was repeated until no

pyridine could be detected, usually 12 to 15 washes. Finally, the pyridine-free precipitate was washed in methanol only, preferably at least twice, and then the methanol was removed by evaporation under reduced pressure and the TMPEG was finally dried by freezing in liquid nitrogen and lyophilising under reduced pressure. The hydroxyl content of the white solid as determined by ^{1}H nmr obtained was undetectable (4.56ppm). Therefore, approximately 100 % of hydroxyl groups in the MPEG were transformed into tresyl esters.

The TMPEG so produced was desiccated over phosphorus pentoxide and stored at 4°C.

(c) Coupling to GM-CSF

The activity of TMPEG samples was monitored by exposure of the samples to gm-CSF at molar ratios of 305:1 (Example 1a and Comparative Example 1a) or 75:1 (Example 1b and Comparative Example 1b) in a standard coupling reaction and estimating the percent of the preparation remaining unmodified after the reaction as shown in Fig.2: the relative activities of TMPEG preparations obtained as described above (Examples 1a and b) and of TMPEG made by a prior art process (Comparative Examples 1a and b) is plotted against the storage period. TMPEG made by the process of the invention and used at 305:1 (squares), throughout the observation period, gave <10% residual unmodified gm-CSF. The equivalent result when using the same material at 75:1 (diamonds) was circa 20% unmodified material. With both preparations there was no evidence of a trend of worsening activity with storage. In contrast preparations made from MPEG as obtained from the manufacturer by a previously described method (WO90/04606, Example 1) (triangles; downwards triangles 305:1 and upwards triangles 75:1) showed: (1) lower mean activity (reflected in higher mean residual unmodified material); (2) a very broad scatter of reactivities; (3) 3 samples completely inactive at 75:1 and 2 inactive at 305:1 after

only 5-12 weeks of storage. At 305:1 the process of the invention consistently produced 92-95% modification, irrespective of the age of the TMPEG and using a coupling ratio of 75:1, circa 80% of the gm-CSF preparation was modified.

The process described above (Example 1) has been repeated on a number of occasions with similar results.

The gm-CSF PEGylated using the process of Example 1 showed no significant loss of its growth stimulating activity as assessed by granulocyte-macrophage colony assay (Fig.3a) or by thymidine uptake (Fig. 3b). Dose response analyses are a relatively insensitive means for demonstrating subtle differences in bioactivity and are also difficult to analyse after pooling because of the high contribution to errors of the variation in the response level between experiments. A better approach is to perform a correlation analysis, plotting the response obtained with equivalent amounts of the modified and unmodified materials on an XY plot. Identical activity gives datum points randomly distributed about the line representing equal activity (the dashed lines). Reduced activity reveals itself as a curvilinear departure from the equal activity line which converges towards the line at the extremities (if sufficiently broad a dose response range is examined such that the plateau of maximum stimulation is reached). In contrast, the presence of inhibitory material, with or without loss of intrinsic activity, produces a departure, usually without convergence to the upper extremity. In the latter case (i.e. where there is no loss of intrinsic activity) failure to observe divergence at the lower extremity indicates that the inhibitor is masking activity only at relatively high inhibitor levels; divergence throughout the plot indicates either an inhibitor with powerful effect at low dilution or combined inhibition and

loss of activity.

Two assays for the growth stimulating activity of GM-CSF prepared by the methods of Example 1 (■ in Fig.3) and Comparative Example 1 (□ in Fig.3) show that the process of the invention gives better conservation of biological activity. Colony counts or 3H-thymidine uptake (normalised with respect to the maximum per experiment to avoid a contribution of between-experiment differences to the correlation) were plotted for comparable amounts of PEG-GM-CSF and GM-CSF over the dose range spanning the upper and lower asymptotes of the dose response curve (0.1 to 8 ng/ml for colony assays and 0.0006 to 1.0ng/ml for thymidine uptake assays). Datum points are means of colony counts in triplicate dishes for three independent experiments (Fig. 3a) or of two independent thymidine uptake experiments (Fig 3b). The results in the thymidine uptake demonstrate no significant loss of activity with the process of Example 1 and loss of activity without significant inhibitory material for the process of Comparative Example 1 (TMPEG in equivalent doses was not inhibitory in this assay). The results for colony stimulating activity again show no significant loss of activity with process of the invention but indicate an additional inhibitory activity for this assay when the old method was used possibly accompanied by loss of bioactivity.

Example 2

a) Preparation of ditresyl PEG (TPEGT)

PEG-6000 (10.5 g, 1.75 mmol) was dissolved in benzene (30 ml) and dried as in Example 1 above. The dry PEG-6000 was then immediately dissolved in 25 ml of dichloromethane (dried as in Example 1), cooled on ice and pyridine (1 ml, 2.4 mmol) followed by tresyl chloride (1 ml, 9 mmol) were added dropwise. The mixture was left to react (two hours at room temperature) and the dichloromethane was evaporated as

in Example 1. The solid was resuspended in methanol:hydrochloric acid and was treated as above.

b) Coupling to GM-CSF

To test that this material was bivalent and could couple target(s) at both ends of the PEG chain, this TPEGT was used to aggregate GM-CSF. ^{125}I-GM-CSF (1.4nmol/ml) was reacted with TPEGT (160mg/ml) for 2h at room temperature. The resulting aggregates were estimated by FPLC and contained 95% of the total GM-CSF. Thus the bivalent AM-polymer-AM construct is demonstrated to be functional.

Example 3

Example 2 was repeated using TMPEG prepared from a sample of MPEG containing 8% PEG as contaminant, and thus containing about 8% TPEGT. When used to aggregate GM-CSF, this material (160 mg/ml) produced an aggregate estimated by FPLC to contain only 20% of the total GM-CSF. This demonstrates that the higher proportion of conjugates seen in Example 2 was related to the additional TPEGT and not merely due to non-specific aggregation. It should be noted that using a prior art process, the present inventors have shown [Malik et al (1992) Experimental Hematology, 20, 1028, fig. 4] that both the non-specific aggregated gm-CSF in unPEGylated reactions and aggregates generated in PEGylation reactions (which include cross-linked products due to TPEGT) have an extremely high specific activity, as assessed by thymidine incorporation, with respect to monomeric gm-CSF). Thus it is anticipated that the bivalent 2-polymer construct generated in Examples 2 and 3 would have a higher specific activity than monomeric unmodified gm-CSF.

Example 4 and Comparative Examples 2,3 and 4

To document the better conservation of biological activity, direct comparisons were made with three of the

widely used current methods, using erythropoietin as the target peptide. It is an important prerequisite in experiments of this type to perform preliminary experiments (using at least two independent assays of bioactivity and some measure of the degree of modification) to select the optimum coupling ratio and duration of coupling reaction for maximum retention of biological activity. It is important to record the degree of modification since this may vary between the methods being analysed and only materials substituted to approximately the same extent should be compared for retention of activity.

Serial dilutions of TMPEG produced as in Example 1 were mixed with the same amount of erythropoietin and the resultant PEG-erythropoietin adducts were assessed first by FPLC for the degree of modification and also in the thymidine uptake assay [Malik et al., (1992) Experimental Hematology, 20: 1028] for a preliminary estimate of activity. Based on the latter a smaller range of activities were analysed in colony assays using the methyl cellulose assay system of Ash et al., Blood, 58:309-316 (1981), Knusli, C. et al. (1992) Br. J. Haematol. 82(4): 654.

Commercially available activated PEGs (Sigma Limited) were used to PEGylate recombinant human erythropoietin (Cilag Ltd.) by the cyanuric chloride (Comparative Example 2), succinimidyl succinate (Comparative Example 3) and phenylchloroformate (MPEG-p-nitrophenylcarbonate) methods (Comparative Example 4). TMPEG, prepared as described above, or the alternate activated PEGs, were incubated (for 2 h) with erythropoietin (100 μg/ml total protein, i.e. carrier plus erythropoietin) in coupling buffer (PBS) at room temperature in a rotary mixer, at an activated-PEG:lysine molar ratio of 75:1. Conditions were standardised so that differences in pH and duration of the coupling reaction could not account for differences in the residual bioactivity. Representative reactions at the same molar ratios were checked by FPLC and found to be ≥85%

modified. Modified material was assayed in methylcellulose cultures of normal human bone marrow progenitor cells essentially by the method of Ash et al (1981) Blood, 58 309-316, but substituting recombinant human GM-CSF for leucocyte conditioned medium. Erythroid bursts were scored microscopically on encoded, encrypted dishes on day 14-16 of culture. The results for the optimised TMPEG-derived adducts and for products of the other coupling reactions having the same coupling ratio are shown in Fig.4 as means of triplicate culture dishes except in Panel A where the results are means ± SEM for 3 independent experiments. Fig 4a shows the excellent conservation of biological activity achieved with EPO PEGylated with the TMPEG (filled circles) compared with unmodified EPO (open circles). Datum points are superimposed except at 4U/ml (33.6 ng/ml) erythropoietin. Similar effects observed in CFUgm assays were found to be due to a modest inhibitory effect of TMPEG in the assay system.

Fig. 4b shows a complete loss of detectable activity when the cyanuric chloride method (filled circles) was used compared with PEG-EPO prepared according to Example 1 (open circles) and a high dose inhibition of endogenously stimulated erythroid colonies. This indicates either the presence of a profoundly inhibitory substance in the reaction mixture or loss of all intrinsic erythropoietic activity in conjunction with some inhibitory material. Lack of even a slight increment in colony formation at low doses and the shallow dose related inhibition of endogenously stimulated colonies at high concentrations favours the latter interpretation. The FPLC profile for this material also differed somewhat from that obtained with the other three activated PEG preparations in that there was a higher proportion of material eluting with the void volume, indicating the presence of more aggregates. This suggests that crosslinking of target molecules may be occurring (as has previously been observed for this agent [Leonard

(1984)]).

Fig. 4c shows a somewhat different picture for PEG-EPO prepared by the succinimidyl succinate method (filled circles), with detectable activity only at 4U/ml (33.6ng/ml) compared with PEG-EPO according to the invention (open circles). This type of shift in the dose-response curve is less likely to be due to inhibitor and probably represents over an order of magnitude loss in bioactivity. This is somewhat surprising because this method is claimed to have good conservation of biological activity [Katre (1987), Zalipsky (1992)]. However such claims have been made on the basis of short term assays. In the assay used here the erythropoietin needs to be available throughout the 14-16 day culture period. The cells in these cultures are also a rich source of esterases and the PEG-erythropoietin made by this method contains a potentially labile bond (see Table 1). In this and some related active ester methods, removal of the PEG leaves the molecule modified as follows:- Target-NH_2 forms

Target-NH-CO-CH_2-$(CH_2)_n$-CO-PEG

then esterase cleavage forms

Target-NH-CO-CH_2-$(CH_2)_n$-COOH.

This process might well influence bioactivity adversely since there is a charge conversion from a lysine amino group to a carboxyl group at the previously PEGylated site.

Fig. 4d shows PEG-erythropoietin made using monomethoxy PEG-p-nitrophenylcarbonate (filled circles) compared with unmodified (sham-treated) EPO (open circles). Here there are increments in colony number at low doses similar to that seen with the tresyl chloride activated PEG, but the high-dose inhibition of colony formation is

much more evident, indicating the presence of inhibitory material.

Comparative Example 5

An attempt was made to make PEG-erythropoietin using the carbonyldiimidazole method under comparable conditions to those used above, but on this time scale and coupling ratio the degree of modification achieved was not significant.

Example 5

A solution (50μl) of amphotericin (Fungizone) in distilled water (20 mg/ml) was mixed with HEPES buffer (450μl, pH 9.0) containing TMPEG produced according to Example 1 (60 mg/ml). The mixture was then incubated at room temperature for 24 h. As a control, amphotericin was similarly treated but with MPEG substituted for TMPEG. To demonstrate the covalent linkage of the TMPEG to the amphotericin, the partition coefficient of amphotericin in both samples was measured as follows: 100μl samples were mixed with 1 ml of top and 1 ml of bottom phases of a biphasic system containing 5% dextran T-500, 5% PEG-6000, 0.15 M sodium chloride and 0.01 M sodium phosphate pH 6.8. After shaking for 1 min. the system was left to settle for 20 min. and then 500μl from the top and bottom phases were removed to quantify amphotericin (by measuring the absorbance at 330 nm). The % material in the top (PEG-rich) phase was: a) control 4.9 ± 0.2%; b) MPEG control 4.1 ± 0.4%; c) TMPEG (preparation 1) 92.8 ± 0.1%; d) TMPEG (preparation 2) 92.7 ± 0.2%.

Example 6

As an example of creation of an affinity ligand PEG-

WGA (polyethyleneglycol modified wheat germ agglutinin) was constructed in exactly the same manner as used in Example 1 and used to bind rightside-out vesicles from human erythrocyte membranes thus altering their partition in a PEG-dextran aqueous two-phase system. Rightside-out vesicles exposed to phosphate buffered saline prior to partitioning showed the following distribution: 17.6 ± 1.2% to the top phase, 48.7 ± 9.0% to the interface and 33.6 ± 8.6% to the bottom phase (mean ± SEM, n=3). Rightside-out vesicles exposed to the PEG-WGA ligand prior to partioning showed the following distribution: 30.1 ± 1.2% to the top phase, 32.7 ± 1.4% to the interface and 7.2 ± 0.6% to the bottom phase. This change in partitioning can be exploited to remove rightside-out vesicles from a mixture with inside-out vesicles thus obtaining a pure preparation of inside-out vesicles from human erythrocyte membranes.

Example 7

Aliquots of human erythrocytes (50μl containing 0.95 x 10^7 cells) were added to one of the following reagents (500μl):

a) sodium phosphate buffer (0.05M, pH 7.5) containing sodium chloride (0.125M) (PBS).

b) TMPEG freshly prepared as in Example 1 in PBS (36 mg/ml, equivalent to 1.9 ng/cell).

c) TMPEG (36 mg/ml) inactivated with lysine (Sigma Ltd. 4mg/ml) at 2.5:1 molar lysine:TMPEG for 2h at room temperature.

After 30 min incubation at 37°C cells were pelleted down and resuspended in PEG-rich top phase (1 ml) so that their PEGylation could be monitored in a PEG-dextran phase system. Cells incubated in PBS partitioned with 26.2 ± 11.8% (mean ± SD) cells in the top phase. With TMPEG exposure of cells this increased to 72.1 ± 10.7%, whereas

with prior inactivation of TMPEG to prevent coupling to cells there was only 32.7 ± 9.3% in the top phase, indicating that covalent attachment of the PEG to the erythrocytes was responsible for the change in partitioning behaviour. The erythrocytes remained intact in the TMPEG-treated and control experiments indicating that the method does not disrupt the cell membrane.

Example 8 and Comparative Example 6

Liposomes were reacted with TMPEG prepared by the process of WO90/04384 (Comparative Example 6) and the process of Example 1 (Example 8). The success of the PEGylation was followed in a PEG-dextran phase system by quantitating the liposome content of the top (PEG-rich) and bottom (dextran-rich) phases and at the interface. Because the TMPEG prepared by the process of Example 1 was known to be more active, only half the molar ratio was used. Despite this, a much higher degree of substitution of the liposome was achieved. This greater reactivity has the advantage that the liposomal preparation does not have to be exposed to so much activated PEG (the level of the latter is limited by its effect on liposomal stability and/or aggregation). 100 nm diameter unilamellar vesicles of bovine spinal cord phosphatidylserine (PS) were prepared by extruding lipid dispersions of PS (10 mg/ml in HEPES buffer pH9), spiked with ^{3}H-dipalmitoylphosphatidylcholine through 100 nm polycarbonate filters ten times using an extruder device (Lipex Biomembranes, Canada). Vesicles (300 µl) were incubated with TMPEG (39 mg, molar ratio TMPEG:PS at outer surface 4:1 or 19.5 mg, molar ratio 2:1) in HEPES buffer (60 µl) for 18 hrs at room temperature. As a control MPEG was substituted for TMPEG. To demonstrate the covalent attachment of PEG to the outer surface of the vesicles the distribution of the vesicle in a two-phase system was measured as follows: samples (20 µl) were mixed with top

phase (1 ml) and bottom phase (1 ml) of a biphasic system containing dextran T-500 (5%) and PEG 6000 (5%), sodium chloride (0.15M) and sodium phosphate buffer (0.01M) prepared at 25°C. After shaking for 1 min, triplicate samples (50 μl) were removed for total counts. After the phases had separated at 25°C for 20 min triplicate samples were taken from the top phase (50 μl) and the bottom phase (20 μl) for scintillation counting. Vesicle partitionings, calculated as the percentage of added vesicles that were present in the top(T) and bottom(B) phases and at the interface (100-T-B) were as shown in Table 2.

Table 2

TMPEG sample	TMPEG:PS Molar ratio	Partitioning (%) (mean of triplicate partitions)		
		Top	Interface	Bottom
Old Method	4:1	6.3±0.6	25.3±4.0	68.4±3.7
Control MPEG		5.5±0.3	9.1±4.9	85.4±4.8
New Method	2:1	71.6±1.2	11.1±1.2	17.3±0.5
Control MPEG		4.9±0.2	1.6±1.6	104.3±7.3

The increase in interface partitioning with associated decrease in bottom phase partitioning with the old method indicated some PEGylation. However with the activated PEG made by the new method, even at the lower molar ratio there is extensive partitioning to the top phase indicating the highest degree of PEGylation of the two samples.

To increase the PEGylation with the rather unreactive old method sample, the molar ratio was increased to 20:1, using a final concentration of 35% w/w TMPEG. This caused the vesicles to aggregate. Controls with MPEG also showed aggregation. Addition of 75µl of the reaction mixture to 2.2 ml of N-tris-(hydroxymethyl)methyl-2-amino-ethane-sulphonic acid (TES) buffer [Fisher et al (1991) Cell and Model Membrane Interactions p.47 Plenum Press, New York] pH 7.4 gave solutions with OD_{650} of 0.26 whereas untreated

vesicles in control buffer had OD_{650} of 0.01, indicating that the aggregation observed with the TMPEG and MPEG was not completely reversible. It is well established that PEG solutions can produce fusion and/or permeability increases [Tilcock & Fisher (1982) Biochimica et Biophysica Acta, 688 645-652, Aldwinkle et al., (1992) ibid, 689: 548]

Example 9

(a) 1μg of the supercoiled plasmid pBR322 was digested with 100 units of the restriction enzyme Rsa I for two hours at 37°C, in low salt buffer consisting of 10mM Tris HCl pH 7.5, 10mM $MgCl_2$, 1 mM dithiothreitol (DTT). This yields four blunt ended fragments per molecule of pBR322. Protein was removed by phenol/chloroform extraction. After ethanol precipitation the DNA was resuspended in a small volume of tris-EDTA (TE) pH 7.6 and the DNA was end labelled with [γ32P] dATP using a BCL kit as per the manufacturer's instructions. Removal of the free [^{32}P] dATP was achieved using Sephadex G-50 columns. The DNA was then split into 6 aliquots. Three of these aliquots were made single stranded by boiling and then exposed to either TMPEG or MPEG, at a concentration of 400mg/ml in coupling buffer (consisting of 0.005M sodium phosphate 0.125M sodium chloride pH 7.5) or to coupling buffer only, at a volume ratio of 150 μl:150μl), for 20 minutes. Three other aliquots, which were allowed to remain double stranded, were incubated with either TMPEG, MPEG or

coupling buffer only, under identical conditions. After incubation, all the samples were again made single stranded by boiling. The samples were examined in a 2% alkaline agarose gel, (50mM NaOH, 1mM EDTA pH 8.0) using alkaline loading buffer. This was a 6x stock consisting of 0.3M NaOH, 6mM EDTA pH 8.0, 18% Ficoll 400, and 0.15% bromocresol green. The samples were run overnight at 50v. The dried gel (Fig. 5) was analysed by autoradiography, the film was developed in an automated Fuji X-ray film developer. Lanes 1-6 from left to right are: 1-3 DNA exposed while double stranded; 4-6 DNA exposed while single stranded; 1&4 coupling buffer; 2&5 MPEG; 3&6 TMPEG. Only single stranded DNA exposed to TMPEG showed a mobility shift demonstrating coupling of PEG to the DNA.

(b) Eco RI digested pBR322 containing a single cleavage site yielding one double stranded fragment with a 3' recessed 4bp cut and the following single stranded overhangs:-

5'NC.....AATTCN3'

3'NGTTAA.....GN5'.

Of three aliquots, one was treated with a reaction mixture consisting of TMPEG (400 mg/ml) in coupling buffer (50 ml), DNA (circa 0.1 μg in 50 ul of tris EDTA). The coupling buffer (pH 7.5) was a solution of sodium chloride (0.125M) and sodium phosphate (0.05M). The reaction was conducted at

room temperature for 20 min. A second aliquot was similarly teated with TMPEG (40 mg/ml) in coupling buffer and the third was treated with coupling buffer alone.

(c) Bam HI digested pBR322 containing a single cleavage site yielding one double stranded fragment with a 3′ recessed 4bp cut and the following single stranded overhangs:-

5′NG.....GATCCN3′

3′NCCTAG.....GN5′.

This material was divided into three aliquots which were treated with two concentrations of TMPEG and coupling buffer as in (b).

To detect the extent of PEG-modification the staggered ended DNA was end-labelled with ^{32}P and then partitioned in a PEG-phosphate phase system to determine the partition coefficient (K), results being shown in Table 3.

Table 3

	No PEG	TMPEG 40mg/ml	TMPEG 400mg/ml
DNA digest	EcoR1 50μg/ml	ECoR1 50μg/ml	ECoR1 50μg/ml
PEG-phase (%)*	41.7	58.4	96.5
PO_4-phase (%)*	58.3	41.5	3.5
log(K)	-0.145	-0.148	1.44
DNA digest	BamH1 50μg/ml	BamH1 50μg/ml	BamH1 50μg/ml
PEG-phase (%)*	41.7	51.0	69.4
PO_4-phase (%)*	58.3	49.0	30.6
log(K)	-0.145	-0.017	0.356

* Yields corrected for differential recovery from the phases via recovery controls.

Up to saturation there is known to be a linear relationship between the number of PEG molecules attached per target molecule and log(K). The DNA cleaved with EcoRI (with two free amino groups supplied by two adenine bases) is more readily modified than the DNA cleaved with BamHI (with three free amino groups supplied by adenine, guanine and cytosine).

Example 10

BALB/c, male, 6-8 week-old mice, weighing approximately 20g, were pooled into groups of three per condition, with *adlib* access to food and water. PEG-modified GM-CSF samples

were prepared as in Example 1, using the concentrations of GM-CSF and TM-PEG indicated in Table 4a. The reaction products were evaluated by FPLC and the proportions of individual species were estimated by fitting summated Gaussian curves to the FPLC profiles and estimating the area under the curve corresponding to each individual peak and expressing this as a % of the total area for the whole FPLC profile (Table 4b). The inventors have previously established that the individual peaks seen at low TMPEG concentrations (peaks 0, 1, 2 and 3) correspond to GM-CSF, PEG_1-GM-CSF, PEG_2-GM-CSF, PEG_3-GM-CSF, respectively. At high TMPEG concentrations the peaks are broader and less well resolved thus fitting of individual Gaussian curves over all regions of the FPLC profile may not be possible. Thus peak 3 and the peaks for more highly substituted GM-CSF (potentially PEG_{4-7}-GM-CSF) have been pooled. The peak eluting with the void volume peak is well resolved from the PEG_{4-7}-GM-CSF and presumably represents aggregates, the area of this peak was used to estimate the proportion of aggregated material (Table 4b).

The different PEGylated samples and unmodified GM-CSF (Hoechst), all containing <4% [^{125}I]GM-CSF (Amersham, 1222 Ci/mmol) to serve as a tracer, were adminstrated at a dose of 0.0524μg in 100μl (3.45×10^{-12} mole; equivalent to 2.5μg/kg body weight) by subcutaneous injection. The amount of TMPEG concomitantly administered is also indicated in Table 4a (MPEG has been shown not to influence $t_{1/2}$, but

does influence egress from the subcutaneous site). Up to eight 25μl tail vein blood samples were collected from each mouse using capillary tubes at various time points ranging between 10 minutes and 80 hours, to give a minimum of three samples per time point. Samples from the capillary tubes were washed immediately into 1ml of PBS containing 50 I.U. of heparin. Radioactivity was determined using a gamma counter (LKB 1270 Rackgamma) results being shown in Fig. 6a (open circles for untreated material, other symbols as indicated on the figure). Clearances for the materials of reactions A and B were clearly biphasic, presumably reflecting the large proportion of unmodified material remaining in these preparations (Table 4b). Half-lives were calculated using linear regression (log concentration versus time) for the slower clearing component if biphasic elimination was present (solid lines Figure 6a; dotted lines give the 95% confidence intervals). The $t_{1/2}$ values ±SE are given in Table 5.

With the exception of the product of reaction D, which is known to contain >50% of aggregates (the latter are known to clear slowly), $t_{1/2}$ for the other reactions (A-C) are similar. Although there may be some increment in $t_{1/2}$ between reactions A and B, surprisingly, there is no additional increment in $t_{1/2}$ betwen reactions B and C. This was not anticipated in view of the fact that reaction C produced a higher proportion of PEG_2-GM-CSF and adducts with higher PEGylation ratios. The difference in $t_{1/2}$

between reactions A and B is also not marked and, with the proviso that dissection of early and late components introduces more error into the $t_{1/2}$ estimates, it can be inferred that the addition of the first PEG molecule has the greatest impact on the clearance of GM-CSF. This is unexpected because the estimates for apparent molecular weight from FPLC were initially: GM-CSF 14.5kDa; PEG_1-GM-CSF 40.5kDa; PEG_2-GM-CSF 67.6 kDa; PEG_3-GM-CSF 112.9 kDa and after 3 or 4 independant estimates the values were: GM-CSF 12.5 ± 1 kDa; PEG_1-GM-CSF 41.5 ± 3.6 kDa; PEG_2-GM-CSF 75.2 ± 10.5 kDa; PEG_3-GM-CSF 138.5 ± 27.3 kDa. Thus, PEG_1-GM-CSF should not exceed the renal molecular weight threshold for excretion and the major increment in the $t_{1/2}$ would have been expected to be between PEG_1- and PEG_2-GM-CSF not between GM-CSF and PEG_1-GM-CSF. This result is also surprising in that the increment in apparent molecular weight is unexpectedly large for the addition of the first MPEG 5000 molecule (12.5 to 41.1 kDa). Other proteins (e.g. recombinant erythropoietin) have shown a surprisingly small increment in apparent molecular weight with the addition of one MPEG 5000 molecule (eg circa 1.4 kDa increment).

In order to establish the contributions to extended $t_{1/2}$ we examined the tissue distribution of material prepared in an identical manner to reaction C, using an identical dose. At each of the times indicated, one aminal was sacrificed and organs/tissue including kidney, spleen, liver, lung, heart and femur were recovered and

radioactivity was measured as above. Figure 6b shows the results. The dotted and dashed lines indicate the blood levels of GM-CSF and PEG-GM-CSF respectively. The filled circles and open circles are the organ concentrations of PEG-GM-CSF and GM-CSF respectively. Comparison of organ:blood concentration ratios indicates that renal accumulation (the kidney is the only organ which achieves high organ:blood ratios and is the site which is known to catabolise the peptide to small fragments), is substantially reduced by PEGylation of the degree achieved in reaction C. This is somewhat surprising since circa 24% of the reaction C mixture represents PEG_1-GM-CSF (i.e. material below the renal threshold). It suggests that the size of PEG conjugates is not the only factor in reduction of renal clearance. Thus the degree of substitution desirable for individual targets will have to be assessed on a case-by-case basis.

Table 4(A)

Coupling Ratios and Compositions for PEGylated GM-CSF Preparations

PREPARATION	GM-CSF (μg/ml)	TMPEG (mg/ml)	GM-CSF (dose, μg)	TMPEG (dose, mg)
Unmodified Control	0.524	0	0.0524	0
Reaction A	0.524	6.46	0.0524	0.646
Reaction B	0.524	19.75	0.0524	1.975
Reaction C	0.524	197.5	0.0524	19.75
Reaction D	0.524	459.7	0.0524	45.97

Table 4(B)

Percentage of GM-CSF in different fractions at various coupling reactions.

	Unmodified GM-CSF (Peak 0)	PEG-modified-GM-CSF			
		Peak-1	Peak-2	Peak-3 & higher	Putative Aggregates
Unmodified Control	100	0.0	0.0	0.0	0.0
Reaction A	48.6	27.7	14.1	3.1	0.0
Reaction B	31.0	26.0	21.6	8.0	1.6
Reaction C	16.8	23.5	15.9	19.2	20.7
Reaction D	11.1	37.7*			51.2

* Combined data for all PEG-GM-CSF Peaks (incompletely resolved)

Table 5

Half-life of late clearing components in PEGylated (GM-CSF) preparations).

	$t_{1/2}$ (hours)	$t_{1/2}$ + SE*	$t_{1/2}$ -SE*
Unmodified Control	1.63	1.81	1.47
Reaction A	11.7 (7.2)	14.0 (8.6)	10.1 (6.2)
Reaction B	18.1 (11.1)	23.1 (14.2)	14.8 (9.1)
Reaction C	16.8 (10.3)	17.3 (10.6)	16.4 (10.1)
Reaction D	25.1 (15.3)	26.0 (15.9)	24.2 (14.8)

* calculated from the slope of the regression of log concentration versus time over portions of dose response curves (shown in fig.6(a)), ± the standard error of the slope.

Figures in parentheses indicate the fold increase over the control figure.

Example 11.

A direct comparison using a 2h. coupling period and a molar ratio of activated PEG:lysine of 305:1 gave the following results (assessing modification by phase partitioning as described by Delgado (1990)) is shown in Table 6.

Table 6

PEGYLATION METHOD	PARTITION COEFFICIENT
Unmodified Control	1.54±0.07
The present invention (TMPEG)	4.77±0.04
Cyanuric Chloride	9.0±0.74*
Carbonyldiimidazole	2.06±0.14
Phenylchloroformate	4.92±0.02
Succinimidyl succinate	3.35±0.25

* Result compounded by the presence of large amounts of cross-linked products for which log K will not be a linear function of modification.

These results demonstrate that a fast reaction rate is achieved with the present invention so that there is less time for a target material to be damaged by the possibly hostile environment of the coupling reaction.

Example 12

After storage at 4°C, ^{125}I-GM-CSF shows degradation with the appearance of label in low molecular weight material. This process is slowed by PEG modification. Fig.7 shows FPLC profiles of representative examples stored for 1 day (upper panels) and 33 days (lower panels). When supplied, ^{125}I-GM-CSF has little or no low molecular weight labelled species. After storage for 1 day of an unmodified (open circles) preparation and a modified preparation (exposed to TMPEG at a molar ratio of 305:1 as described

above, filled circles) there was a small amount of labelled low molecular weight material (peak 3) in both preparations. In both, the majority of the material (peak 1) is high molecular weight (the size distribution difference is commensurate with the PEGylation of the intact protein and the low molecular weight material probably represents free iodine). After storage the low molecular weight peak had increased substantially and a second peak (peak 2) had appeared between it and the peak of unmodified material (lower panel). There has been generation of intermediate and low molecular weight fragments in both samples. The former are commensurate in size with proteolytic cleavage products and the latter either with free iodine or very small fragments (i.e. < circa 1kDa). The relative amounts of ^{125}I in the samples is listed in the Table 7. Pegylation reduces the loss of high molecular weight species.

Table 7

	Peak	Before Storage	After 1 Month Storage
GM-CSF	1	76.1	9.2
	2	0	20.6
	3	21.5	68.2
PEG-CM-CSF	1	81.1	45.8
	2	0	8.9
	3	12.4	36.3

Example 13

Dry stored TMPEG, prepared as in Example 1 above, derived from an MPEG preparation (Union Carbide UK) contaminated with circa 22% PEG (when estimated by NMR) was used in this Example. This contaminating PEG results (during the polymer activation process) in the formation of biactivated tresyl PEG which produces aggregates in the final product; the formation of aggregates can be reduced by reducing the level of contamination of the MPEG preparation by PEG. The erythropoietin (EPO) preparation used was a commercial preparation obtained from Cilag Ltd and the erythropoietin stock contained 3200 u/ml in PBS. This preparation contains 3200 units of EPO, and 2 mg/ml of human serum albumin. The coupling ratios were calculated on the basis of the total number of available lysine groups in the erythropoietin and carrier protein, and would need to be adjusted accordingly for pure erythropoietin preparations. The erythropoietin preparation was exposed to the stated molar ratios of TMPEG:lysine and was incubated at room temperature for two hours on a rotary mixer. The sham-reacted control was similarly exposed to diluent, (PBS). The resulting samples were analysed by FPLC the profiles being shown in Fig.8 panels A to F; the vertical axis in all cases is C.P.M.[^{125}I]-erythropoietin: A) Sham treated;B to F TMPEG:lysine at ratios B)9.375:1; C) 18.75:1; D) 37.5:1; E) 75:1; F) 305:1

Samples (200μl containing circa 10.5μg/ml total proteins) were analysed on a Pharmacia FPLC system with a Superose 12 HR 10/30 column previously equilibrated with PBS. The samples were loaded onto the column and then eluted with sterile PBS at a flow rate of 0.3ml per minute; 0.25ml fractions were collected. To monitor protein profiles, PEG-EPO was prepared using [^{125}I]-erythropoietin (Amersham) and fractions were analysed using a gamma counter (Nuclear Enterprises NE1600). To check the biological activity of a series of preparations made using the same TMPEG preparation, over a similar range of molar ratios of TMPEG:lysine, using unlabelled EPO (Cilag), serial dilutions of the unfractionated reaction mixture were exposed to the haemopoietic cell-line, TF-1, to induce thymidine uptake. Cultures were performed in microtitre plates containing 50 μl of cell suspension (5 x 10^4 cells/well) in RPMI-1640 medium containing 5% foetal calf serum (FCS) in round bottom microwell plates (NUNC). To increase sensitivity of TF-1 cells to cytokine, they were deprived of their maintenance growth stimulus (GM-CSF at 50 units/ml) for 24 hours prior to assay. Each well contained either PEG-erythropoietin or unmodified erythropoietin, diluted in RMPI-1640. Cultures were incubated in a humidified atmosphere of 5% carbon dioxide in air at 37°C for 18 h. Cells were then exposed to 0.5μCi of [methyl-^{3}H]thymidine 25Ci/mmol. Amersham) in 50μl of culture medium and incubation was continued as above for 4 h. Cells were

harvested onto glass filters (Titertek Flow labs) using a Dynateck multimesh 2000 harvester, washed with methanol and dried for 12 h at room temperature. [^{3}H]-thymidine incorporation was determined by scintillation counting (Beckman LS 5000 CE) using 5ml Filter Count (Packard) the results being expressed as D.P.M. of the test sample minus D.P.M of unstimulated cells; negative values therefore indicate inhibition of background thymidine uptake.

Fig.9a shows the induction of thymidine uptake by all preparations, both PEG-modified and unmodified. Fig. 9b shows the early portion of the dose-response curves for concentrations less than one unit/ml at expanded scale to facilitate comparison. All preparations produced stimulation of incorporation of thymidine, but there is a progressive contamination by inhibitory material, whose activity is most evident at 3 and 10 units/ml of erythropoietin. The inhibitor is related to the TMPEG:lysine molar ratio suggesting that either TMPEG itself or co-product is responsible (TMPEG does have an inhibitory effect in this assay system [Malik (1992)]. This inhibitory material was not evident to a similar degree in PEG-GM-CSF preparations, even those prepared with the same batch of TMPEG, and its nature has not yet been determined but may reflect altered sensitivity of the cell line to inhibition under different growth conditions. The similarity of the upward portion of the dose-response curves indicates that there is little inherent loss of

biological activity for all the preparations studied.

Example 14

NMR analysis showed that a standard preparation of MPEG-5000 (kindly donated by Union Carbide) contained 23.5 mole % PEG and 76.5 mole % MPEG. Method: 1H-nmr spectra were acquired on a Brucker WN 259 spectrometer on polymer samples in DMSO-d_6 (50mg/ml). Integrations of the peaks at 4.56ppm (OH), 3.56 ppm (CH_2CH_2O) and at 3.26 ppm (OCH_3) were made and used to calculate the PEG and MPEG contents (also the molecular mass of the sample which was 5200Da).

PEG contamination results from its production as a by-product during the polymerisation reaction for the manufacture of MPEG (hydroxide used to catalyse the reaction, initiates a side reaction yielding PEG). Since PEG has two termini at which polymerisation can take place, it should achieve a larger molecular weight than that of the MPEG. These data confirm that this side reaction takes place largely during the early phase of the reaction, since the size distribution of the PEG product is approximately double that of the MPEG product and there is no substantial proportion of material spanning a range of intermediate sizes (as would be anticipated if the side reaction continued throughout the polymerisation).

To confirm that the contaminating PEG is, as anticipated, responsible for aggregate formation during the

coupling reaction, a TMPEG preparation derived from the same MPEG preparation analysed above was fractionated on the expectation that it would contain circa 25.5% bi-activated PEG. [Such fractionation requires prolonged exposure to an aqueous environment and resulted in some overall loss of activity (thus requiring appropriate sham-treatment of unfractionated controls) and is therefore not advisable as a step in the process of the invention, rather purification prior to activation is recommended]. The TMPEG was then exposed to ^{125}I-gm-CSF under standard coupling conditions as described over a range of molar ratios as indicated in Table 8 (aggregate formation is more likely at higher molar ratios and/or concentrations of polymer and target). Aggregates were identified by FPLC on Superose 12 (as labelled material eluting with the void volume) and PEG-modified GM-CSF species (as labelled material eluting faster than unmodified GM-CSF, but not as fast as the aggregated material). This identification has been confirmed independently by phase partitioning. The fractionation by vesicle chromatography separates material less prone to produce aggregates (permeable fraction) and more prone (excluded fraction) than the starting material respectively. This validates two points; first that the PEG becomes biactivated and second that the reduction of the contaminating PEG by size fractionation will reduce he amount of aggregates. Since the acceptable level of aggregates will vary from application to application a

limit for contamination of MPEG by PEG will have to be selected on a case-by-case basis.

Table 8

Reduction of PEG contamination reduces aggregate formation. Aggregates are expressed as % total PEG-modified material (aggregates + PEG_n-gm-CSF where n=1-7)

Table 8

	Unfractionated MPEG	Permeable Fraction	Excluded Fraction
PREP 1 (150:1 TMPEG:lysine)			
Aggregates	21.6	6.1	N.T.
PREP 2 (120:1) TMPEG:lysine)			
Aggregates	17.9	0	N.T.
PREP 3 (17:1 TMPEG:lysine)			
Aggregates	0	0	13.3

N.T. = Not Tested

Claims

1. A process for producing an adduct of a polymer and a target material which process comprises the steps of

(a) reacting either

(i) an activating compound of formula (I)

X-AM (I)

wherein

-AM is an activating sulphonyl ester moiety optionally bearing a group for covalent bonding to a solid support, the solvolysis substituent constant of the group -AM being less than that of the trifluoromethane sulphonate group, and

X is a leaving group

or

(ii) reacting a solid support bearing moieties of formula (I')

X-AM'- (I')

wherein

-AM'- is activating sulphonyl ester moiety covalently bound to the solid support, the group -AM'- being such that the solvolysis substituent constant of the group -AM'- is less than that of the trifluoromethane sulphonate group, and

X is as defined above

with a polymer of formula (II)

$$(C)_c\ POL - G_g \qquad (II)$$

wherein

POL is a polymer moiety of valency c+g,

C is a capping group and c is zero or a positive number and

G is a terminal hydroxyl group reactive with the compound of formula (I) and g is a positive number

so as to form

(i) a sulphonate ester-activated polymer of formula (III)

$$(C)_c\ POL - (AM)_g \qquad (III)$$

wherein

C, POL, -AM, c and g are as defined above

and the group(s) -AM are linked to termini of the polymer as sulphonate esters of terminal hydroxyl groups

or

(ii) a solid support-bound, sulphonate ester-activated polymer of formula (III')

$$[(C)_c\ POL-\ (AM')_g]_z \qquad (III')$$
$$\quad\ |$$
$$\quad SS$$

wherein

C, POL, -AM'-, c and g are as defined above,

SS is a solid support and z is the number of sulphonate ester-activated polymer moieties on the solid support and

the groups -AM'- are linked to termini of the polymer as sulphonate esters of terminal hydroxyl groups,

and, when -AM bears a group for covalent bonding to a solid support, reacting the sulphonate ester-activated polymer of formula (III) with a solid support to form a solid support-bound, sulphonate ester-activated polymer of formula (III') as defined above

(b) reacting the sulphonate ester-activated polymer of formula (III) or (III') with the target material and

(c) recovering the adduct of the polymer and the target material,

in which process:

(i) the polymer of formula (II) is dry as determined by benzene distillation,

(ii) the reaction of the compound of formula (I) or (I') with the polymer of formula (II) is conducted in an organic solvent which is inert to the reagents and to the product of formula (III) or (III') and is anhydrous as obtainable using molecular sieves of 0.3nm;

(iii) the reaction of the compound of formula (I)

or (I′) with the polymer of formula (II) is conducted in a reaction vessel from which water is excluded;

(iv) the sulphonate ester-activated polymer of formula (III) or (III′) so produced is recovered and either used directly in step (b) or stored, prior to use in step (b), in the presence of a desiccating agent more hygroscopic than the product of formula (III) or (III′); and

v) the reaction of the sulphonate ester-activated polymer with the target material is conducted in a non-denaturing medium and non-denaturing temperature with respect to the target material.

2. A process according to claim 1 which is conducted in the liquid phase, using a compound of formula (I) in step (a).

3. A process according to claim 1 which is conducted at a solid:liquid interface, using a solid support-bearing at least one moiety of formula (I′) in step (a).

4. A process according to any one of claims 1 to 3 comprising, in step (b), reacting, in predetermined molar ratio and at predetermined concentrations, a sulphonate ester-activated polymer having two moieties -AM with a first target material (target^1), so as to produce a sulphonate ester-activated 1:1 adduct of polymer and target^1, then reacting the 1:1 adduct with a second target material (target^2) so as to produce a target^1:polymer:target^2 adduct, wherein the first and second

target materials may be the same or different, and then recovering the adduct in accordance with step (c).

5. A process according to any one of claims 1 to 3 comprising reacting a sulphonate ester-activated polymer bearing a plurality of activating sulphonyl moieties -AM with a first target material, wherein the proportion of the activating sulphonyl moieties -AM on the sulphonate ester-activated polymer which react with the first target material is controlled such that in at least a proportion of the molecules of intermediate polymer:target adduct produced there remain unreacted activating sulphonyl moieties -AM, and wherein such unreacted reactive groups -AM are then reacted with one or more different further target materials so as to form materials polymer:$[target]_n$ wherein n is 2 or more and the first and further target entities are different; or the unreacted activating sulphonyl moieties are reacted with more of the first target material so as to form materials polymer:$[target]_n$ wherein n is 2 or more and the target entities are all the same; or the unreacted activating sulphonyl moieties are reacted with further unreacted groups in the first target entity of the intermediate polymer:target adduct under conditions which hinder intermolecular reactions, such that the polymer moieties are bonded at two or more positions to the target entity.

6. A process according to any one of claims 1 to 3 comprising, in step (b), reacting, in predetermined molar ratio and at predetermined concentrations, a sulphonate ester-activated polymer having only one moiety -AM or -AM'- with a target material having more than one reactive group so as to form an adduct of the polymer and target having a preselected number of polymer molecules per molecule of target, or having a preselected proportion of the reactive groups reacted with and linked to polymer molecules, and

then recovering the adduct in accordance with step (c).

7. A process according to any one of claims 1 to 3 comprising, in step (b), reacting, in predetermined molar ratio and at predetermined concentrations, a sulphonate ester-activated polymer having two or more activating sulphonyl moieties -AM with a target material having two or more reactive groups so as to produce a sulphonate ester-activated 1:1 adduct of polymer and target then changing the reaction conditions so as to hinder intermolecular reactions whilst permitting intramolecular reactions between activating sulphonyl moities -AM on the polymer and reactive groups on the target so as to form adducts of polymer and target having two or more covalent bonds between the polymer and target moieties, and then recovering the adduct in accordance with step (c).

8. A process according to any preceding claim wherein X is halogen.

9. A process according to any preceding claim wherein X is chlorine.

10. A process according to any preceding claim wherein the activating moiety -AM is selected from:

2,2,2-trifluoroethanesulphonyl,
pentafluorobenzenesulphonyl,
fluorosulphonyl,
2,4,5-trifluorobenzenesulphonyl,
2,4-difluorobenzenesulphonyl,
2-chloro-4-fluorobenzenesulphonyl,
3-chloro-4-fluorobenzenesulphonyl,
4-amino-3-chlorobenzenesulphonyl,
4-amino-3-fluorobenzenesulphonyl,
o-trifluoromethylbenzenesulphonyl,
m-trifluoromethylbenzenesulphonyl,

p-trifluoromethylbenzenesulphonyl,
2-trifluoromethoxybenzenesulphonyl,
4-trifluoromethoxybenzenesulphonyl, and
5-fluoro-2-methylbenzenesulphonyl groups.

11. A process according to claim 10 wherein the group -AM is a 2,2,2 trifluoroethane-sulphonyl group.

12. A process according to any one of claims 1 to 9 wherein the activating moiety -AM is a 2',3',5',6'-tetrafluoro-4-amino-phenyl-azobenzene-4'-sulphonic halide.

13. A process according to claim 12 wherein -AM is 2',3',5',6'-tetrafluoro-4-amino-phenyl-azobenzene-4'-sulphonic chloride.

14. A process according to any preceding claim wherein the polymer is selected from polyalkylene compounds, polyvinyl compounds, polyacrylic compounds, polyionic compounds, polyalkylene polyols, non-ionic surfactants, polyamino acids, synthetic polypeptides, polysaccharides, crosslinked products thereof and polysaccharide containing material, other organic polymers and inorganic polymers and block copolymers thereof.

15. A process according to claim 14 wherein the polymer is selected from poly(oxymethylene), polyethyleneglycols and oxides, methoxypolyethyleneglycols, polymethylethylene-glycol, polyhydroxypropyleneglycol, polypropyleneglycols and oxides, polymethylpropyleneglycol, polyhydroxy-propyleneoxide, straight-chain and branched-chain polypropyleneglycols and derivatives thereof, polyethyleneglycol and polypropyleneglycol and the monomethyl ethers, monocetyl ethers, mono-n-butyl ethers, mono-t-butylethers and monooleyl ethers thereof, esters of polyalkyleneglycols with carboxylic acids and dehydration

condensation products of the polyalkyleneglycols with amines and other polyalkylene oxides and glycols and derivatives thereof, poly (vinylpyrrolidone), polyvinyl alcohol, poly (vinyl acetate), the copolymer poly (vinyl acetate-co-vinyl alcohol), polyvinyloxazolidone, poly (vinylmethyloxazolidone and poly (vinyl methyl ether), poly(acrylic acid)s, poly(methacrylic acid)s, polyhydroxyethylmethacrylates, Poly(acrylamide and poly(methacrylamide) and other amides thereof, poly(N,N-dimethylacrylamide), poly(N-isopropylacrylamide), poly(N-acetamidoacrylamide) and poly(N-acetamidomethacrylamide, and other N-substituted derivatives of the amides, poly(ethyleneimine), poly(ethylsulphonic acid), poly(silicic acid), poly(styrenesulphonic acid), poly(vinyl amine), poly(2-vinylpyridine) and its N-alkyl derivatives, poly (4-vinylpyridine) and its N-alkyl derivatives, poly(vinylsulphuric acid), poly(vinyl alcohol-co-vinyl sulphuric acid), poly(diallyldimethylammonium chloride), poly((dimethylimino) trimethylene(dimethylimino)hexa-methylene dibromide), poly(ethylenephosphonic acid), poly(maleic acid), poly(2-methacryloyloxyethane-1-sulfonic acid), poly-(3-methacryloyloxypropane-1-sulfonic acid), poly(4-vinylbenzoic acid), poly(4-vinylbenzyl-trimethylammonium), poly[3-(vinyl-oxy)propane-1-sulphonic acid)], poly(4-vinylphenol)(poly[p-hydroxystyrene]), poly(4-vinylphenyl sulphuric acid), poly-(2-vinyl piperidine), poly(4-vinylpiperidine), poly(N-vinyl-succinamidic acid), polyoxyethylated glycerol, polyoxyethylated sorbitol, poly sorbates and polyoxyethylated glucose, polyoxyethylene-alkylphenols, polyoxyethylenemercaptans, polyoxyethylene- alkylamines, polyoxyethylene-alkylamides, polymers of D-glutamic acid and D-lysine, polylysine, polyalanine, polyglutamic acid, polyaspartic acid, polyproline, branched or unbranched polysaccharides comprising saccharide monomers selected from glucose, mannose, galactose, fucose,

fructose, xylose, arabinose, glucuronic acid, sialic acid (neuraminic acid), galacturonic acid, mannuronic acid, D-glucosamine and galactosamine, dextran, dextran sulphate, p-aminoethyl cross-linked dextran, carboxymethyl dextran and other dextran derivatives, cellulose, methyl cellulose, carboxymethyl cellulose and other cellulose derivatives, starches (amylopectin and amylose) and dextrins derived from starch, hydroxyethyl starches, agarose, ficoll and its carboxy methyl derivatives, glycosaminoglycan chains of proteoglycans selected from hyaluronic acid, chondroitin sulphates, dermatan sulphate, heparin, heparin fragments, heparin oligosaccharides, heparan sulphate and keratan sulphate, carbohydrate-containing side chains of glycoproteins and glycolipids selected from gangliosides, globosides and sulphatides, polysorbitol, polymannitol and other polymers of sugar alcohols, polysaccharides selected from glycogen, glucans, laminaran and glycosaminoglycans, polysaccharide sidechains of glycoproteins and glycolipids, alginic acid, polymannuronic acid, carrageenan, agar and other sulphated polysaccharides, and other algal polysaccharides, pectins, plant gums, guaran and other seed mucilages, xanthans, gellan, alginate, scleroglucan, schizophyllan, curdlan, pullulan and other bacterial and fungal polysaccharides, polymers and copolymers of amines, olefins, esters, acetal, polyamides, carbonates, ethers and phenylene sulphides, silicones, urea formaldehyde condensation products, phenol formaldehyde condensation products, urethanes, melamine formaldehydes, epoxy resins, acrylic resins, allyl resins, polyacrylic acid and carbomers, silicates and other inorganic polymers containing organic moieties, block copolymers of polyethylene/ polypropylene-glycol, block copolymers of ethylene and maleic anhydride, block copolymers of polyalkylene glycols and polyvinylpyrrolidone or polyvinyl alcohol, block copolymers of polyoxyethylene and polyoxy-propylene, block copolymers of the ethers, esters or

dehydration condensation products of polymers of ethylene glycol and propylene glycol, and block copolymers of acrylamide and acrylic acid.

16. A process according to any preceding claim wherein the target is selected from proteins, antibodies and fragments thereof, , IL-1, IL-2, IL-3, IL-4, IL-5, IL-6, IL-7, IL-8, IL-9, IL-10, IL-11 and other interleukins and subtypes thereof, and other cytokines and derivatives or fragments thereof, granulocyte-macrophage colony stimulating factor, the alpha and beta forms of granulocyte-colony stimulating factor, macrophage-colony stimulating factor, and other colony stimulating factors, erythropoietin, haemopoietin-alpha and kit-ligand and other haemopoietins, IFNalpha, IFNbeta and IFNgamma and other interferons, epidermal growth factor, platelet derived growth factor, transforming growth factor (alpha and beta forms), amphiregulin, somatomedin-C, bone growth factor, fibroblast growth factors, insulin-like growth factors, heparin binding growth factors, tumour growth factors and other growth factors and bifunctional growth modulators, macrophage differentiating factor, differentiation inducing factor (DIF), leukaemia inhibitory factor and other differentiation factors, platelet activating factor, macrophage activation factor, and other activating factors, heparin, proteases and their pro-factors, clotting factors VII, VIII, IX, X, XI and XII, antithrombin III, protein C, protein S, streptokinase, urokinase, prourokinase, tissue plasminogen activator, fibrinogen, hirudin, other fibrinolytic/anticoagulant agents and other coagulation factors, peptide hormones, enzymes, vaccines, transcription factors and transcriptional modulators, carbohydrates, glycosoaminoglycans, glycoproteins and polysaccharides, phosphatidylethanolamine and phosphatidylserine and derivatives thereof, sphingosine, cholesterol and other steroids and derivatives thereof, nucleotides, nucleosides,

heterocyclic bases, DNA, RNA, synthetic and non-synthetic oligonucleotides, vitamins, antibiotics, bacteristatic and bactericidal, antifungal, anthelminthic agents, noradrenalin, alpha adrenergic receptor ligands, dopamine receptor ligands, histamine receptor ligands, GABA/benzodiazepine receptor ligands, serotonin receptor ligands, leukotrienes and tri-iodothyronine and other small effector molecules, doxorubicin, methotrexate and other cytotoxic agents and derivatives thereof.

17. A process according to any one of the preceding claims comprising the steps of

(a) reacting dry MPEG (as determined by benzene distillation) containing less than 10% by weight of PEG (as determined by nmr and/or chromatography) with tresyl chloride in dry dichloromethane (as determined using 0.3 nm molecular sieves) in the presence of pyridine in a reaction vessel from which water is excluded, so as to form TMPEG, recovering the TMPEG so formed and either storing it over phosphorus pentoxide or using it directly in step (b),

(b) reacting the TMPEG so formed, optionally after storage, with a target material such as erythropoietin (EPO) in aqueous medium and about 20°C and

(c) recovering the Target:MPEG adduct (eg EPO:MPEG) so formed.

18. A polymer:target adduct obtainable by the process of any one of the preceding claims, having polymer and target moieties directly linked by stable, non biodegradable covalent bonds.

19. A liposome bearing linear polymeric linking groups bound to the surface of the liposome at one terminal of the polymer and bearing a receptor ligand, receptor molecule, antibody, antigen or other molecule of therapeutic or diagnostic interest at the other terminal.

20. A construct comprising a plurality of target molecules linked to a single polymer moiety, the polymer being a linear polymer having two reactive termini linked to two target molecules or being a branched polymer having three or more reactive termini or a polymer having reactive pendant groups linked to three or more target molecules so as to enhance the biological activity thereof.

21. A construct according to claim 20 wherein the target molecules are different.

22. A construct comprising a polymer moiety linked to a target molecule at both termini of a linear polymer or to two or more pendant reactive groups of a polymer or the termini of a branched polymer, at two, three or more sites on the target molecule.

23. A product for use in a therapeutic or diagnostic method of treatment of the human or animal body.

24. Use of a product in the manufacture of a medicament for use in a therapeutic or diagnostic method of treatment of the human or animal body.

25. A pharmaceutical composition comprising a product according to any one of claims 18 to 22 or produced in accordance with the process of any one of claims 1 to 17 or obtainable by the process of any one of claims 1 to 17 together with pharmaceutically acceptable diluents or carriers.

Abstract

Polymer modification

A process for producing adducts of a polymer and a target material which process comprises the steps of

(a) reacting either

(i) an activating compound of formula (I)

X-AM (I)

wherein

-AM is an activating sulphonyl ester moiety optionally bearing a group for covalent bonding to a solid support, the solvolysis substituent constant of the group -AM being less than that of the trifluoromethane sulphonate group, and

X is a leaving group

or (ii) reacting a solid support bearing moieties of formula (I')

X-AM'- (I')

wherein

-AM'- is an activating sulphonyl ester moiety covalently bound to the solid support, the group -AM'- being such that the solvolysis substituent constant of the group -AM'- is less than that of the trifluoro- methane sulphonate group, and

X is as defined above

with a polymer of formula (II)

$$(C)_c\ POL - G_g \qquad (II)$$

wherein

POL is a polymer moiety of valency c+g, C is a capping group and c is zero or a positive number and

G is a terminal hydroxyl group reactive with the compound of formula (I) and g is a positive number so as to form

(i) a sulphonate ester-activated polymer of formula (III)

$$(C)_c\ POL - (\ddot{AM})_g \qquad (III)$$

wherein

C, POL, -AM, c and g are as defined above and in which the group(s) -AM are linked to termini of the polymer as sulphonate esters of terminal hydroxyl groups

or (ii) a solid support-bound, sulphonate ester-activated polymer of formula (III')

$$[(C)_c\ POL\text{-}\ (AM')_g]_z \quad (III')$$
$$\Big|$$
$$SS$$

wherein

C, POL, -AM'-, c and g are as defined above,

SS is a solid support and z is the number of sulphonate ester-activated polymer moieties on the solid support

and the groups -AM'- are linked to termini of the polymer as sulphonate esters of terminal hydroxyl groups,

and, when -AM bears a group for covalent bonding to a solid support, reacting the sulphonate ester-activated polymer of formula (III) with a solid support to form a solid support-bound, sulphonate ester-activated polymer of formula (III') as defined above

(b) reacting the sulphonate ester-activated polymer of formula (III) or (III') with the target material and

(c) recovering the adduct of the polymer and the target material,

in which process:

(i) the polymer of formula (II) is dry as determined by benzene distillation,

(ii) the reaction of the compound of

formula (I) or (I') with the polymer of formula (II) is conducted in an organic solvent which is inert to the reagents and to the product of formula (III) or (III') and is anhydrous as obtainable using molecular sieves of 0.3nm;

(iii) the reaction of the compound of formula (I) or (I') with the polymer of formula (II) is conducted in a reaction vessel from which water is excluded;

(iv) the sulphonate ester-activated polymer of formula (III) or (III') so produced is recovered and either used directly in step (b) or stored, prior to use in step (b), in the pesence of a desiccating agent more hygroscopic than the product of formula (III) or (III'); and

(v) the reaction of the sulphonate ester-activated polymer with the target material is conducted in a non-denaturing medium and non-denaturing temperature with respect to the target material.

Fig.1a.

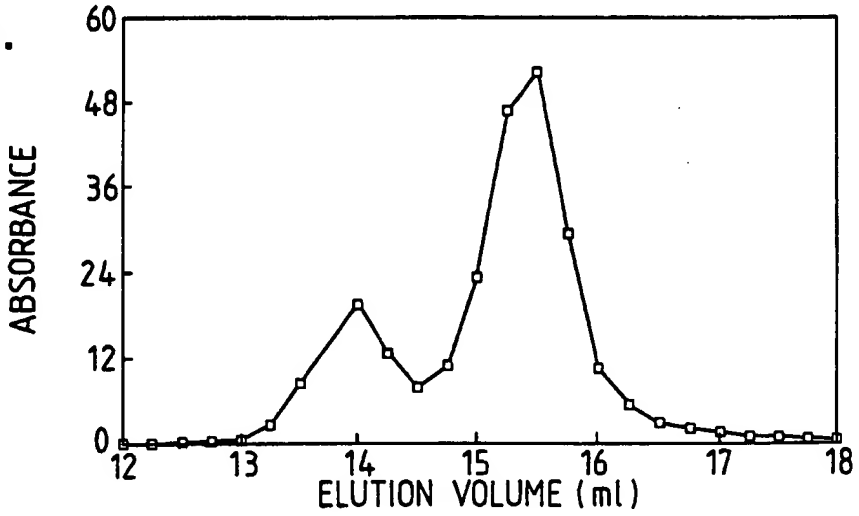


Fig.1b.

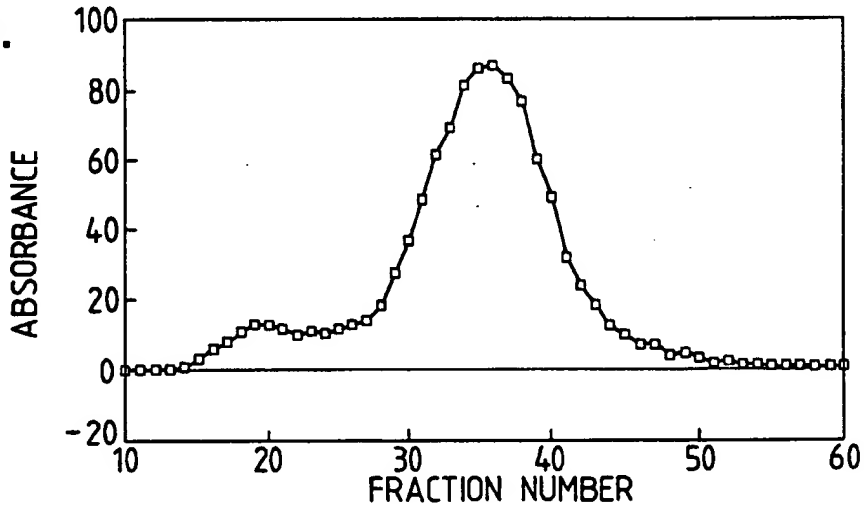


Fig.1c.

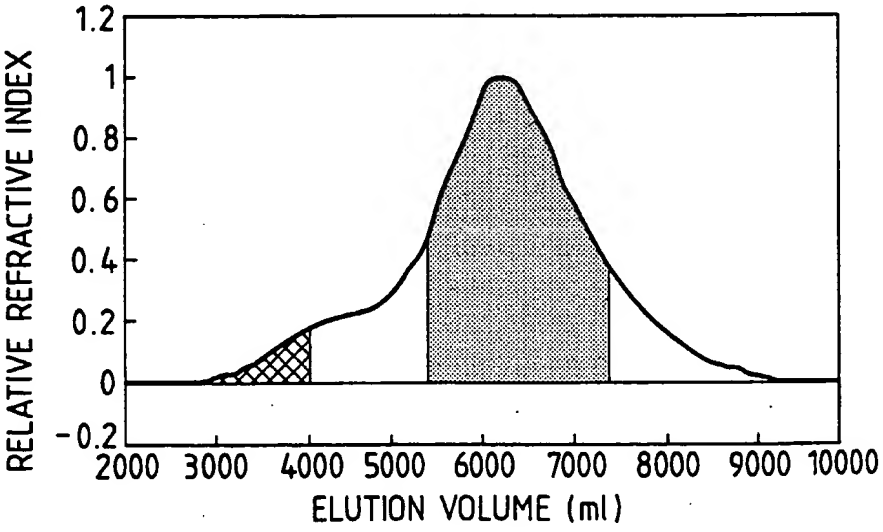


Fig.1d.

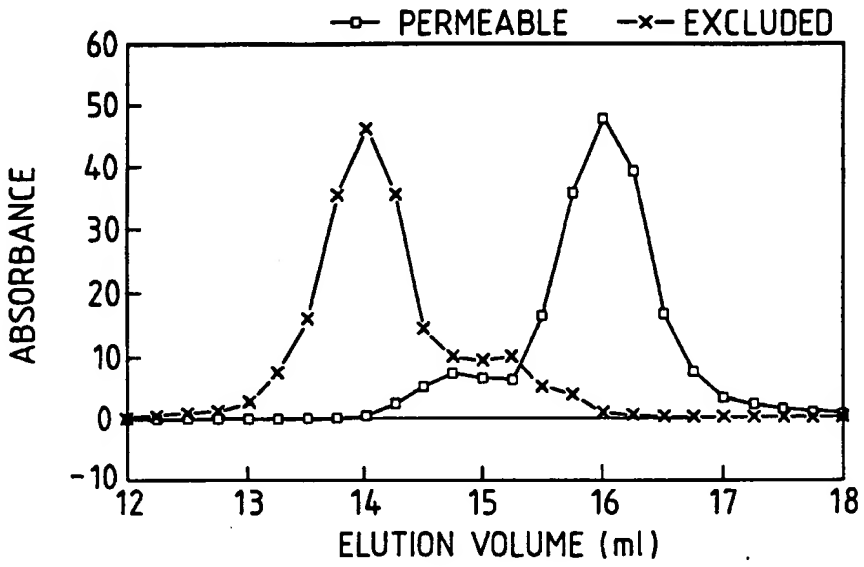

PERMEABLE
EXCLUDED
ABSORBANCE
60
50
40
30
20
10
0
-10
12
13
14
15
16
17
18
ELUTION VOLUME (ml)

Fig.1e.

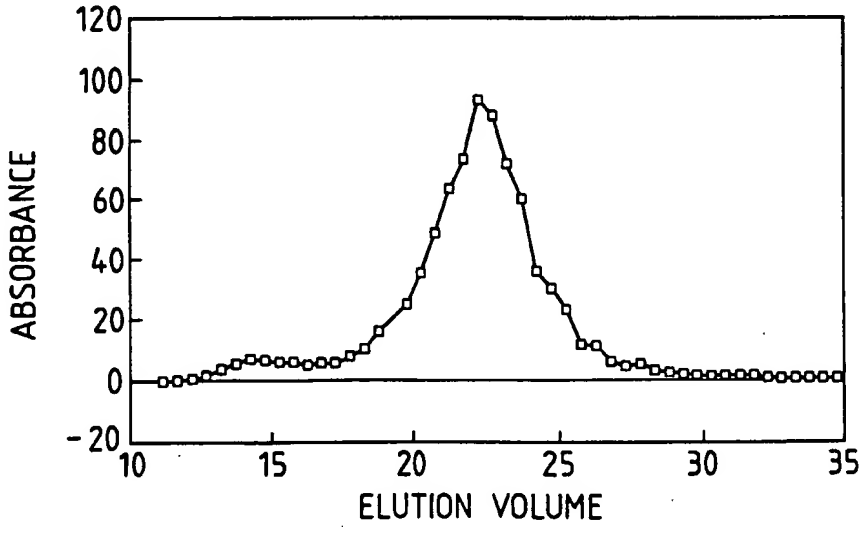

ABSORBANCE
120
100
80
60
40
20
0
-20
10
15
20
25
30
35
ELUTION VOLUME

Fig.2.

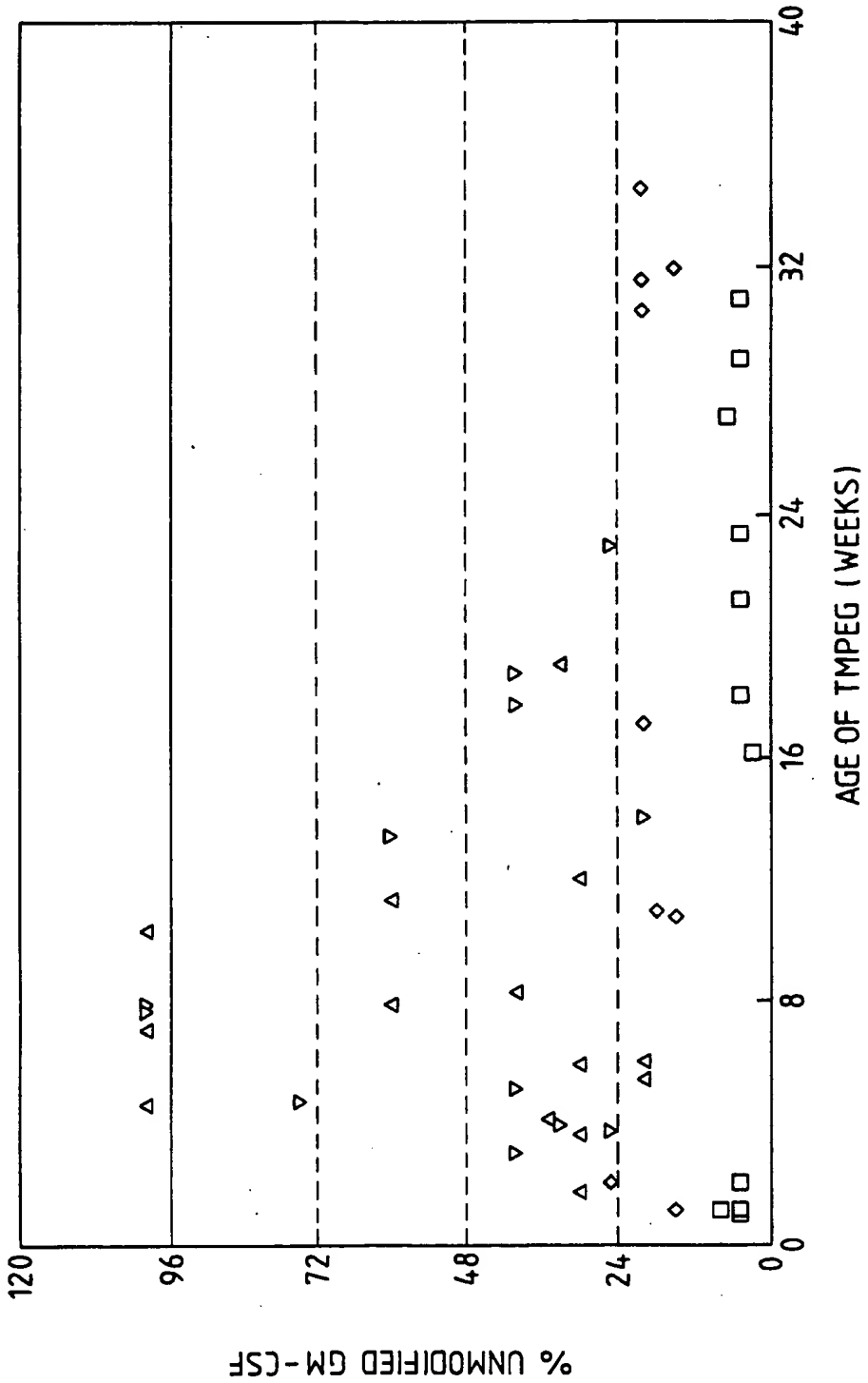

120
96
72
48
24
0
% UNMODIFIED GM-CSF
0
8
16
24
32
40
AGE OF TMPEG (WEEKS)

Fig.3a.

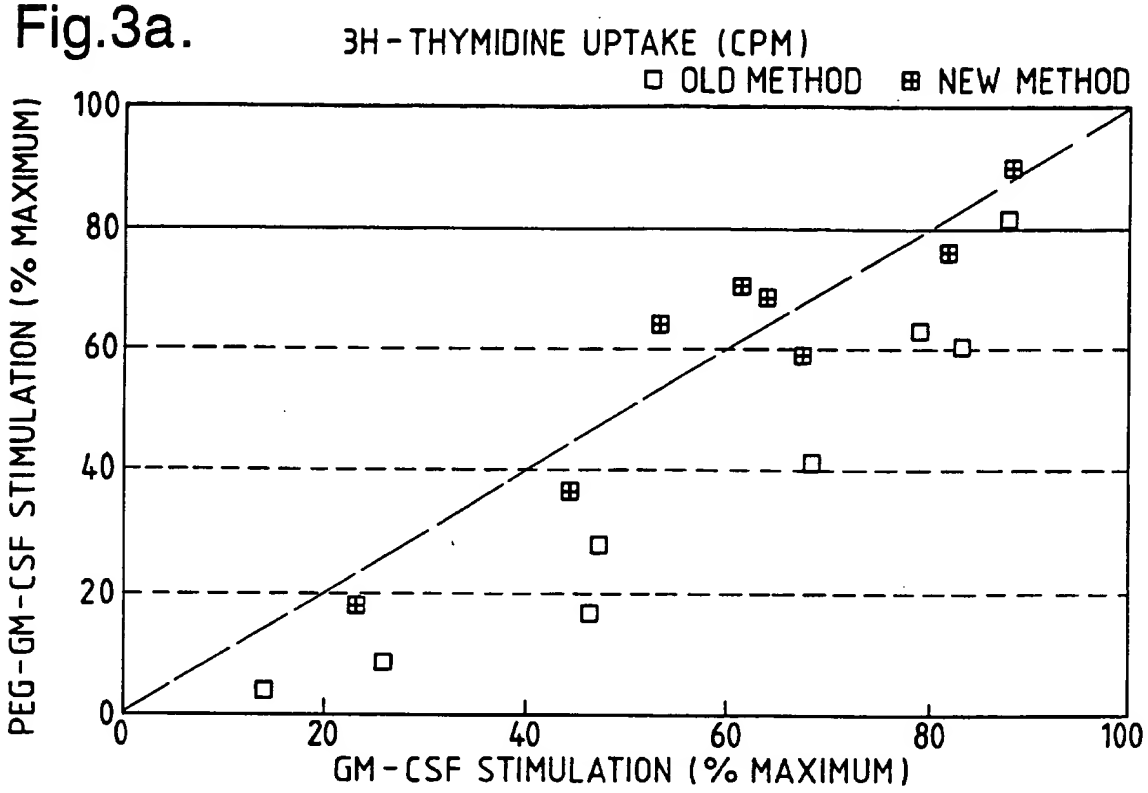
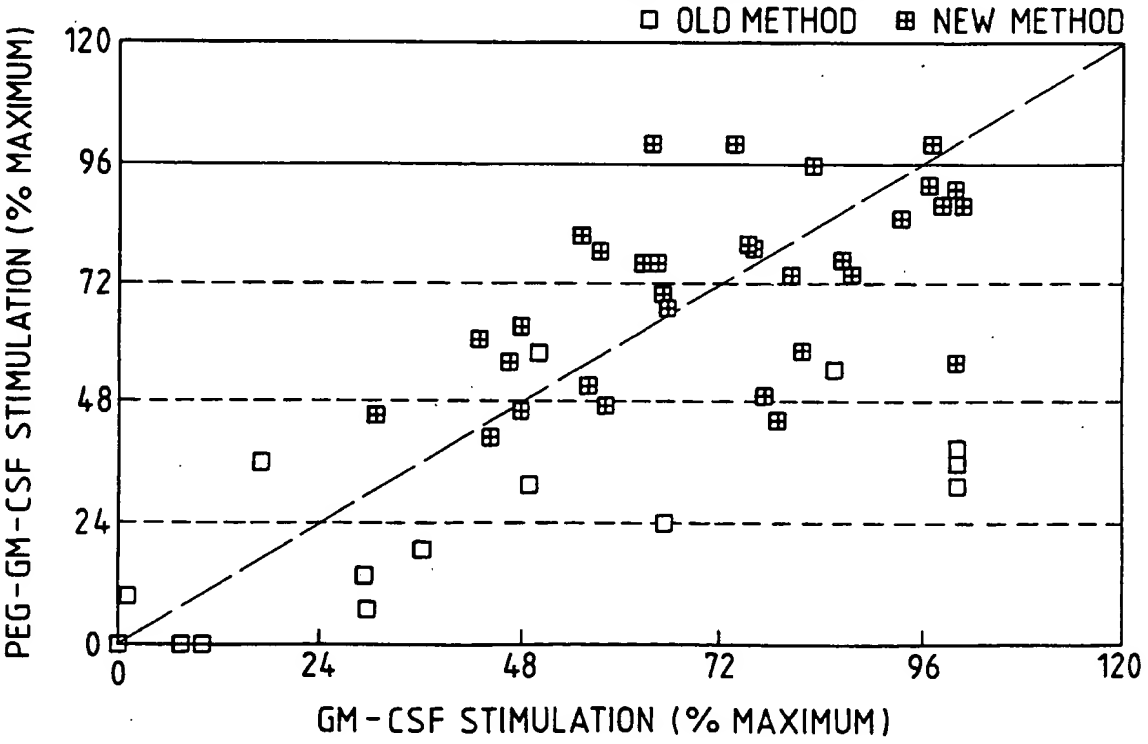

3H-THYMIDINE UPTAKE (CPM)
OLD METHOD
NEW METHOD
PEG-GM-CSF STIMULATION (% MAXIMUM)
GM-CSF STIMULATION (% MAXIMUM)
0
20
40
60
80
100

Fig.3b.


GRANULOCYTE-MACROPHAGE COLONIES
OLD METHOD
NEW METHOD
PEG-GM-CSF STIMULATION (% MAXIMUM)
GM-CSF STIMULATION (% MAXIMUM)
0
24
48
72
96
120

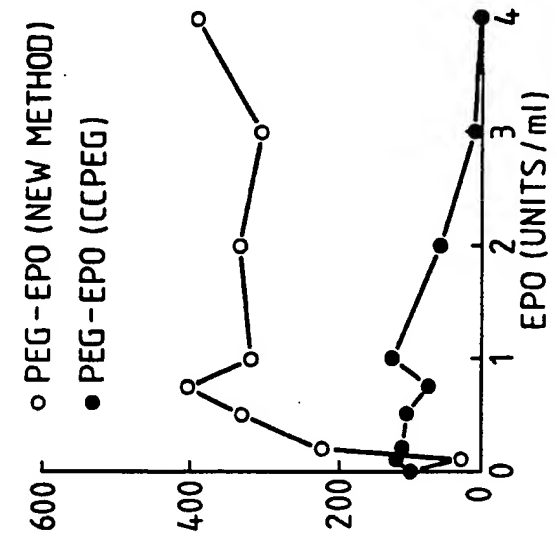


Fig.4b.

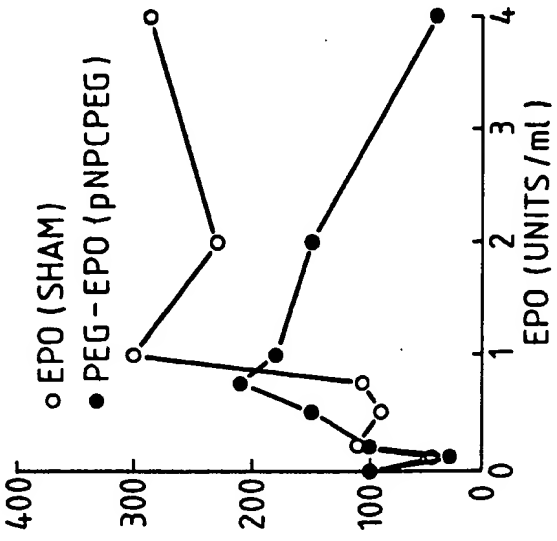


Fig.4d.

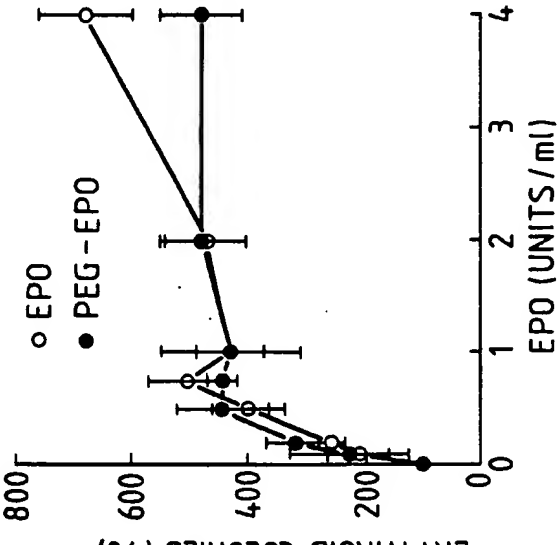


Fig.4a.

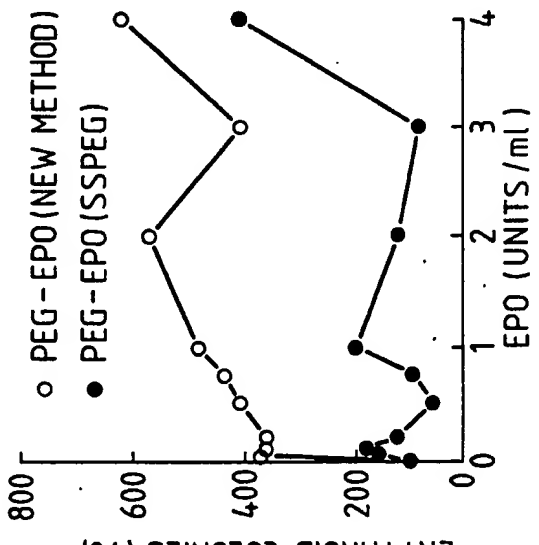


Fig.4c.

Fig.5.

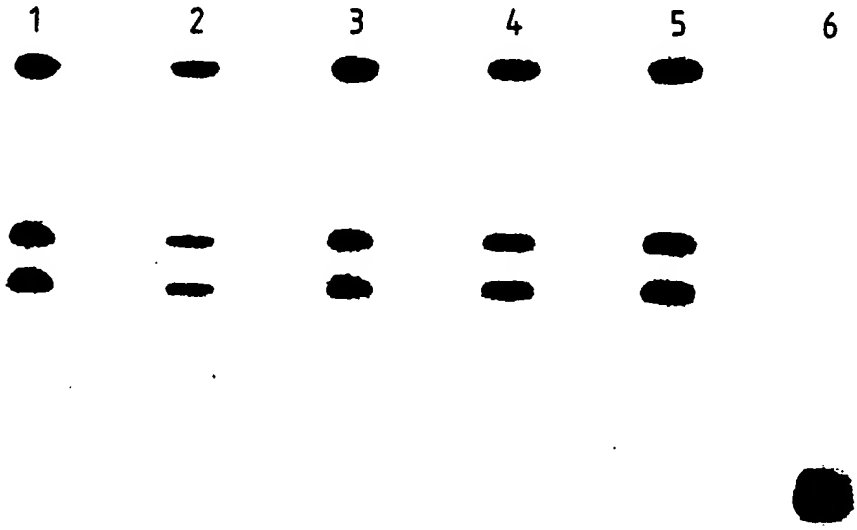

1
2
3
4
5
6

Fig.6a.

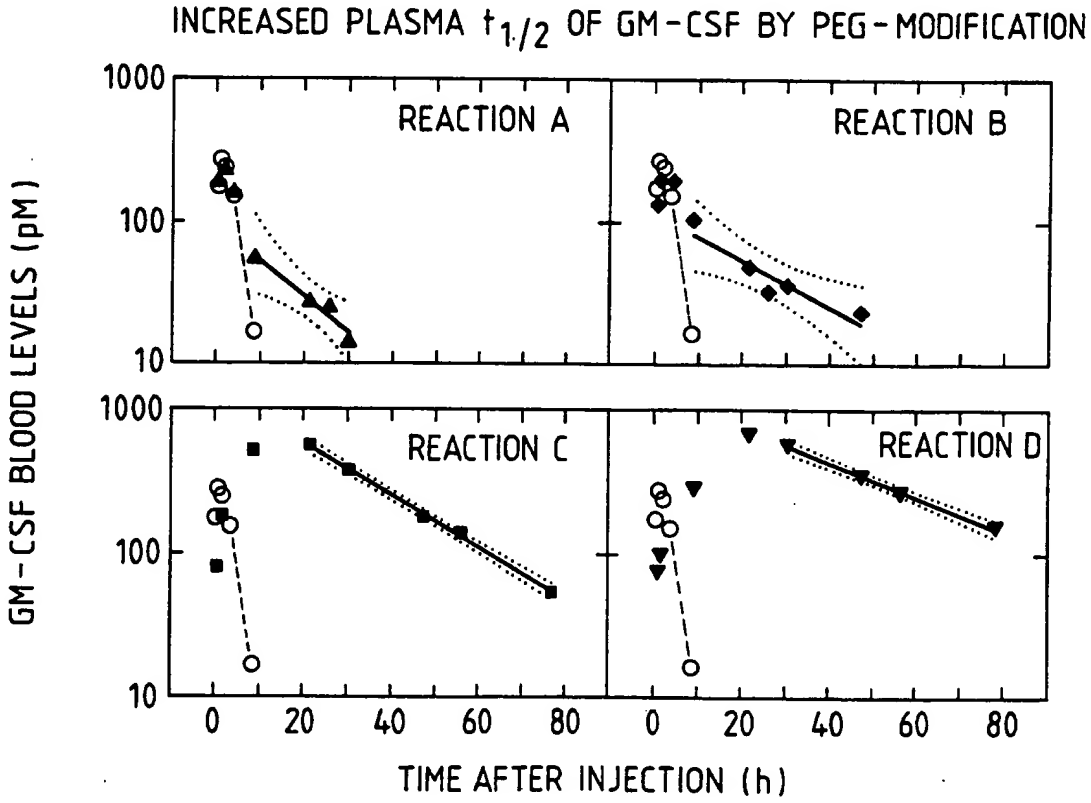

INCREASED PLASMA $t_{1/2}$ OF GM-CSF BY PEG-MODIFICATION
REACTION A
REACTION B
REACTION C
REACTION D
GM-CSF BLOOD LEVELS (pM)
1000
100
10
0
20
40
60
80
TIME AFTER INJECTION (h)

Fig.6b.

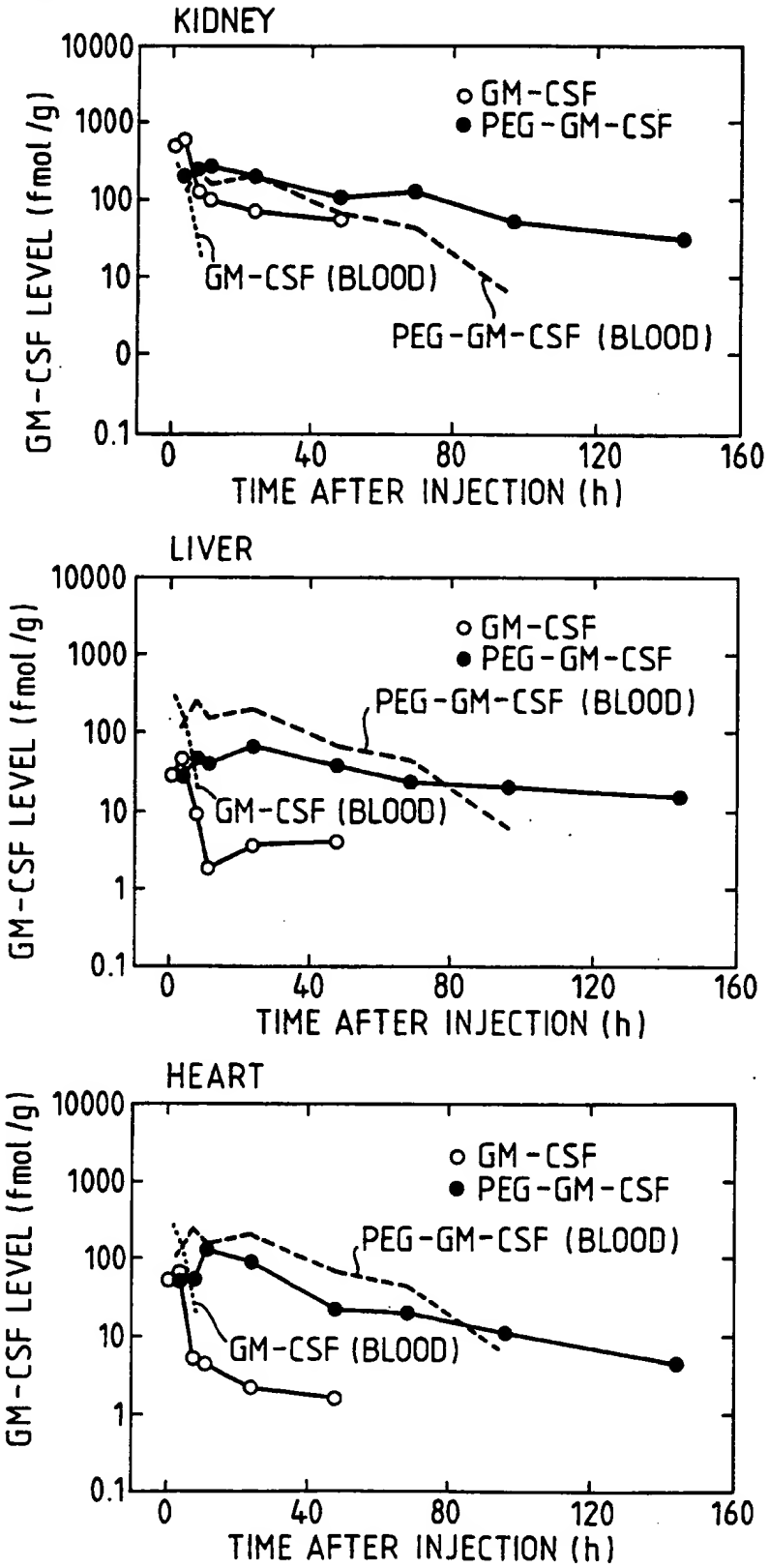
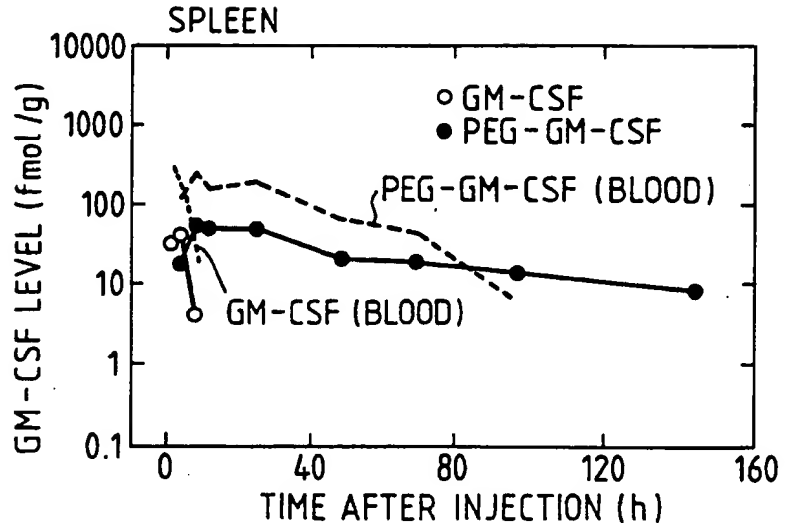
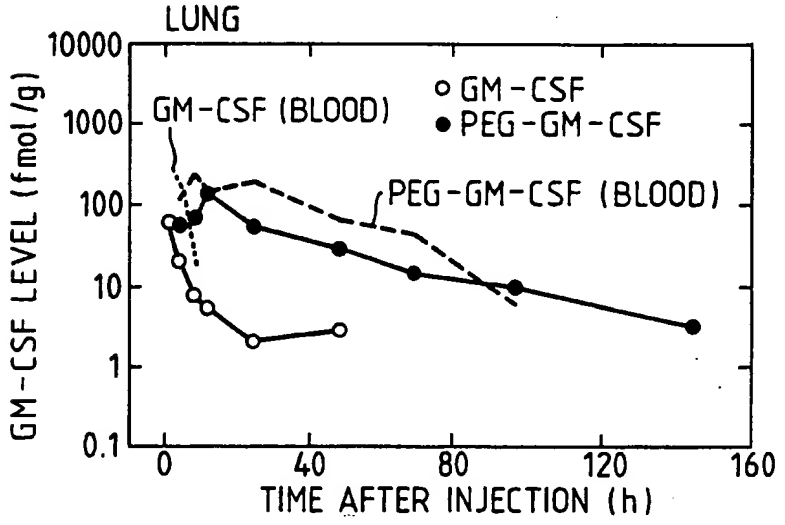

KIDNEY
GM-CSF LEVEL (fmol/g)
10000
1000
100
10
0
0.1
GM-CSF
PEG-GM-CSF
GM-CSF (BLOOD)
PEG-GM-CSF (BLOOD)
0
40
80
120
160
TIME AFTER INJECTION (h)
LIVER
GM-CSF LEVEL (fmol/g)
10000
1000
100
10
1
0.1
GM-CSF
PEG-GM-CSF
PEG-GM-CSF (BLOOD)
GM-CSF (BLOOD)
0
40
80
120
160
TIME AFTER INJECTION (h)
HEART
GM-CSF LEVEL (fmol/g)
10000
1000
100
10
1
0.1
GM-CSF
PEG-GM-CSF
PEG-GM-CSF (BLOOD)
GM-CSF (BLOOD)
0
40
80
120
160
TIME AFTER INJECTION (h)

Fig.6b(Cont).


SPLEEN
GM-CSF LEVEL (fmol/g)
10000
1000
100
10
1
0.1
o GM-CSF
● PEG-GM-CSF
PEG-GM-CSF (BLOOD)
GM-CSF (BLOOD)
0
40
80
120
160
TIME AFTER INJECTION (h)


LUNG
GM-CSF LEVEL (fmol/g)
10000
1000
100
10
1
0.1
GM-CSF (BLOOD)
o GM-CSF
● PEG-GM-CSF
PEG-GM-CSF (BLOOD)
0
40
80
120
160
TIME AFTER INJECTION (h)

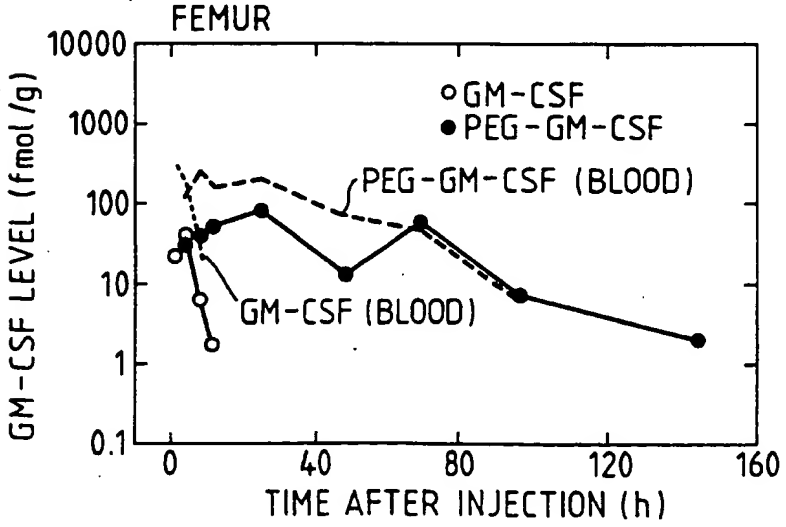

FEMUR
GM-CSF LEVEL (fmol/g)
10000
1000
100
10
1
0.1
o GM-CSF
● PEG-GM-CSF
PEG-GM-CSF (BLOOD)
GM-CSF (BLOOD)
0
40
80
120
160
TIME AFTER INJECTION (h)

Fig.7.

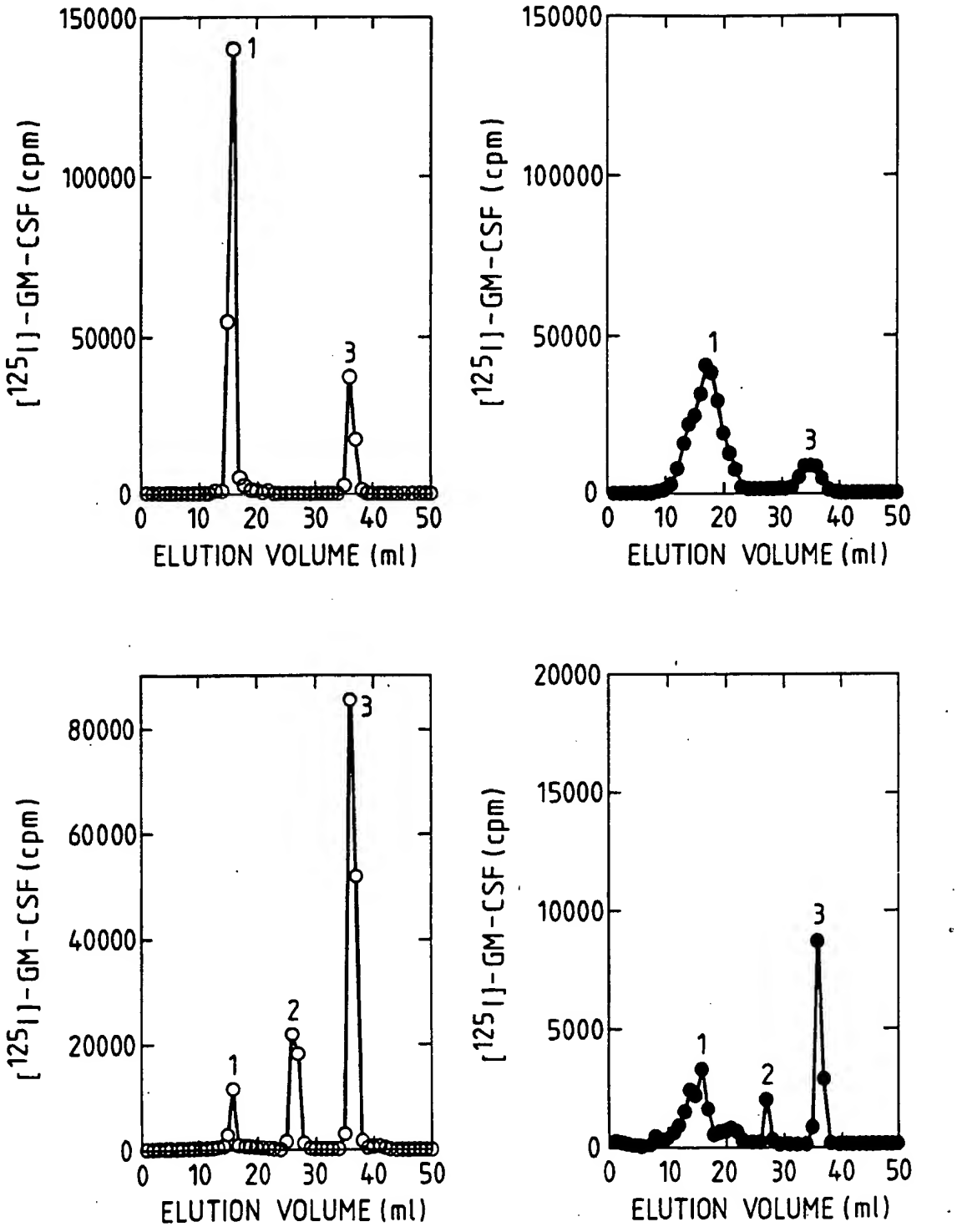

150000
100000
50000
0
[125I]-GM-CSF (cpm)
1
3
0 10 20 30 40 50
ELUTION VOLUME (ml)
150000
100000
50000
0
[125I]-GM-CSF (cpm)
1
3
0 10 20 30 40 50
ELUTION VOLUME (ml)
80000
60000
40000
20000
0
[125I]-GM-CSF (cpm)
1
2
3
0 10 20 30 40 50
ELUTION VOLUME (ml)
20000
15000
10000
5000
0
[125I]-GM-CSF (cpm)
1
2
3
0 10 20 30 40 50
ELUTION VOLUME (ml)

Fig.8a.

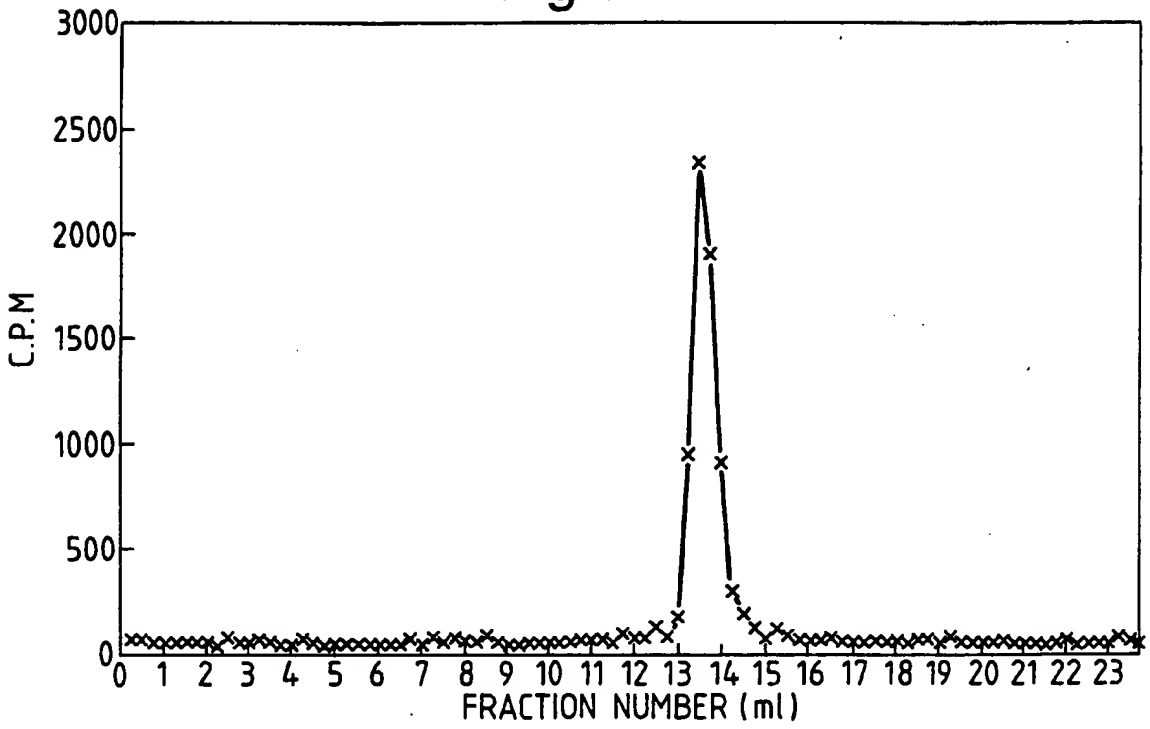

3000
2500
2000
1500
1000
500
0
C.P.M
0 1 2 3 4 5 6 7 8 9 10 11 12 13 14 15 16 17 18 19 20 21 22 23
FRACTION NUMBER (ml)

Fig.8b.

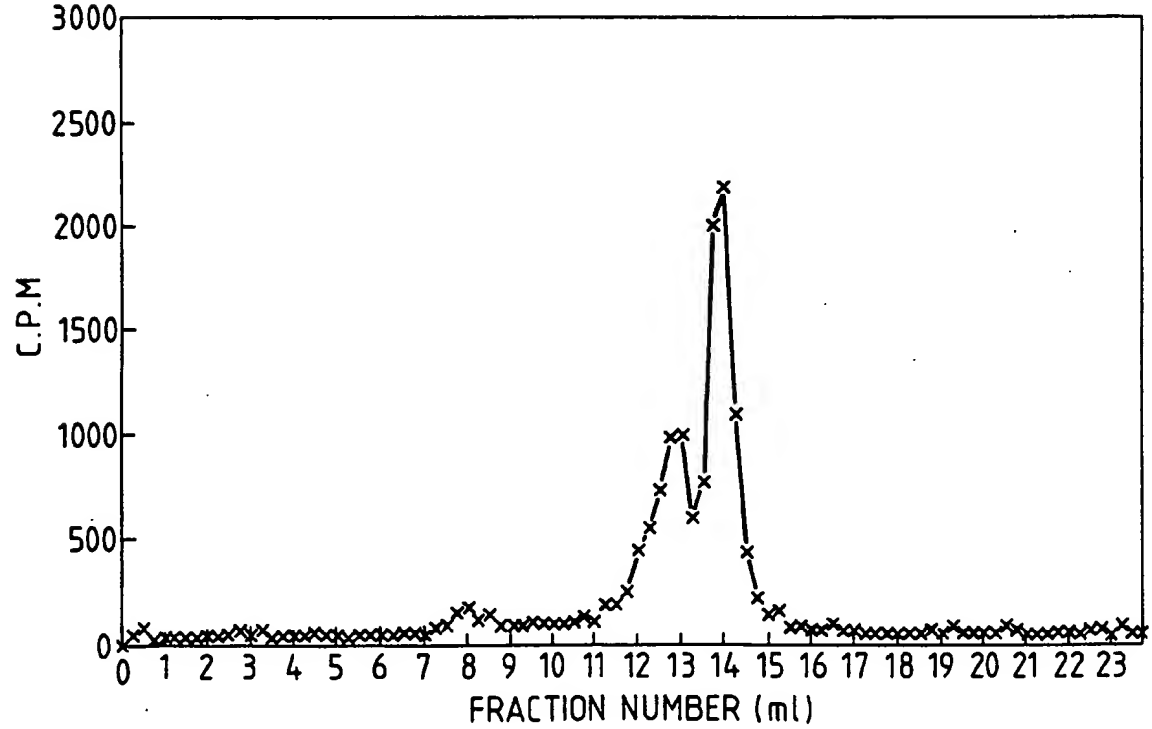

3000
2500
2000
1500
1000
500
0
C.P.M
0 1 2 3 4 5 6 7 8 9 10 11 12 13 14 15 16 17 18 19 20 21 22 23
FRACTION NUMBER (ml)

Fig.8c.

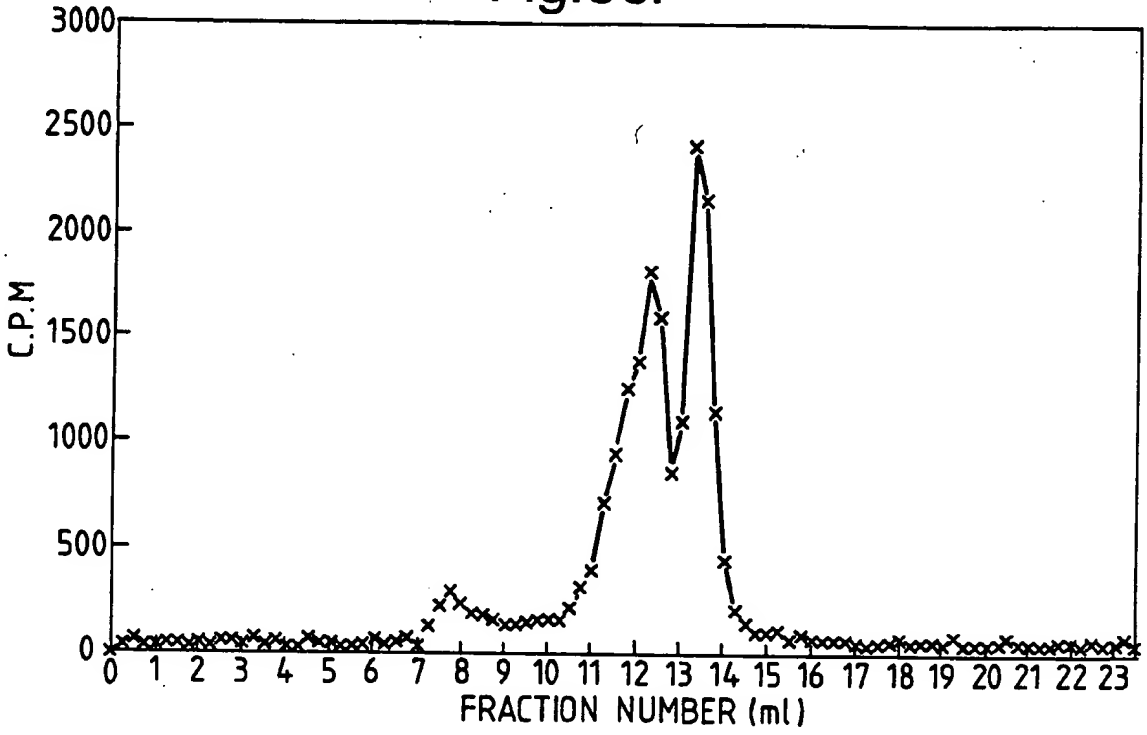

3000
2500
2000
1500
1000
500
0
C.P.M
0 1 2 3 4 5 6 7 8 9 10 11 12 13 14 15 16 17 18 19 20 21 22 23
FRACTION NUMBER (ml)

Fig.8d.

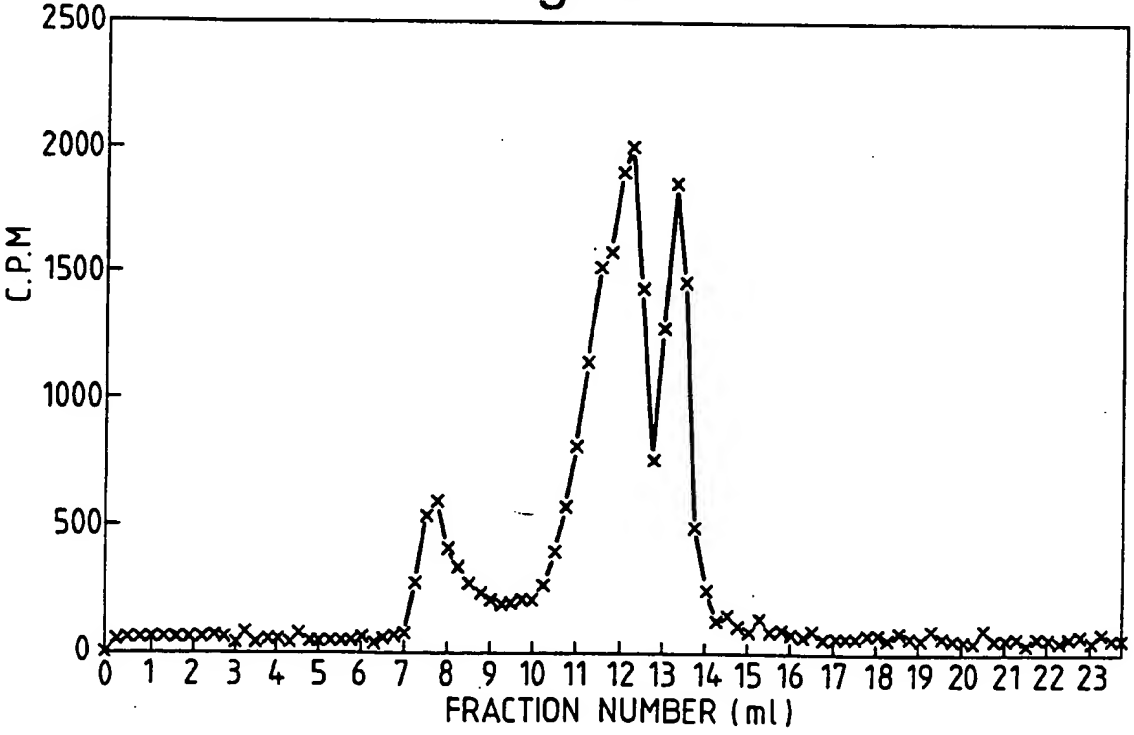

2500
2000
1500
1000
500
0
C.P.M
0 1 2 3 4 5 6 7 8 9 10 11 12 13 14 15 16 17 18 19 20 21 22 23
FRACTION NUMBER (ml)

Fig.8e.

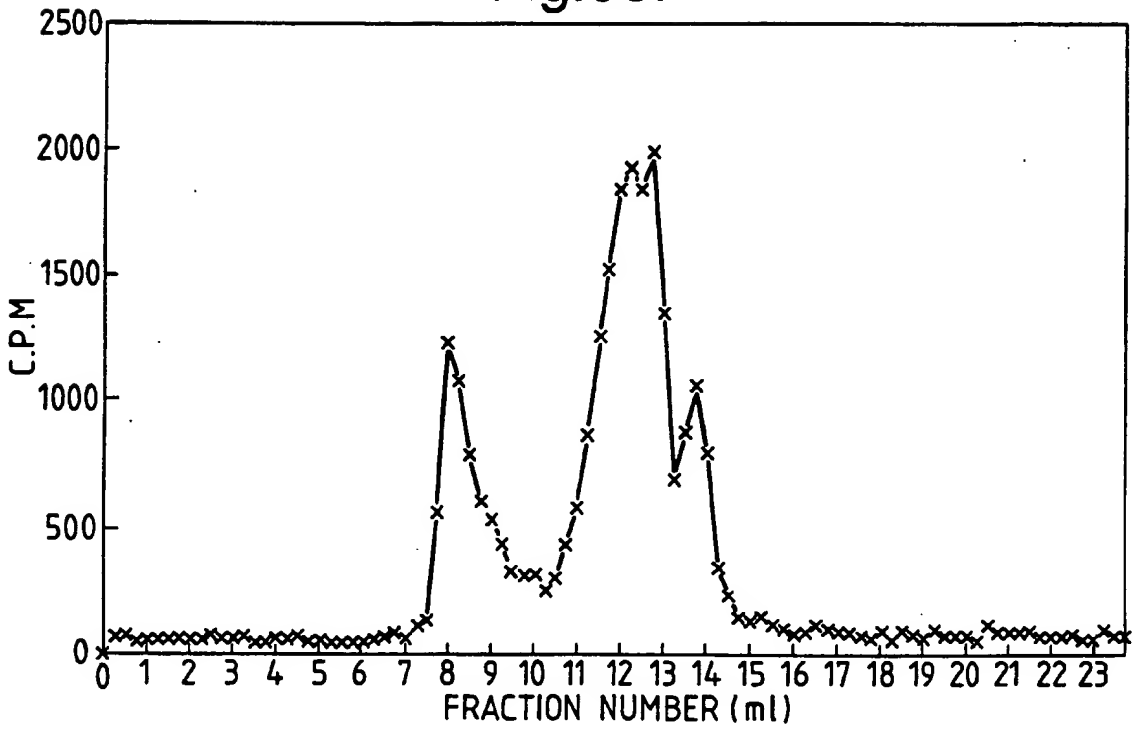

2500
2000
1500
1000
500
0
C.P.M
0 1 2 3 4 5 6 7 8 9 10 11 12 13 14 15 16 17 18 19 20 21 22 23
FRACTION NUMBER (ml)

Fig.8f.

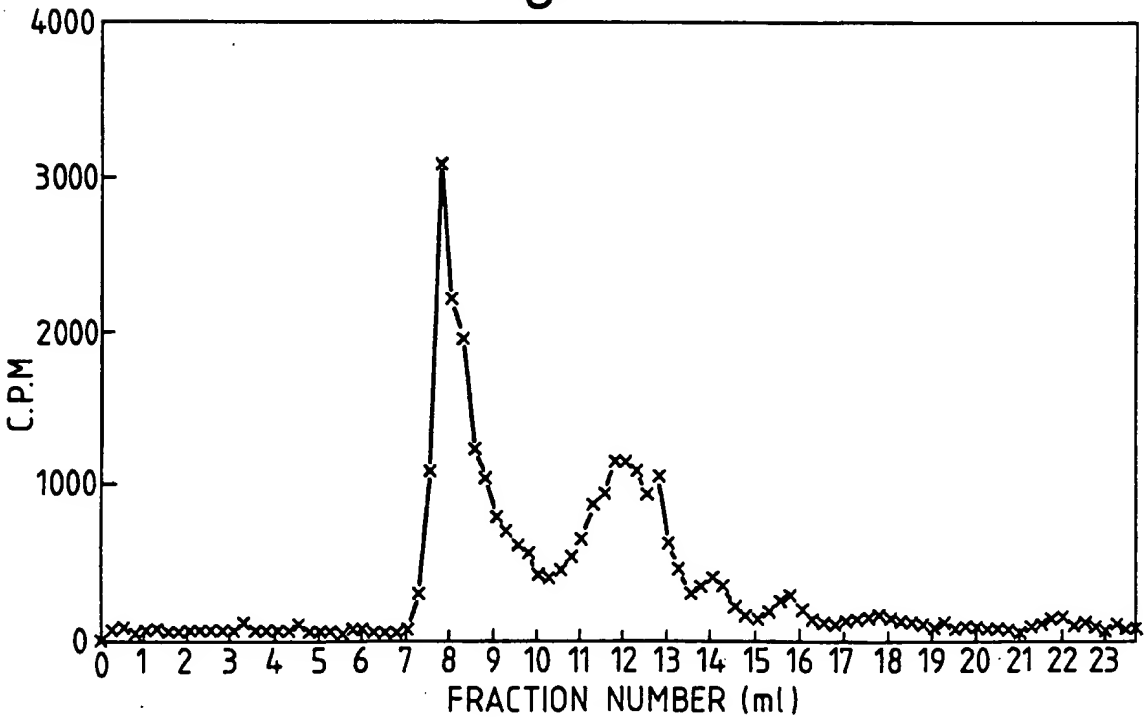

4000
3000
2000
1000
0
C.P.M
0 1 2 3 4 5 6 7 8 9 10 11 12 13 14 15 16 17 18 19 20 21 22 23
FRACTION NUMBER (ml)

Fig.9a.

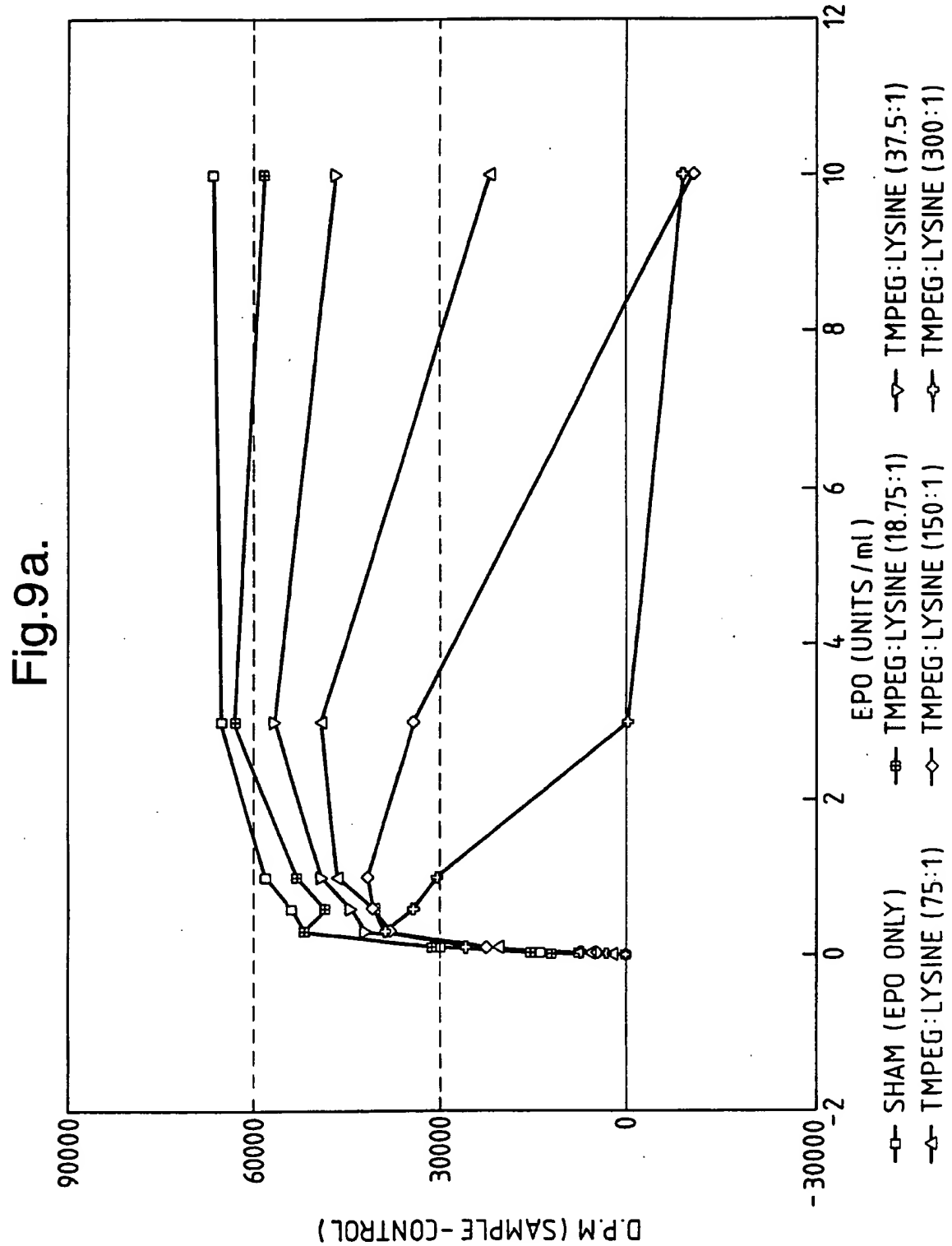
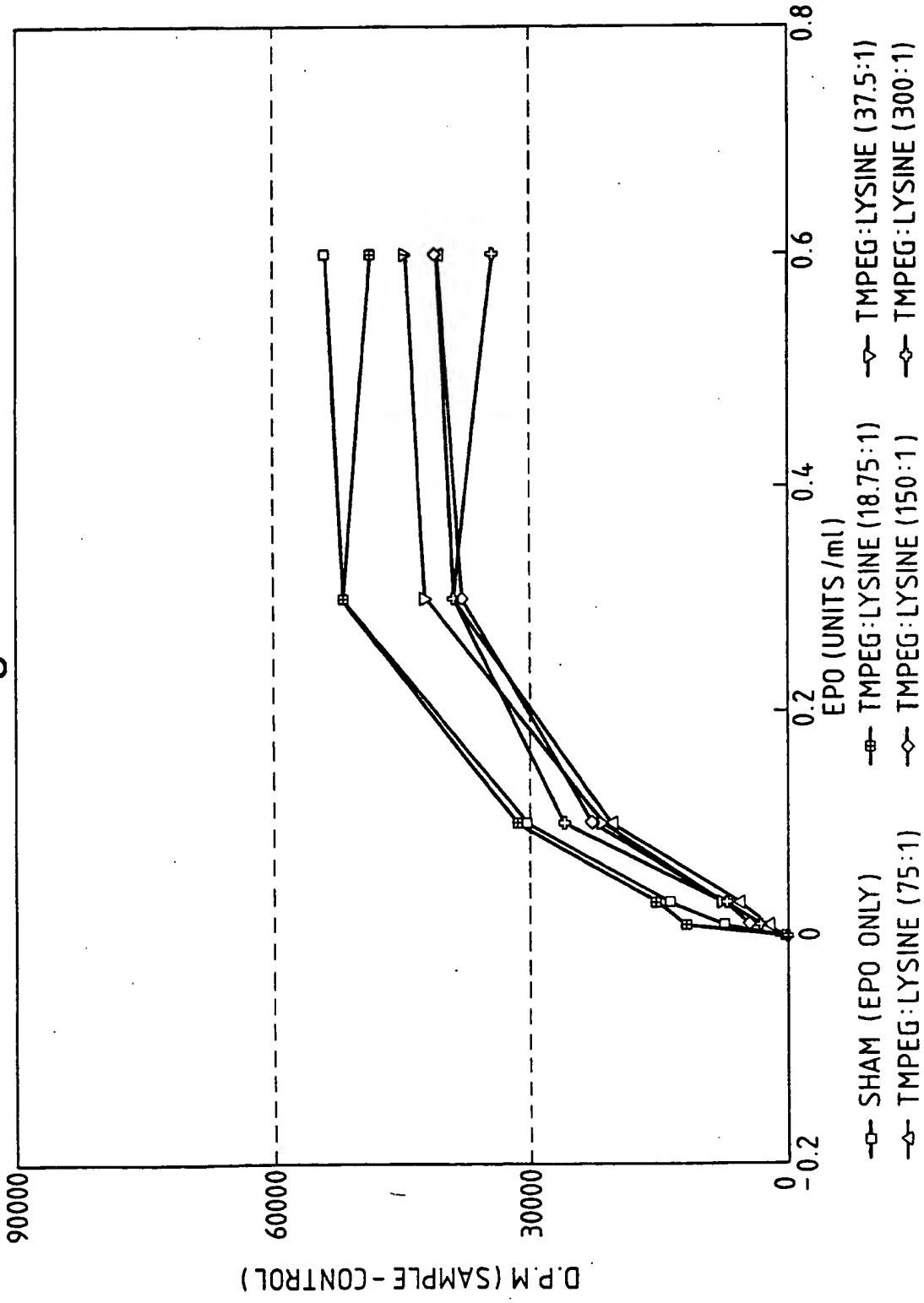

D.P.M (SAMPLE - CONTROL)
90000
60000
30000
0
-30000
-2
0
2
4
6
8
10
12
EPO (UNITS / ml)
SHAM (EPO ONLY)
TMPEG:LYSINE (75:1)
TMPEG:LYSINE (18.75:1)
TMPEG:LYSINE (150:1)
TMPEG:LYSINE (37.5:1)
TMPEG:LYSINE (300:1)

Fig.9b.


D.P.M (SAMPLE - CONTROL)
90000
60000
30000
0
-0.2
0
0.2
0.4
0.6
0.8
EPO (UNITS/ml)
SHAM (EPO ONLY)
TMPEG:LYSINE (75:1)
TMPEG:LYSINE (18.75:1)
TMPEG:LYSINE (150:1)
TMPEG:LYSINE (37.5:1)
TMPEG:LYSINE (300:1)

INTERNATIONAL SEARCH REPORT

Inter nal Application No
PCT/GB 94/01844

A. CLASSIFICATION OF SUBJECT MATTER
IPC 6 C07K1/10 C07K1/13 A61K49/00 A61K47/48 A61K9/127

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
IPC 6 C07K A61K

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	WO,A,90 04606 (ROYAL FREE HOSPITAL SCHOOL OF MEDICINE) 3 May 1990 cited in the application see page 14 - page 16; table II	1,2, 4-11, 20-25
X	WO,A,90 04650 (ROYAL FREE HOSPITAL SCHOOL OF MEDICINE) 3 May 1990 cited in the application see page 7 - page 9	1,2, 4-11, 14-18, 20-25
X	WO,A,90 04384 (ROYAL FREE HOSPITAL SCHOOL OF MEDICINE) 3 May 1990 cited in the application see page 3, line 8-9	1,2, 4-11, 14-25

-/--

[X] Further documents are listed in the continuation of box C.

[X] Patent family members are listed in annex.

* Special categories of cited documents :

"A" document defining the general state of the art which is not considered to be of particular relevance

"E" earlier document but published on or after the international filing date

"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

"O" document referring to an oral disclosure, use, exhibition or other means

"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.

"&" document member of the same patent family

Date of the actual completion of the international search	Date of mailing of the international search report
15 December 1994	01. 02. 95
Name and mailing address of the ISA European Patent Office, P.B. 5818 Patentlaan 2 NL - 2280 HV Rijswijk Tel. (+ 31-70) 340-2040, Tx. 31 651 epo nl, Fax (+ 31-70) 340-3016	Authorized officer Deffner, C-A

Form PCT/ISA/210 (second sheet) (July 1992)

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	EXP.HEMATOL., vol.20, 1992 pages 1028 - 35 F.MALIK ET AL. 'Polyethylene Glycol (PEG)-modified Granulocyte-Macrophage Colony-stimulating Factor (GM-CSF) with conserved Biological Activity' *Materials and Methods* ---	1,2, 4-11, 14-18, 20-25
X	BIOTECHNOL.APPL.BIOCHEM., vol.12, no.2, 1990 pages 119 - 128 C.DELAGO ET AL. 'Coupling of Poly(ethylene glycol) to Albumin under Very Mild Conditions by Activation with Tresyl Chloride: Characterization of the Conjugate by Partitioning in Aqueous Two-Phase Systems' *Materials and Methods* ---	1,2, 5-11, 14-25
X	BIOCHEM.BIOPHYS.ACTA, vol.106, 1991, NETHERLAND pages 77 - 82 J.SENIOR ET AL. 'Influence of surface hydrophilicty of liposomes on their interaction with plasma protein and clearance from the circulation: studies with poly(ethylene glycol)-coated vesicles' see the whole document ---	1,2, 4-11, 14-25
X	BRITHISH JOURNAL OF HAEMATOLOGY, vol.82, 1992 pages 654 - 663 C.KNUSLI ET AL. 'Polyethylene glycol (PEG) modification of granulocyte-macrophage colony stimulating factor (GM-CSF) enhances neutrophil priming activity but not colony stimulating activity' see figures 1-4 ---	1,2, 4-11, 14-23
X	ANALYTICAL.BIOCHEM., vol.134, 1983 pages 60 - 72 K.NILSSON ET AL. 'High-Performance Liquid Chromatography on Silica-Bound Alcohol Dehydrogenase' *Materials and Methods* ---	1,2, 4-11, 14-18, 20-25
X	BIOCHEM.SOC.TRANS., vol.16, no.6, 1988 pages 968 - 969 C.DELAGO ET AL. 'Immunoaffinity cell partitioning of erythrocytes' see the whole document -----	1,2, 4-11, 14-18, 20-25

1

INTERNATIONAL SEARCH REPORT

...information on patent family members

Inter. nal Application No
PCT/GB 94/01844

Patent document cited in search report	Publication date	Patent family member(s)		Publication date
WO-A-9004606	03-05-90	EP-A-	0439508	07-08-91
		JP-T-	4501260	05-03-92
		US-A-	5349052	20-09-94
WO-A-9004650	03-05-90	EP-A-	0439502	07-08-91
		JP-T-	4501356	12-03-92
WO-A-9004384	03-05-90	DE-D-	68915001	01-06-94
		DE-T-	68915001	04-08-94
		EP-A-	0445131	11-09-91
		EP-A-	0572049	01-12-93
		JP-T-	4501117	27-02-92